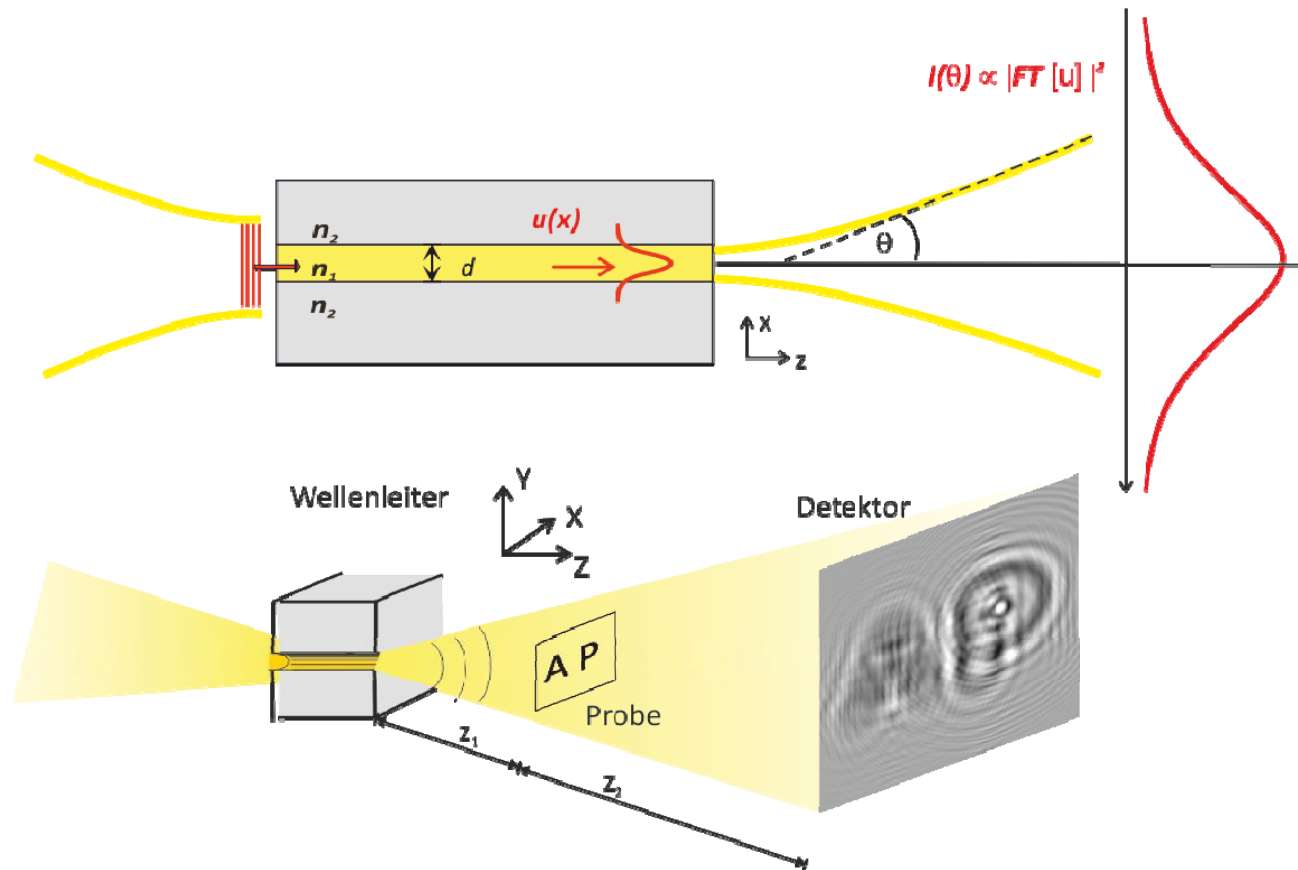


*x-ray imaging at the nanoscale /
mit Röntgenaugen im Nanokosmos unterwegs*



Tim Salditt, Institut für Röntgenphysik
joint work with Matthias Bartels, Robin Wilke, Marius Priebe
Klaus Giewekemeyer, Markus Osterhoff
Universität Göttingen,
Physik-Kolloquium Oldenburg, 7.11.2011

Content

1. Why x-ray imaging ?
2. The phase problem and its solution by iterative phasing
- 3. far-field (CDI) versus near-field (propagation) imaging**
- 4. The Göttingen endstation for nano-imaging**
at the coherence beamline PETRAIII HASYLAB /DESY
- 5. X-ray waveguide optics**
- 6. Applications in biological imaging**
7. The advent of X-ray Free Electron Lasers (XFEL)

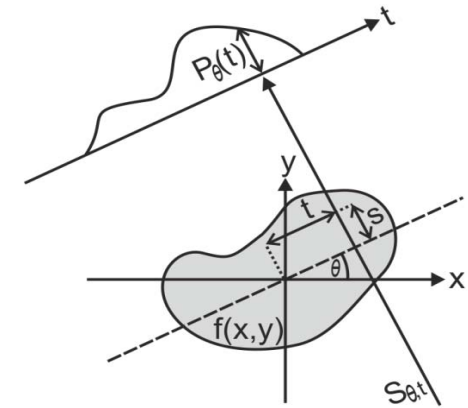
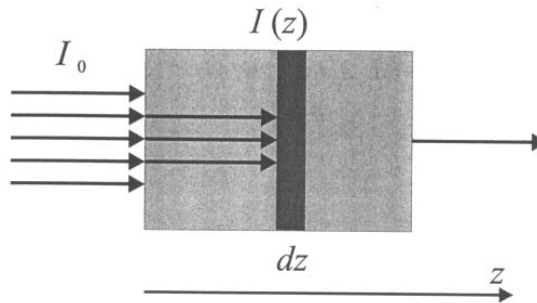
joined work with

*Matthias Bartels, Robin Wilke, Marius Priebe, Markus Osterhoff, Sebastian Kalbfleisch
Scen Krüger, Henrike Neubauer, Dr. Klaus Giewekemeyer*

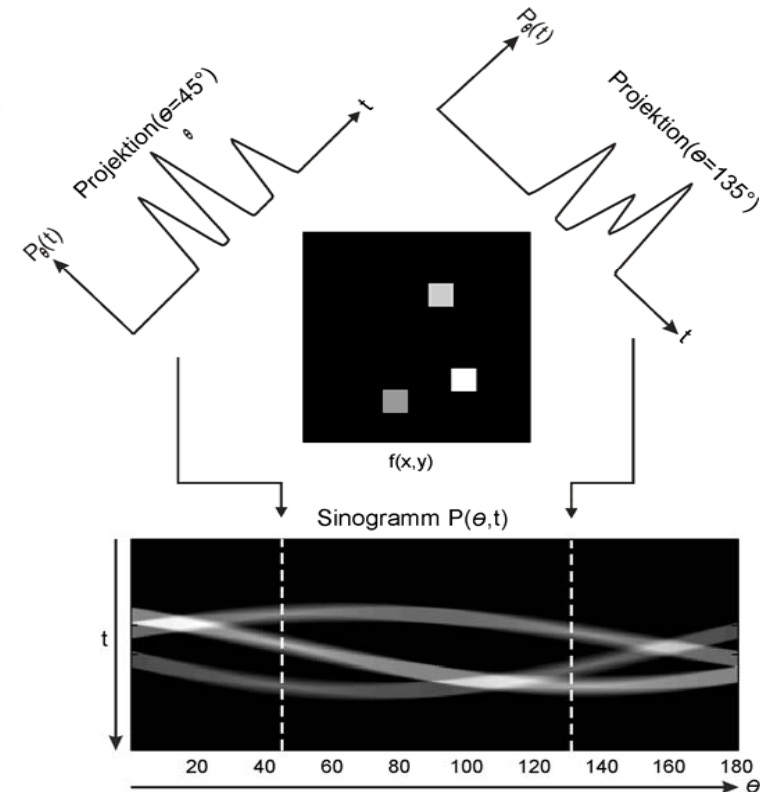
1. Imaging with x-rays- advantage No.1: transparency



$$I(z) = I_0 e^{-\mu z}$$



tomography



absorption coefficient $\mu \sim E^{-3} Z^{-4}$

look into biomaterials

(bulk information)

absorption versus phase contrast

$$n = 1 - \delta + i\beta$$

x-ray index of refraction

$$u(x, y) = u_0(x, y) \tau(x, y)$$

$$\tau(x, y) = \exp\left[-k \int_z^{z+d} dz (\beta(x, y, z) + i\delta(x, y, z))\right]$$

$$\delta = 10^{-5} \dots 10^{-9}$$

$$\beta = 10^{-7} \dots 10^{-13}$$

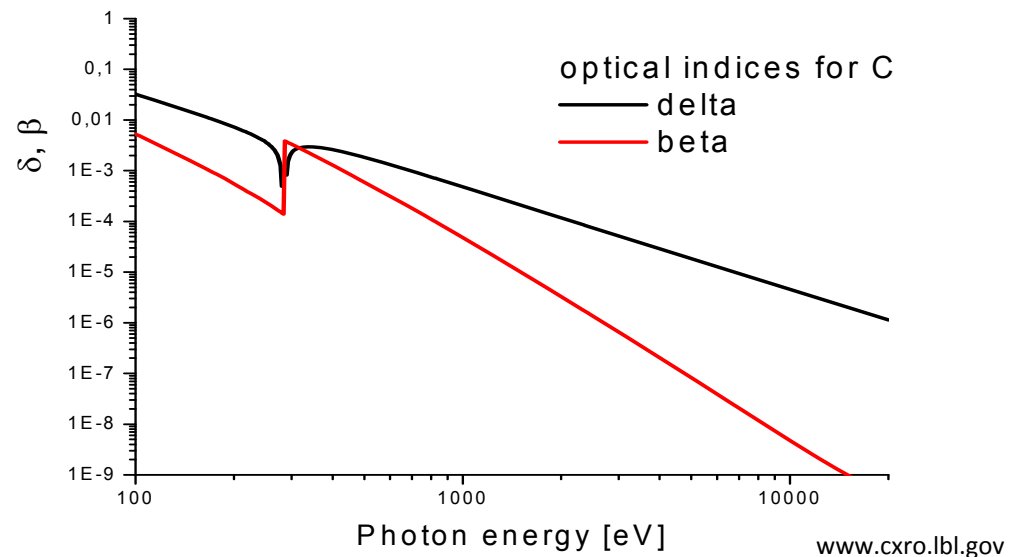
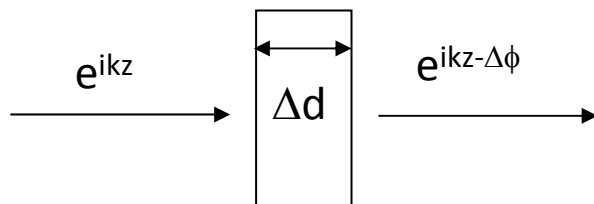
Absorption length μ

$$\beta = \frac{\mu}{2k}$$

Phase shift

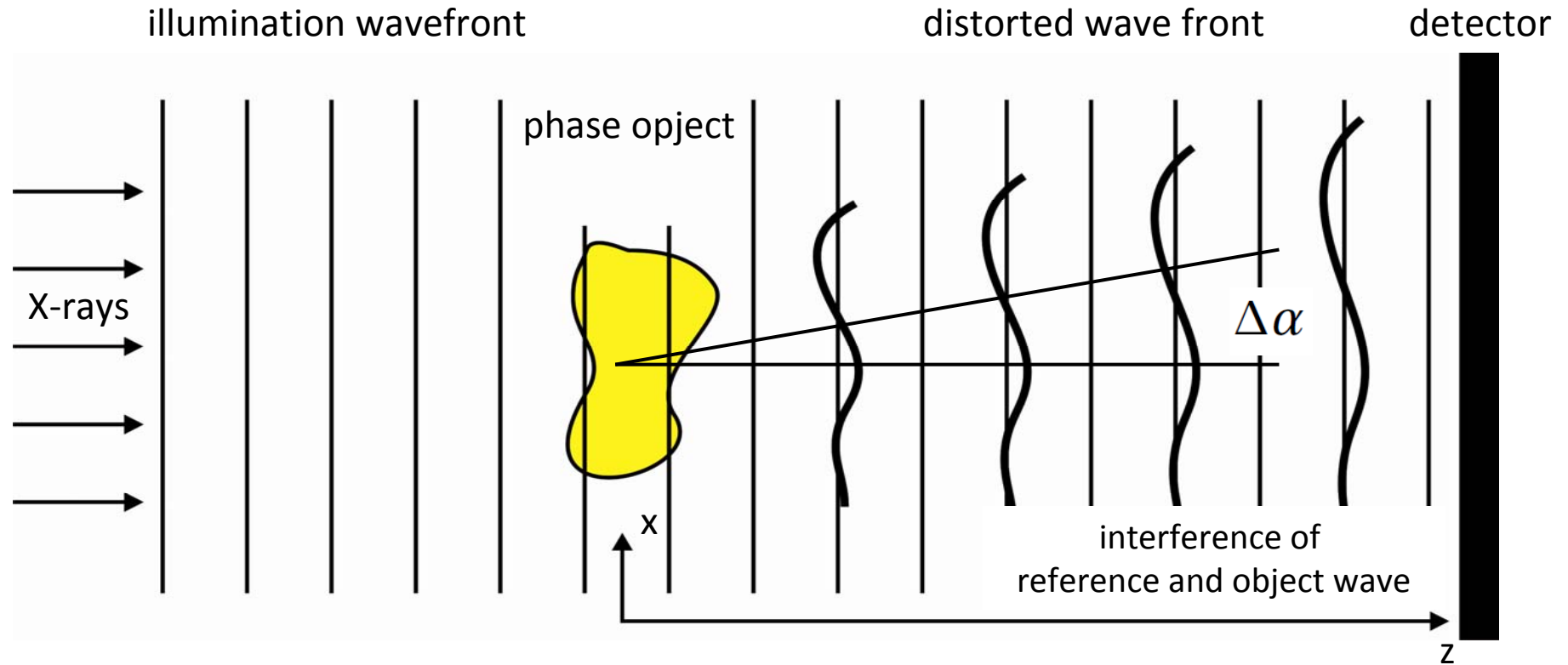
$$\Delta\phi = k \Delta d (1 - n)$$

slab with index n



$\delta \gg \beta$ for low Z elements and high photon energies \rightarrow phase contrast

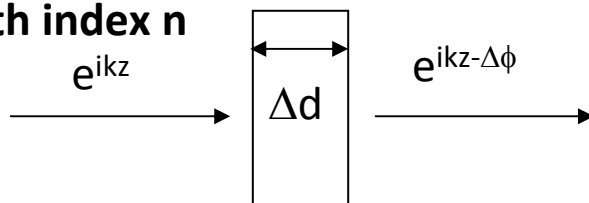
Propagation imaging



phase shift

$$\Delta\phi = k \Delta d (1 - n)$$

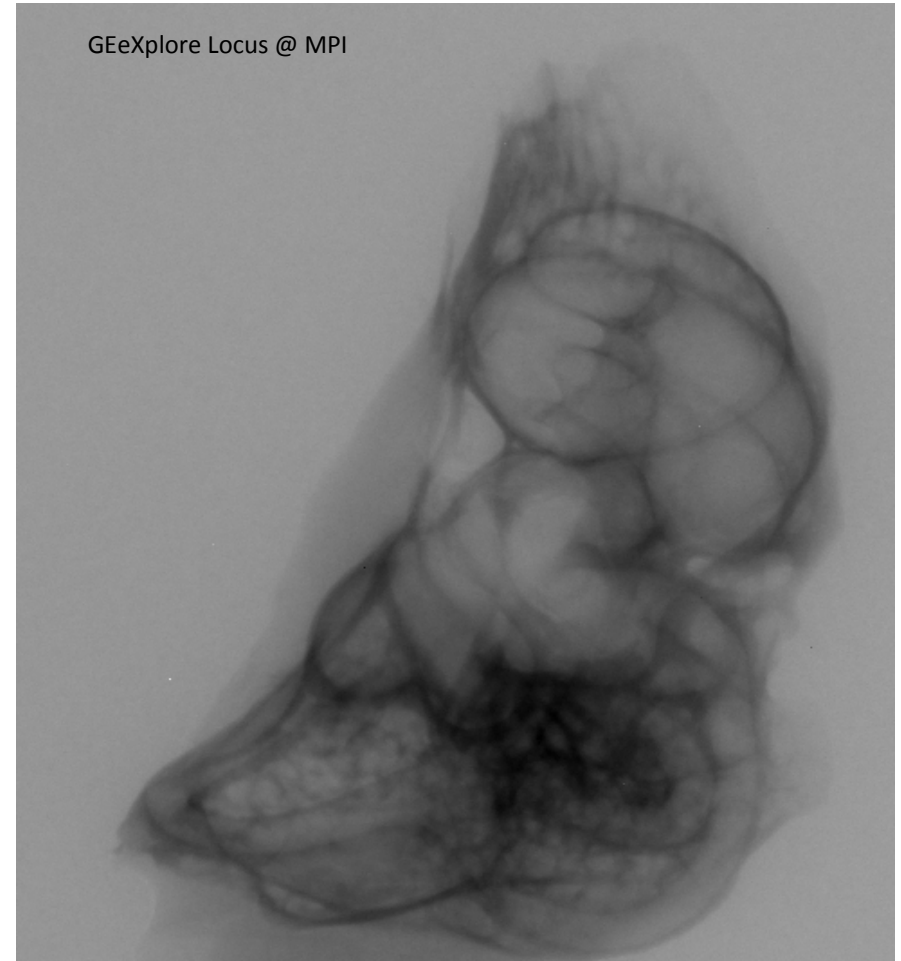
slab with index n



free space propagation

$$\Delta\alpha = \frac{\lambda}{2\pi} \frac{\partial\phi}{\partial x}$$

Density in 3D : *resolution AND contrast matter !*



Cochlea: Phase contrast vs. Absorption contrast

X-ray advantage No.2:

(a) quantitative contrast and weak scattering cross section

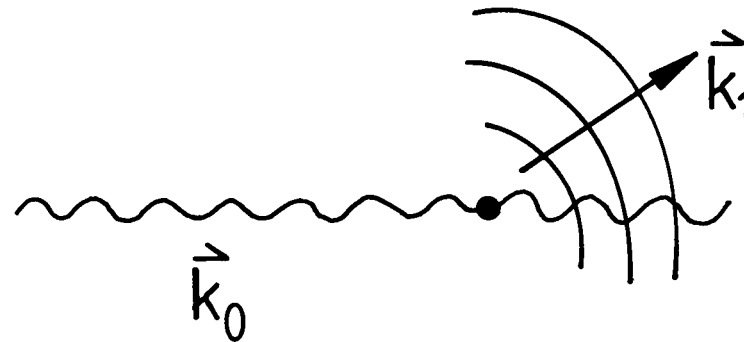


index $n = 1 - \delta + i\beta$, $\delta, \beta \approx 10^{-5}-10^{-6}$
close to 1.

⇒ reduced reflections at internal interfaces

no multiple scattering

(look through foam of beer, R.W. Pohl 1939)

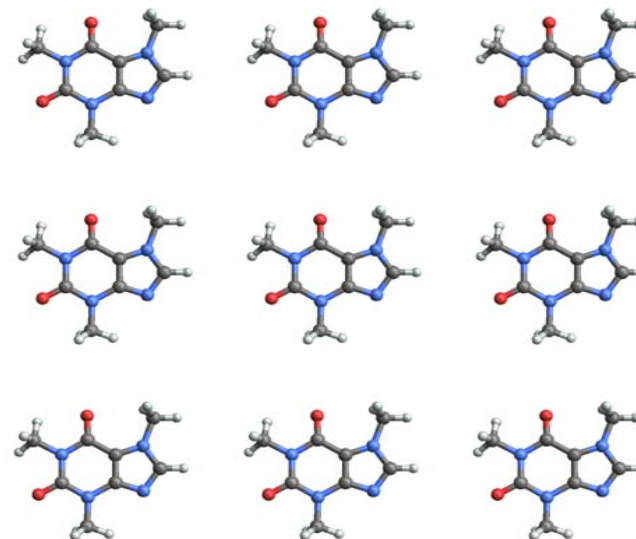
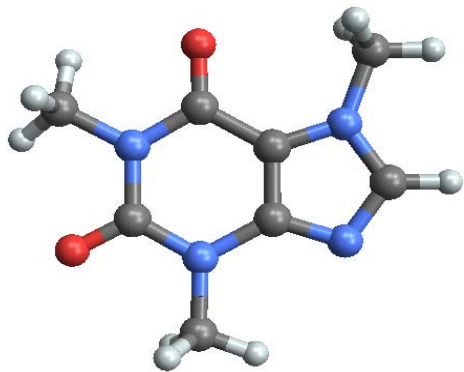


$$e^{i\vec{k}_0 \cdot \vec{r}} \longrightarrow e^{i\vec{k}_0 \cdot \vec{r}} + f(\Omega) \frac{e^{i\vec{k}_0 \cdot \vec{r}}}{r}$$

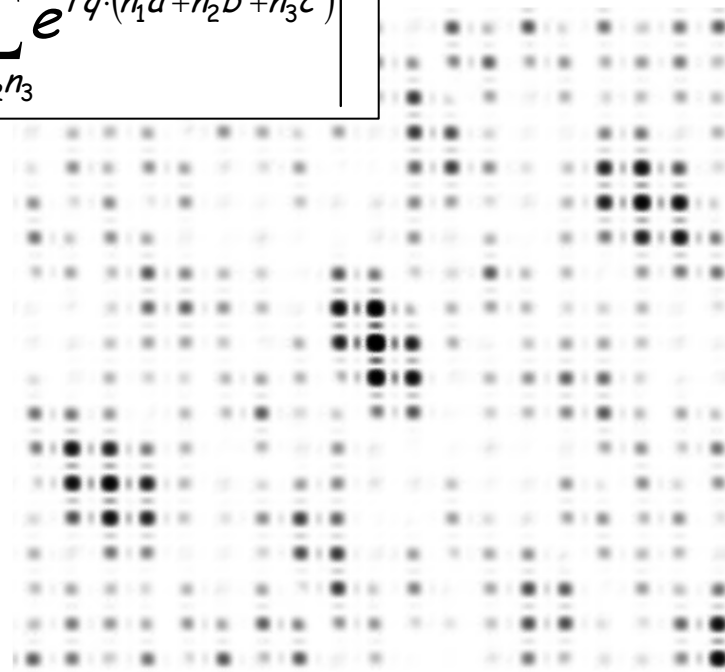
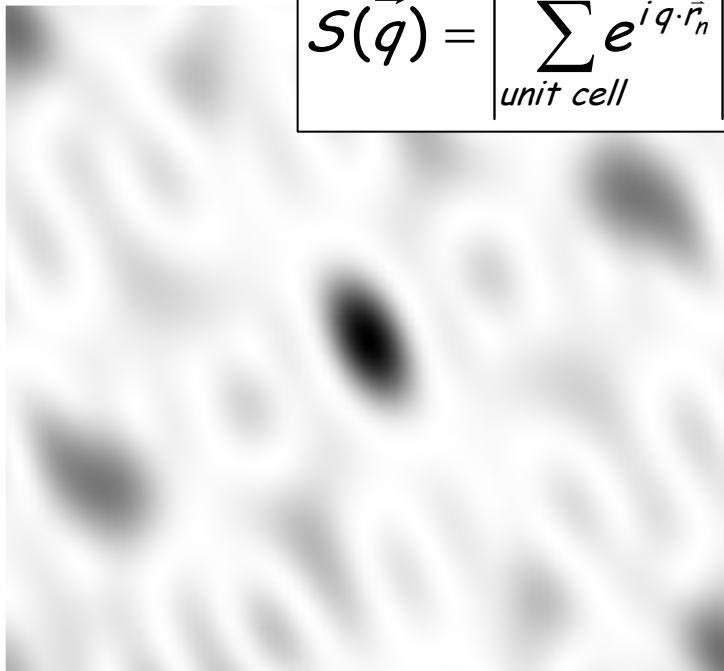
$f(\Omega)$ amplitude, $[f(\Omega)] = m$ „scattering length“
 $f = 2.82 \cdot 10^{-15} \text{ m}$

(Born Approx.)

crystallography = averaging over $10^{12} - 10^{18}$ copies of the same molecule



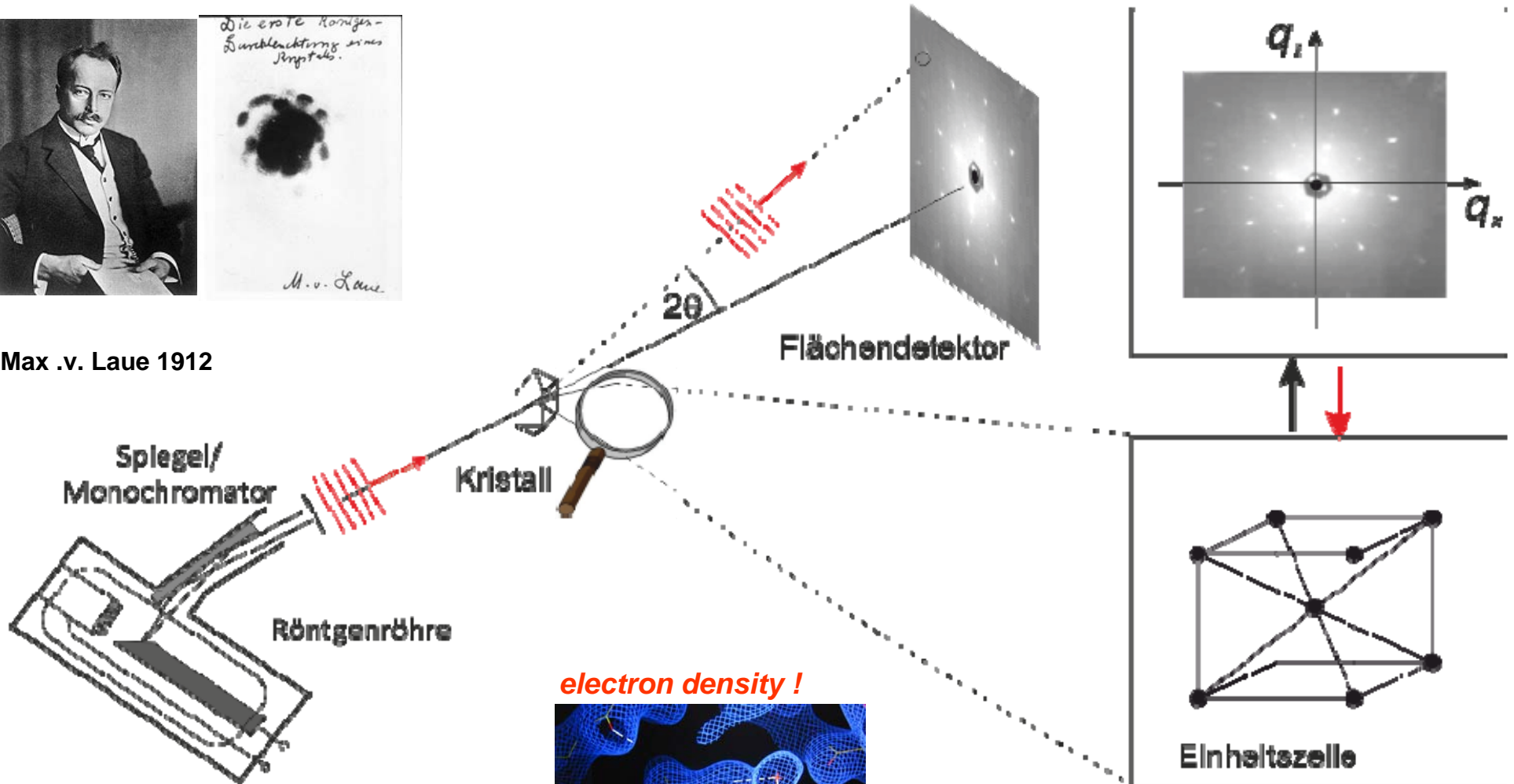
$$S(\vec{q}) = \left| \sum_{\text{unit cell}}^N e^{i\vec{q}\cdot\vec{r}_n} \right|^2 \left| \sum_{n_1 n_2 n_3} e^{i\vec{q}\cdot(n_1\vec{a}+n_2\vec{b}+n_3\vec{c})} \right|^2$$



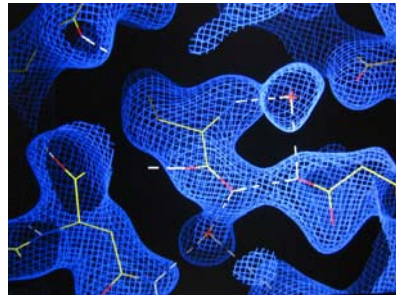
Advantage No.3: small wavelength – high resolution



Max .v. Laue 1912



electron density !

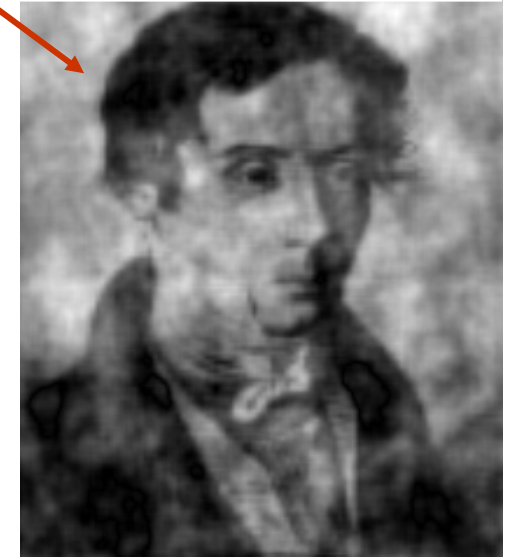
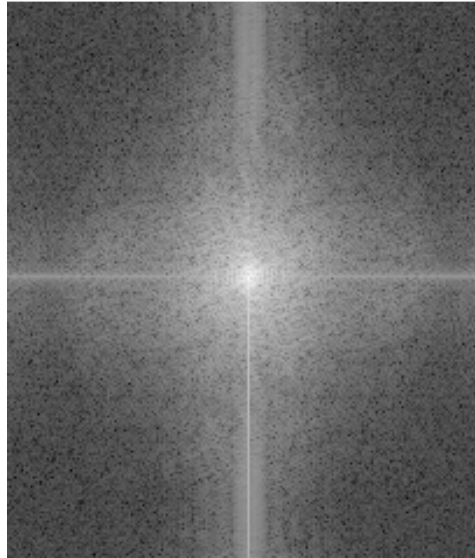
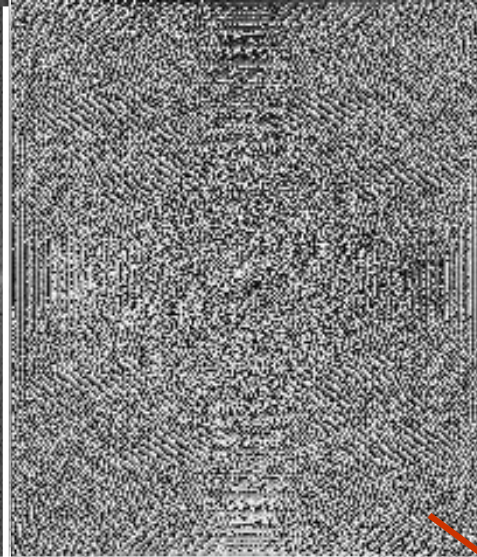
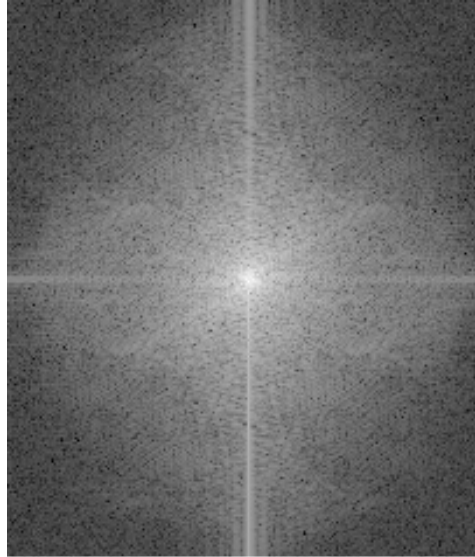


X-ray nobel prizes:
Laue, Bragg, Debye, Perutz&Kendrew, Hodgkin, Watson&Crick,
Deisenhofer, Huber & Michel, Agre, McKinnon,
And many more (> 25 scientists !)

The phase problem

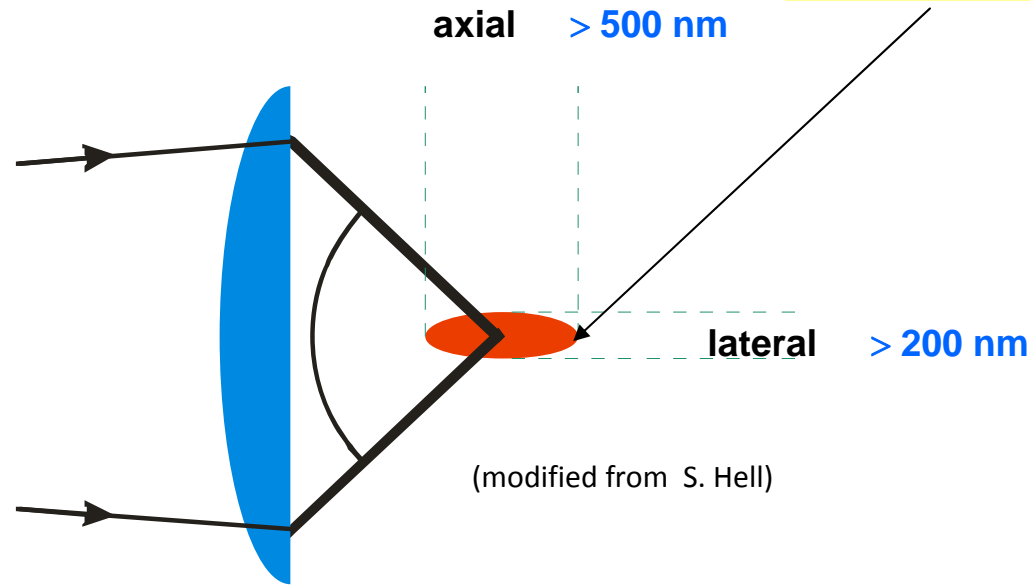
Amplitude

Phase



$$\hat{\rho}_{kl} = \frac{1}{\sqrt{N \cdot M}} \sum_{i=0}^{N-1} \sum_{j=0}^{M-1} \rho_{ij} e^{-2\pi i \left(\frac{ik}{N} + \frac{j'l}{M} \right)}$$

$$\Delta x \approx \frac{\lambda}{2n \sin \alpha}$$



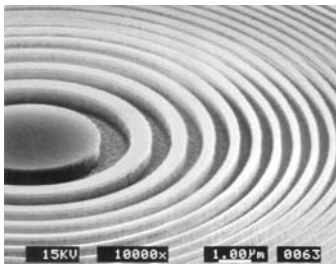
Conventional light microscopy is limited by diffraction.

lens / zone plate

axial $\sim 1 \mu\text{m}$

lateral 20 nm

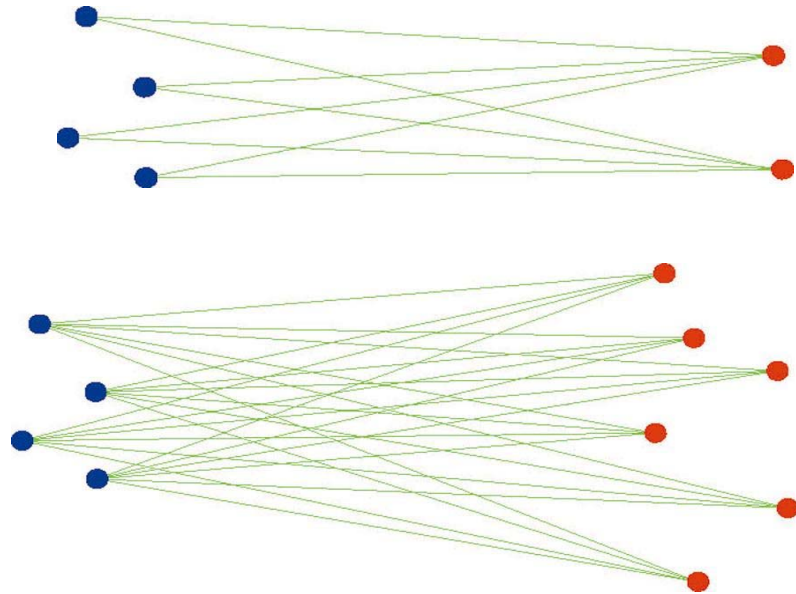
Conventional X-ray microscopy is limited by diffraction Structures.



Fresnel Zone Plate (FZP)

„Oversampling“: a strategy to render the problem unique ?

real space $|\mathcal{F}|$ reciprocal space



**Information theory (Shannon) ?
really more information**

“Oversampling”

$$I(q_{kl}) = F(q_{kl}) F^*(q_{kl}) = \left| \sum_i \sum_j \rho_{ij} e^{-i(q_k x_i + q_l y_i)} \right|^2$$

$$h, k, i, j = 0 \dots N - 1$$

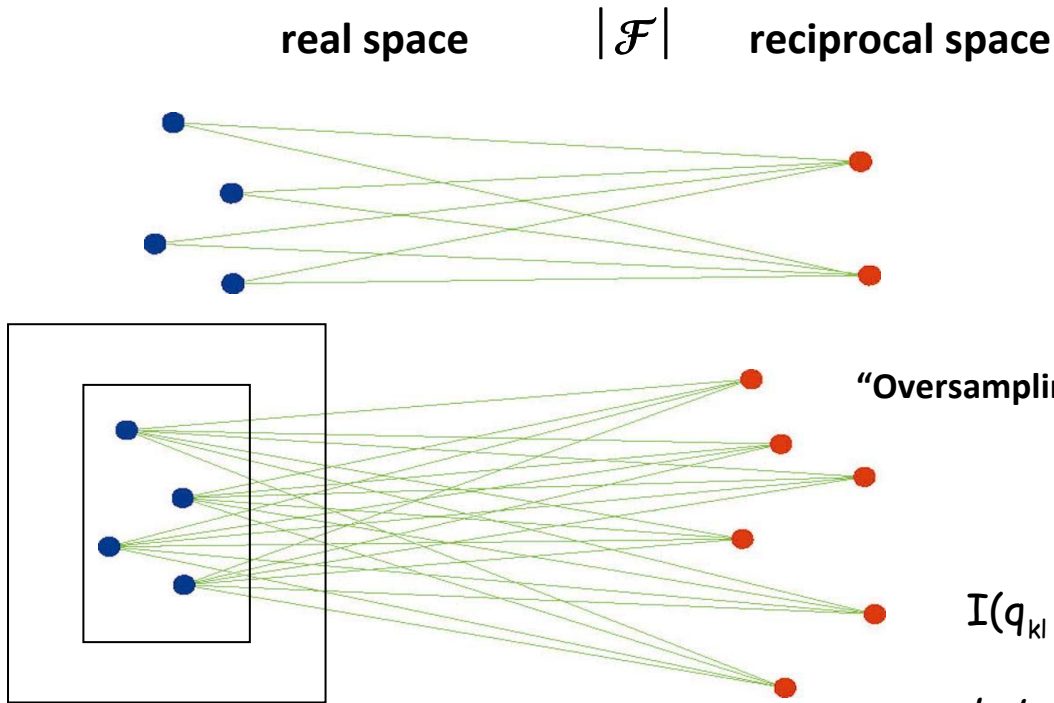
$$F(q) = F^*(-q)$$

J.Miao et al., *J. Opt. Soc. Am.* '98

J.Fienup, *Appl. Opt.* 21, 2758 (1982)

J.Miao, J. Kirz & D. Sayre, *Acta Cryst. D* 56, 1312 (2000)

„Oversampling“: a strategy to render the problem unique ?



**Information theory (Shannon) ?
really more information**

“Oversampling”

$$I(q_{kl}) = F(q_{kl}) F^*(q_{kl}) = \left| \sum_i^{N-1} \sum_j^{N-1} \rho_{ij} e^{-i(q_k x_i + q_l y_i)} \right|^2$$

$$h, k, i, j = 0 \dots N - 1$$

N^2 unknowns ρ_{ij} ,
but only $N^2/2$ independent equations

$$F(q) = F^*(-q)$$

$\rho(r) = 0$ out of support !

If support is half the size of
the field of view in both both dimensions:

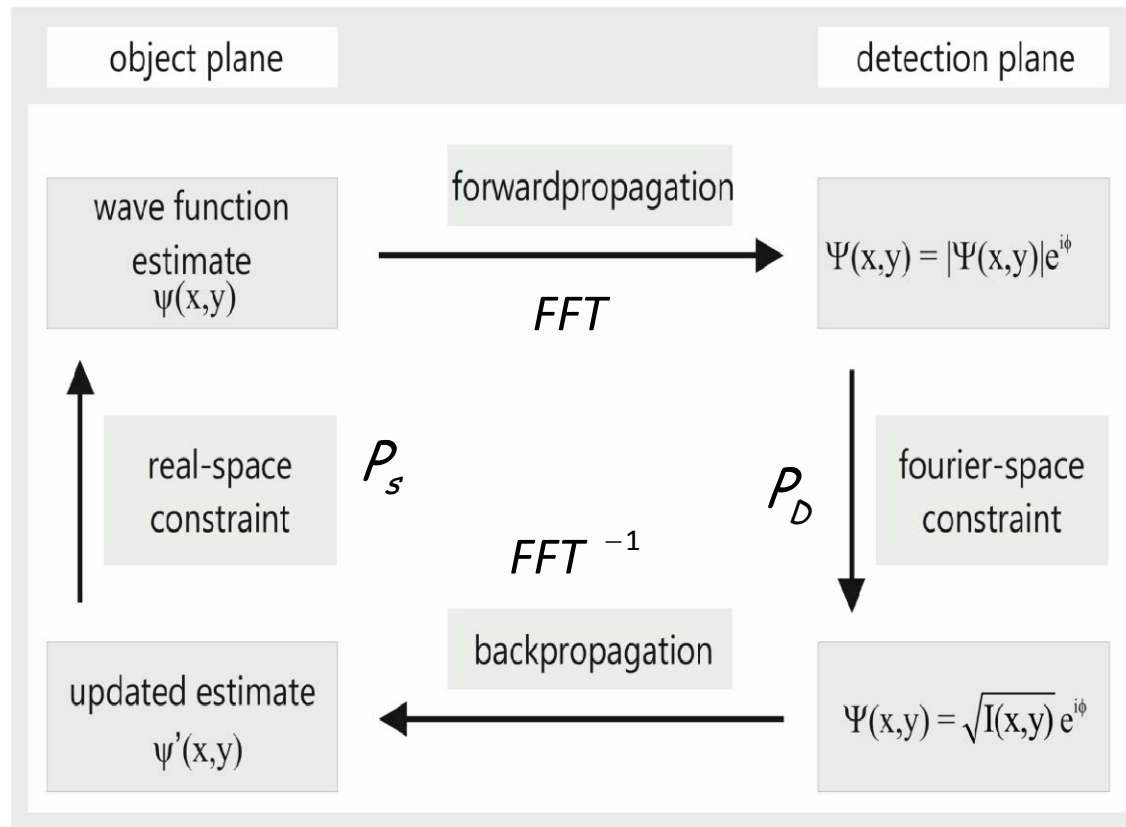
N^2 unknowns ρ_{ij} ,
4 N^2 equations
2 N^2 independent equations

J.Miao et al., *J. Opt. Soc. Am.* '98

J.Fienup, *Appl. Opt.* 21, 2758 (1982)

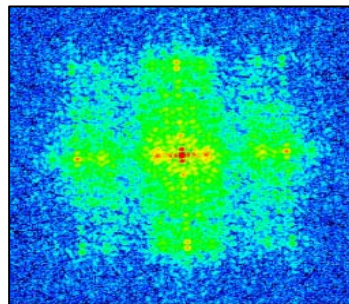
J.Miao, J. Kirz & D. Sayre, *Acta Cryst. D* 56, 1312 (2000)

how to solve the nonlinear set of equations: iterative algorithms



$$\rho_{i+1}(r) =$$

$$\begin{cases} \rho_i(r) & r \in S \cap \rho_i(r) > 0 \\ \rho_i(r) - \beta \rho_i(r) & r \notin S \cup \rho_i(r) \leq 0 \end{cases}$$



coherent scattering patte

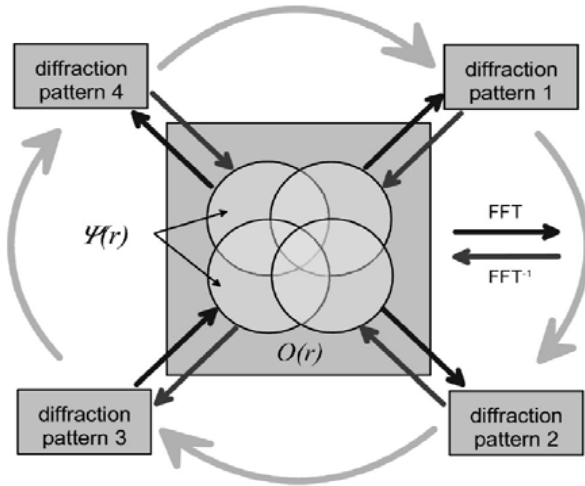


reconstructed image

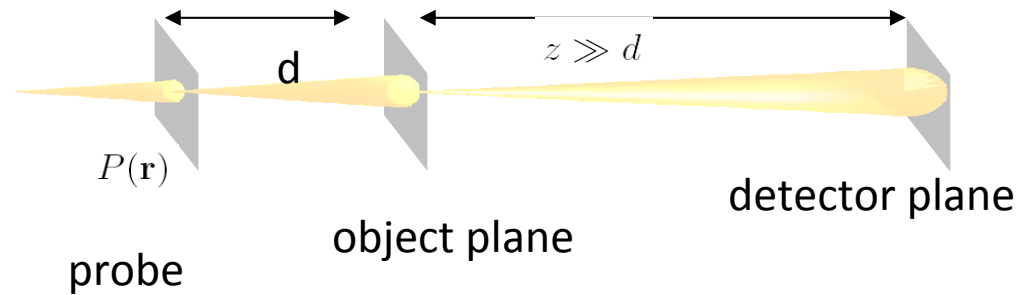
J. Miao et al., Nature **400**, 342 (1999)

Ptychography: using the overlap constraint

$$\Psi(\mathbf{r}) = P(\mathbf{r} + (0, 0, d)) \cdot O(\mathbf{r}) \quad |\mathcal{F}(\Psi)|^2 = |\mathcal{F}(P_d) \times \mathcal{F}(O)|^2$$



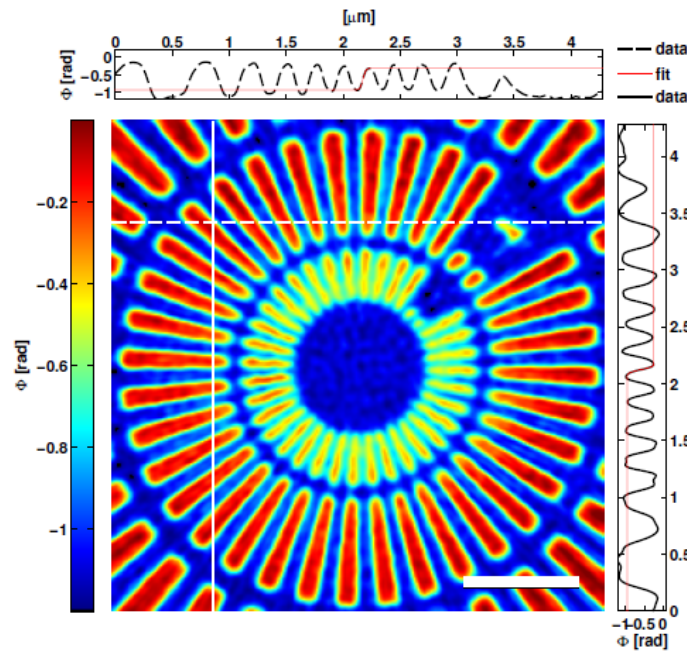
Rodenburg *et al.* PRL **98**, 034801 (2007)



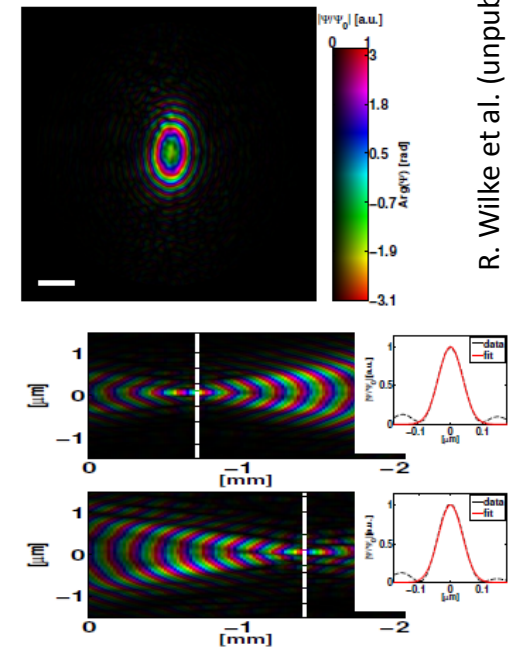
ptychographic reconstruction with x-rays:
Rodenburg *et al.* PRL (2007)

simultaneous reconstruction of illumination field:
Thibault *et al.* Science (2008)
Guizar-Sicairos, Fienup, Optics Express (2008)

application to biological cells:
Klaus Giewekemeyer *et al.*, PNAS (2010)



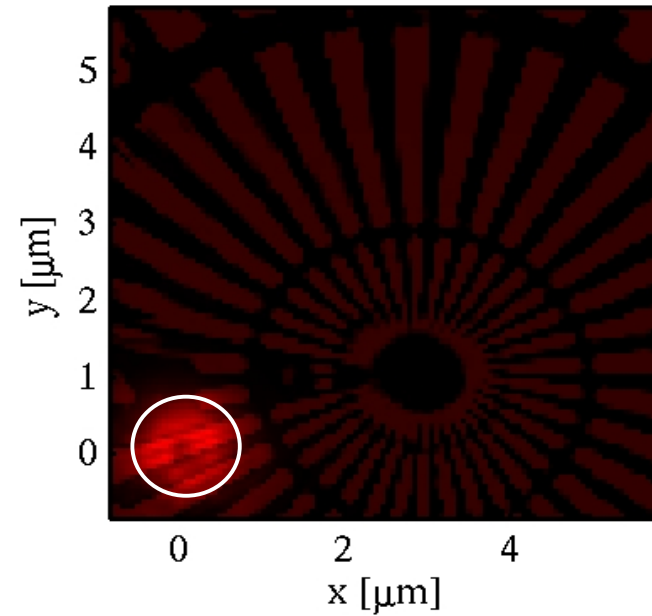
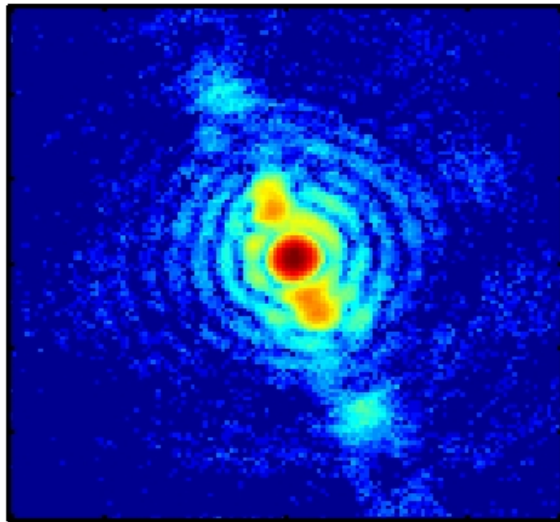
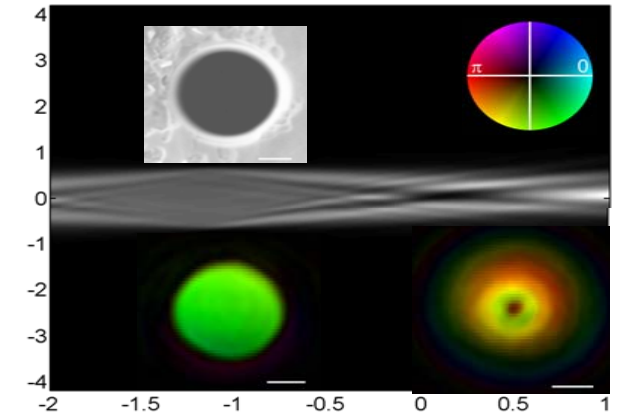
(a)



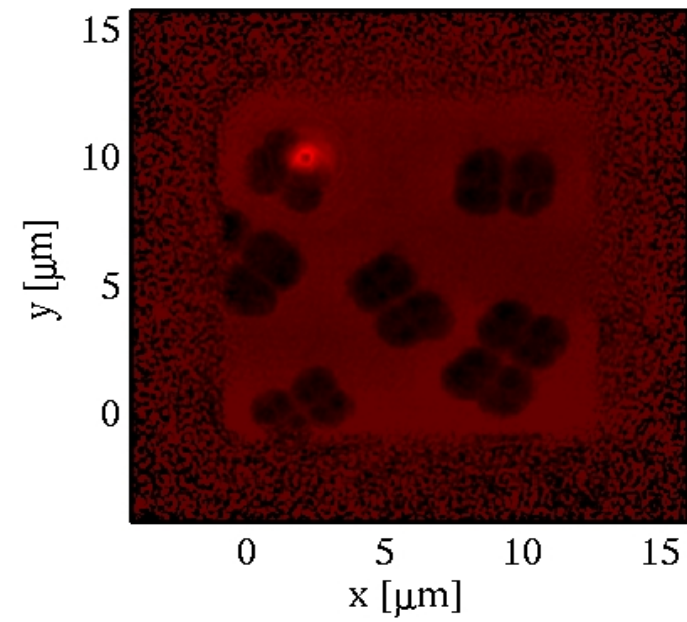
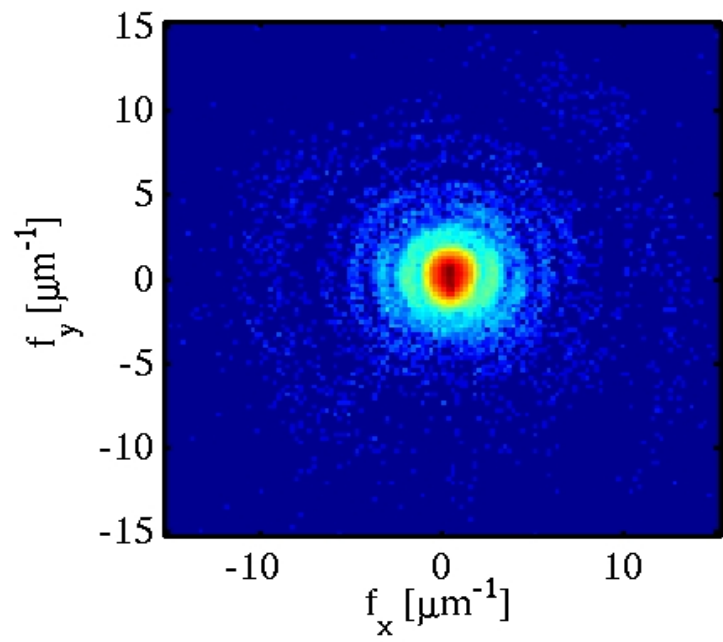
(b)

R. Wilke *et al.* (unpublished)

scanning and diffraction

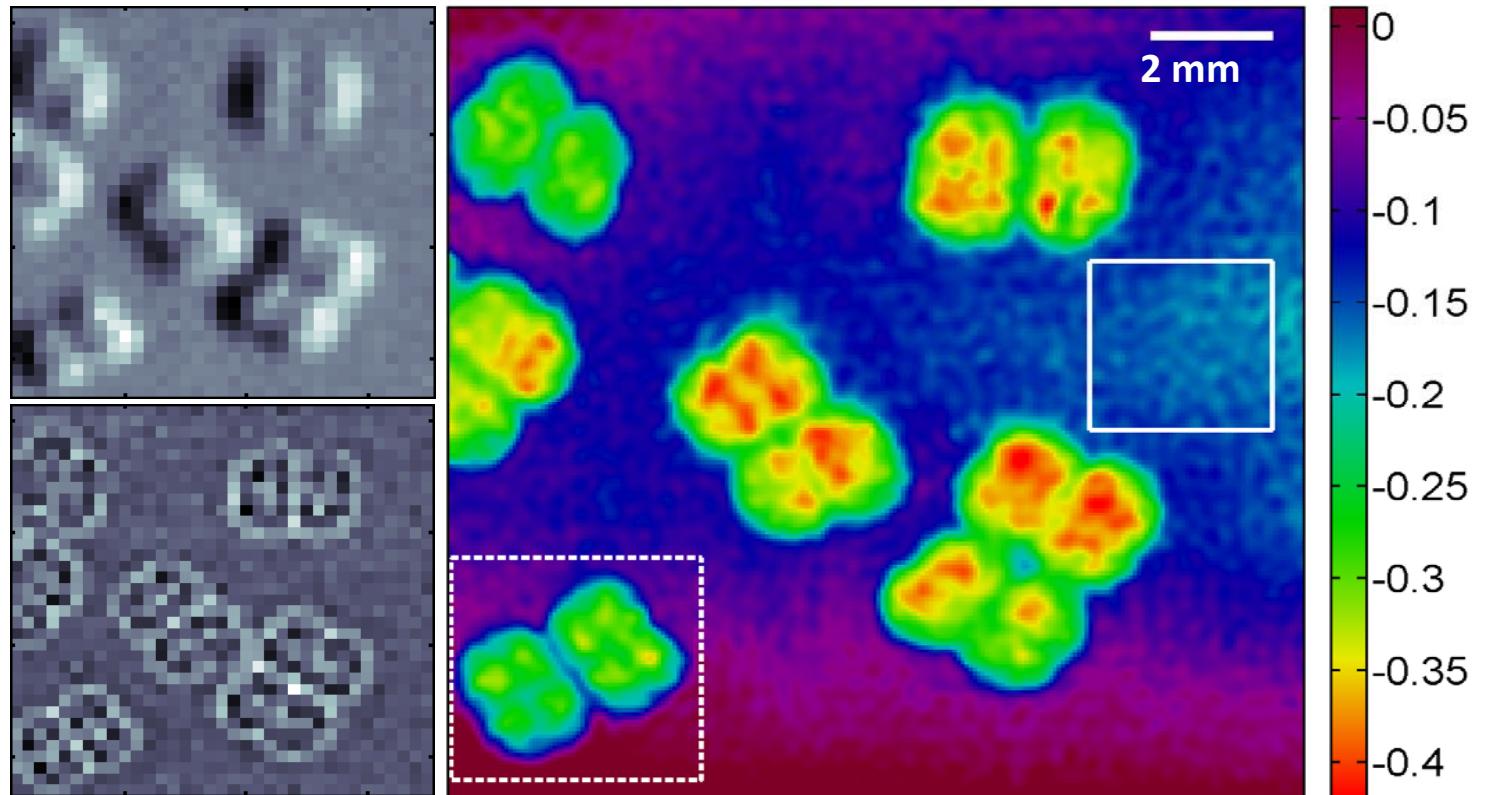


Maximum spacial frequency given by detector size and distance (Pilatus pixel det.)
15/ μm ($d = 67\text{nm}$), possible, but noise issues (Poissonian noise)!



DNA packing in nucleoids: *Deinococcus Radiodurans*

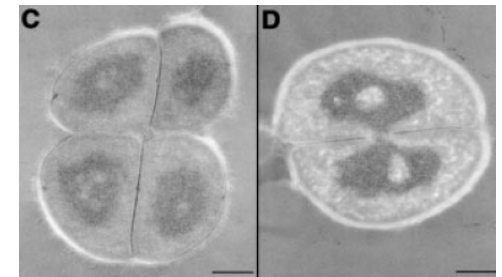
- Among most radiationresistant organisms on earth, can survive 15 kGy of ionizing radiation
- Very effective DNA repair mechanism, DNA packing debated



Left: Scanning X-ray Microscopy
DPC / dark field

Right: super-resolution by phasing the
coherent diffraction pattern

- Freeze-dried, unstained and unsliced cells
- Overall phase shift of single cell 0.25-0.3 rad (< 10% p), consistent with simulations
- 2500 iterations of SXDM algorithm, averaged over each 5th iterate, starting at 2000



TEM-slices, Os-stained chromatin
Levin-Zaidman, Science (2003)

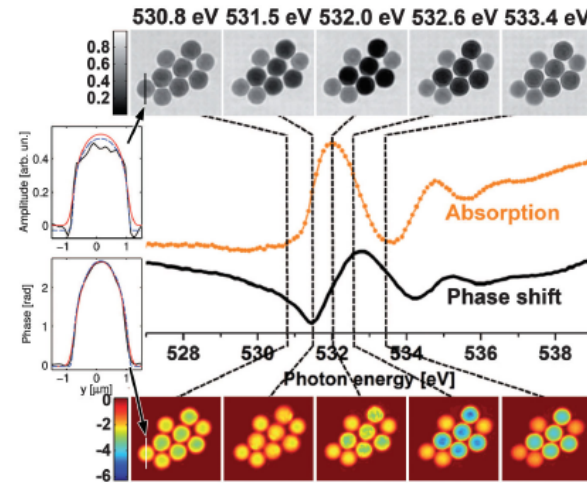


2x3 μ m size, tetrad morphology
4 identical copies of the genome

Chemical Contrast in Soft X-Ray Ptychography

Mike Beckers,^{1*} Tobias Senkbeil,¹ Thomas Gorniak,¹ Michael Reese,² Klaus Gieweker,³ Sebastian Glaser,⁴ Tim Salditt,³ and Axel Rosenhahn^{1,5,†}

Soft x-rays (water window):
Absorption and phase
Carbon K-edge
-> chemical contrast



6 FIG. 2 (color). Reconstructions of amplitude and unwrapped phase (in radians) of five ptychographic data sets recorded at different energies around the measured C = O absorption peak of PMMA. The sample, a mixture of five PMMA beads and four SiO₂ beads each 2 μm in size, shows absorption and phase shift

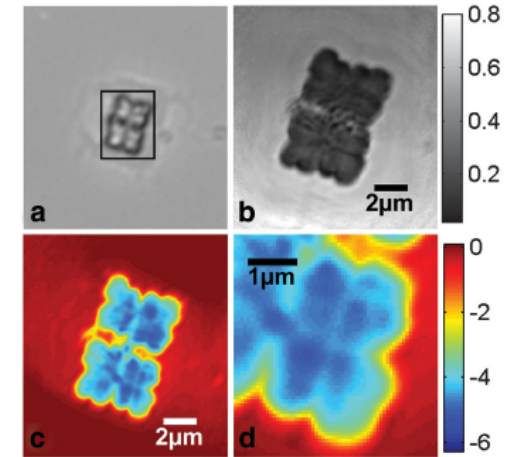
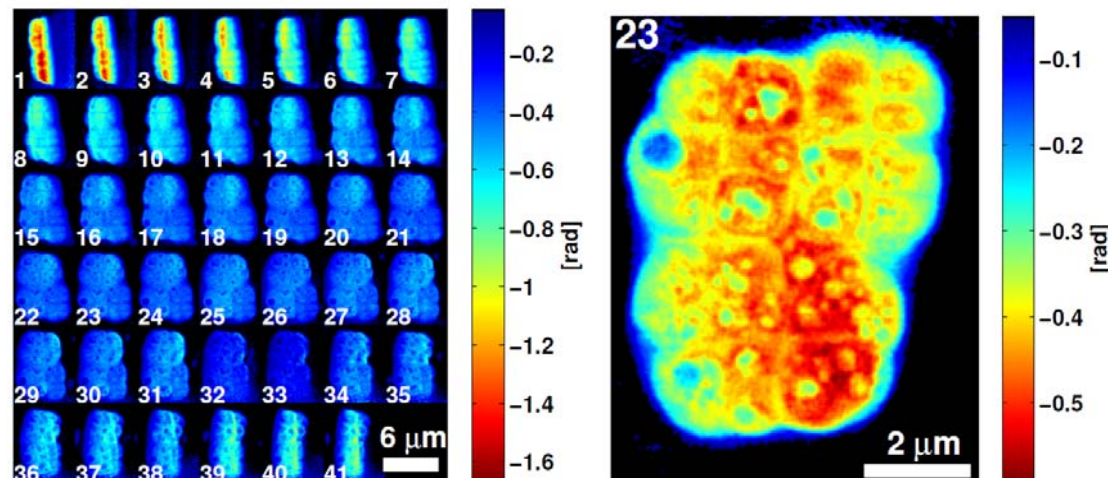
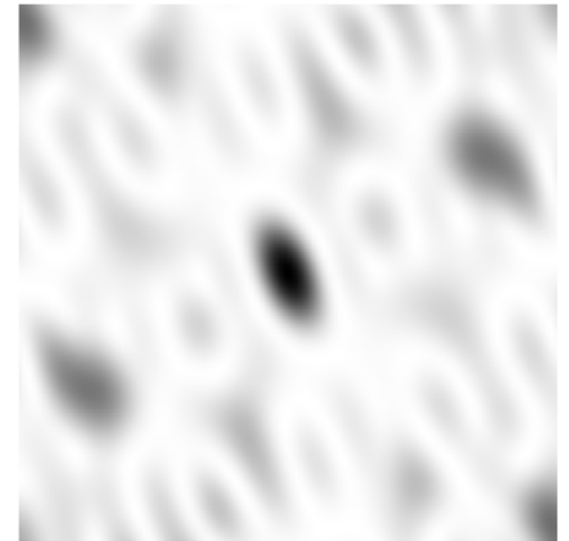
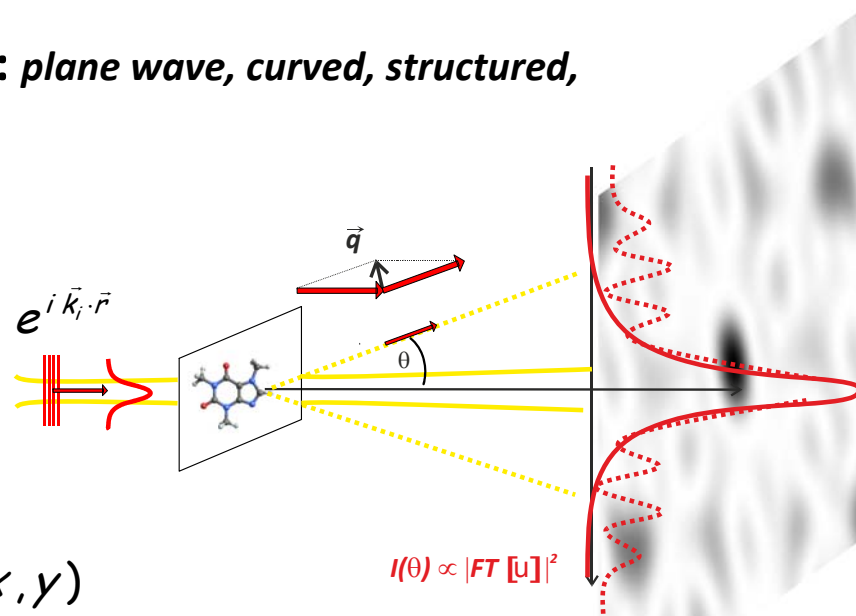


FIG. 3 (color). *D. radiodurans* cells. (a) Bright field microscopy image of a part of the specimen. Marked is the area of the ptychographic scan used for reconstruction. (b) Reconstructed amplitude of the cells. (c) Unwrapped phase shift of the cells and (d) detailed view.

Hard x-rays :
Absorption negligible
large penetration and focal depth
-> tomography

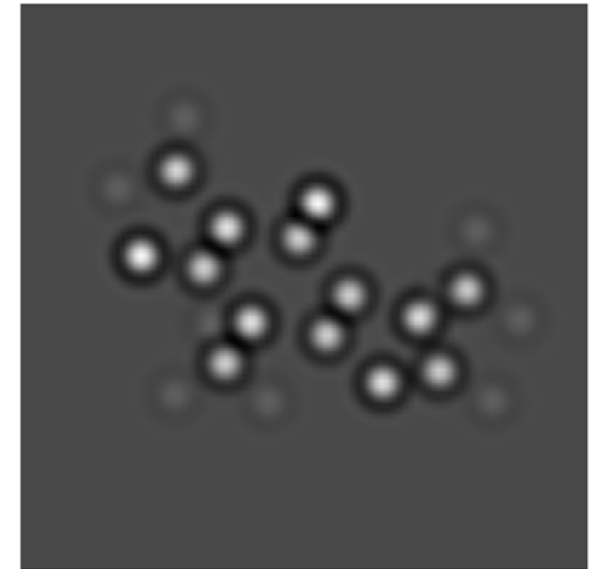
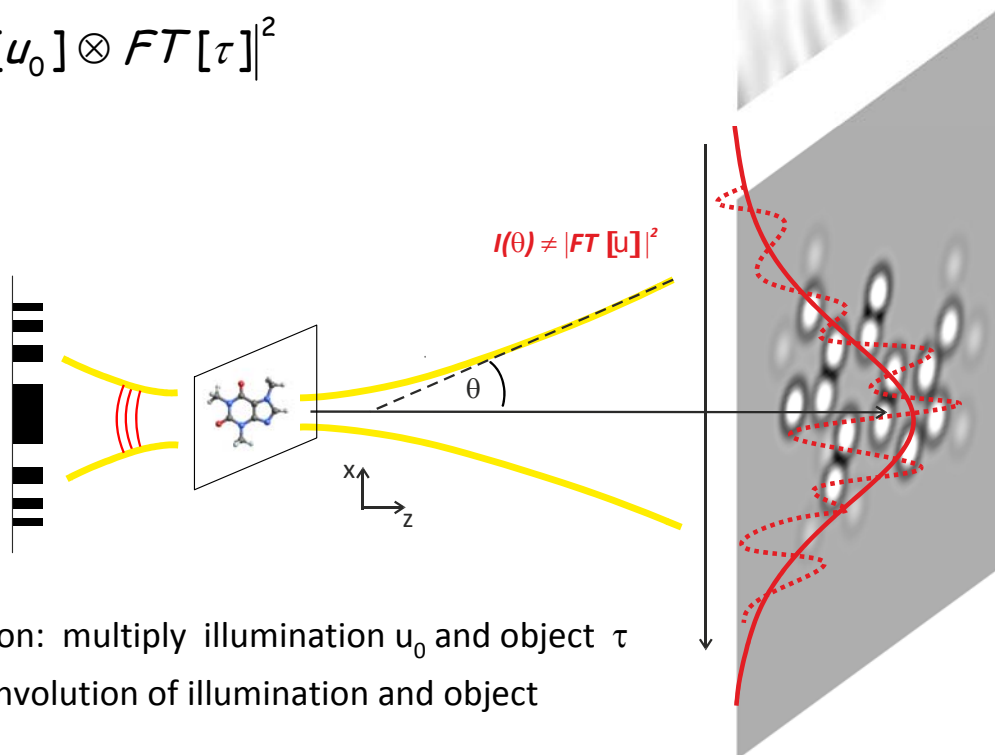


illumination function: *plane wave, curved, structured, unknown ?*



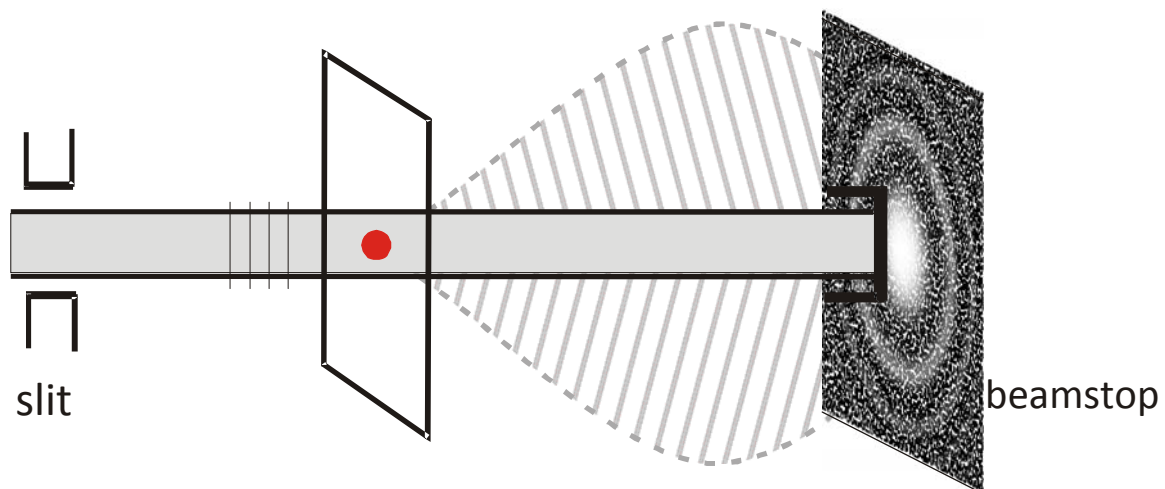
$$u(x, y) = u_0(x, y) \tau(x, y)$$

$$|FT[u]|^2 = |FT[u_0] \otimes FT[\tau]|^2$$

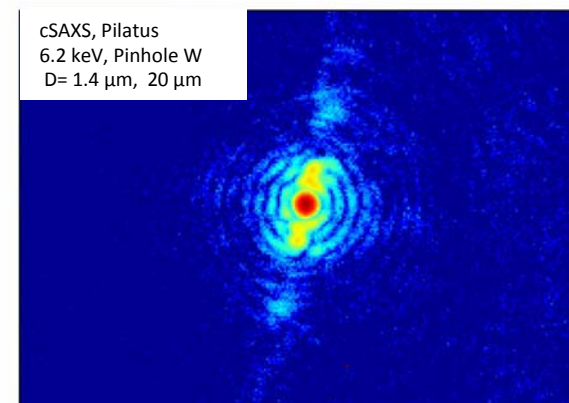


- projection approximation: multiply illumination u_0 and object τ
- measured intensity: convolution of illumination and object

Far-field and near-field diffraction patterns !

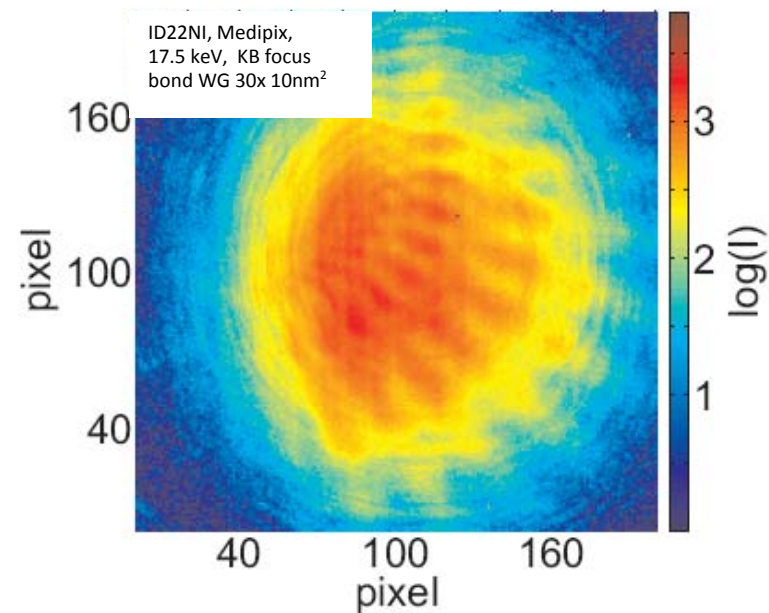
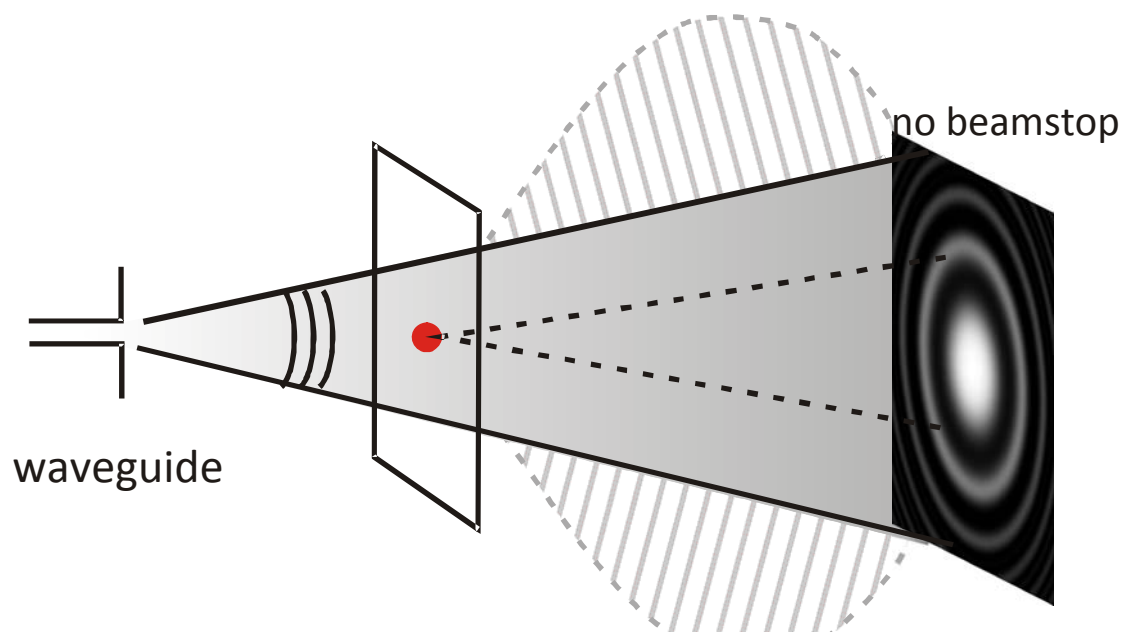


coherent farfield diffraction pattern

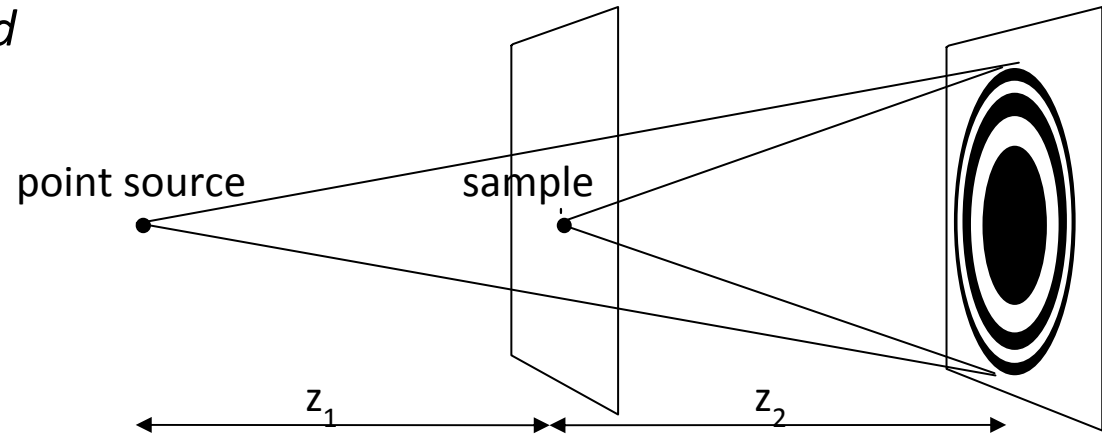


Missing low-q components

Fresnel diffraction pattern



Fresnel scaling theorem:
an equivalence between parallel and point source illumination

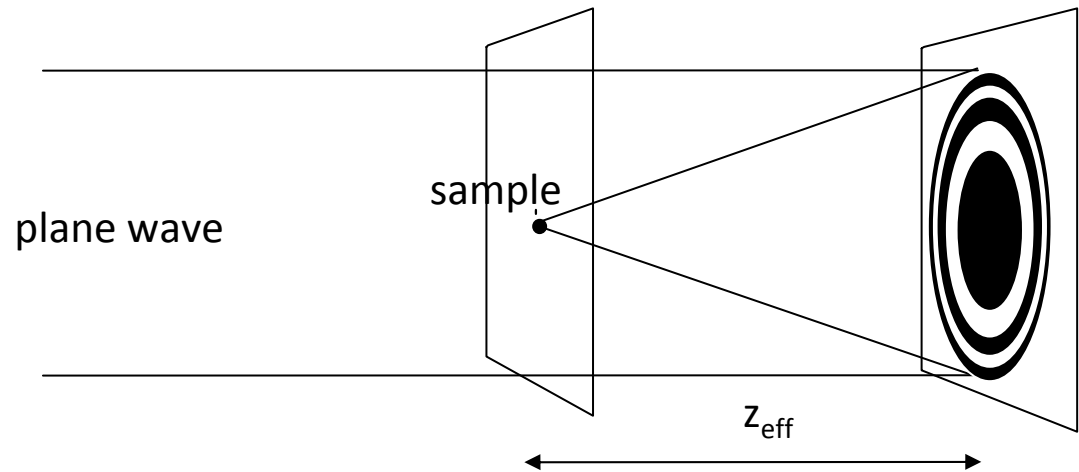


hologram recorded with the point source corresponds to a hologram recorded with a plane wave at an effective defocusing distance

$$z_{eff} = \frac{z_1 z_2}{z_1 + z_2}$$

magnified by

$$M = \frac{z_1 + z_2}{z_1}$$



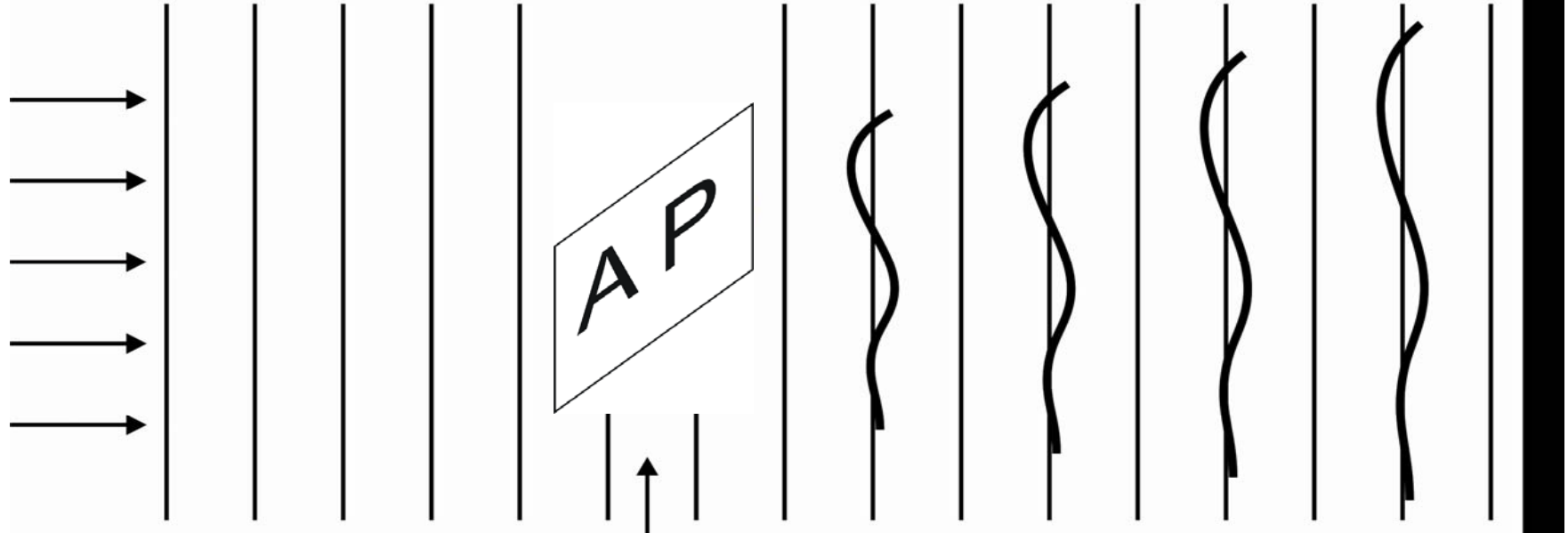
→ magnification allows for a spatial resolution below detector pixel size!

→ plane wave setup used for simulations and reconstruction

Imaging formation: Fresnel diffraction integrals


$$\psi(x', y', z) = \frac{1}{i\lambda} \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} \psi(x, y, 0) \frac{1}{r} \exp(ikr) \frac{1 + \cos(\vec{n} \cdot \vec{r})}{2} dx dy$$

$$\psi(x, y, 0) = \psi_0 \tau(x, y)$$



object with complex transmission function $\tau(x, y)$

$$\psi(z) = FT^{-1} \left[\exp[iz \sqrt{k^2 - k_x^2 - k_y^2}] FT[\psi(0)] \right]$$


 Absorption Phase

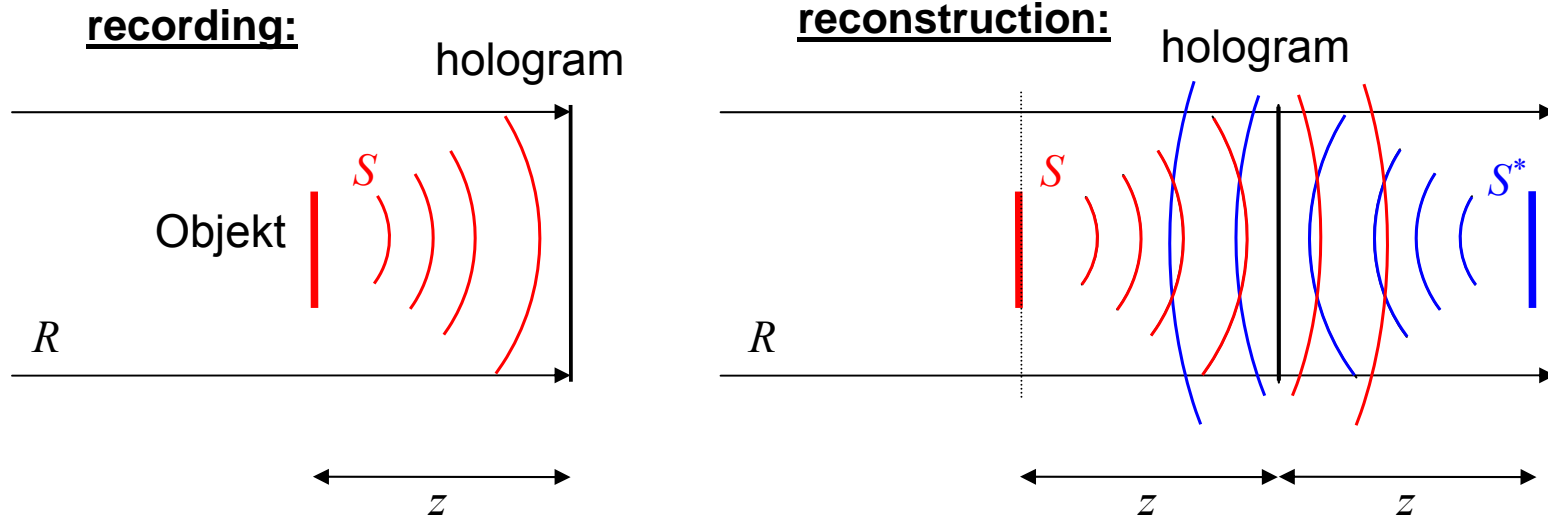


transformation from spherical to parallel beam,
 $z \rightarrow z_{\text{eff}}$, M magnified coordinate system

$$I(x, y) = |D_{z_{\text{eff}}}[\psi_{\text{in}}\chi(x, y)]|^2 \simeq |\psi_{\text{in}}D_{z_{\text{eff}}}[\chi(x, y)]|^2$$

normalisation of the measured
 intensity I by empty beam

$$\begin{aligned} \bar{I}(x, y) &\simeq |\psi_{\text{in}}D_{z_{\text{eff}}}[\chi(x, y)]|^2 / |\psi_{\text{in}}|^2 \\ &= |D_{z_{\text{eff}}}[\chi(x, y)]|^2. \end{aligned}$$



reference beam

$$\chi(x, y) = 1 + \tau(x, y)$$

signal

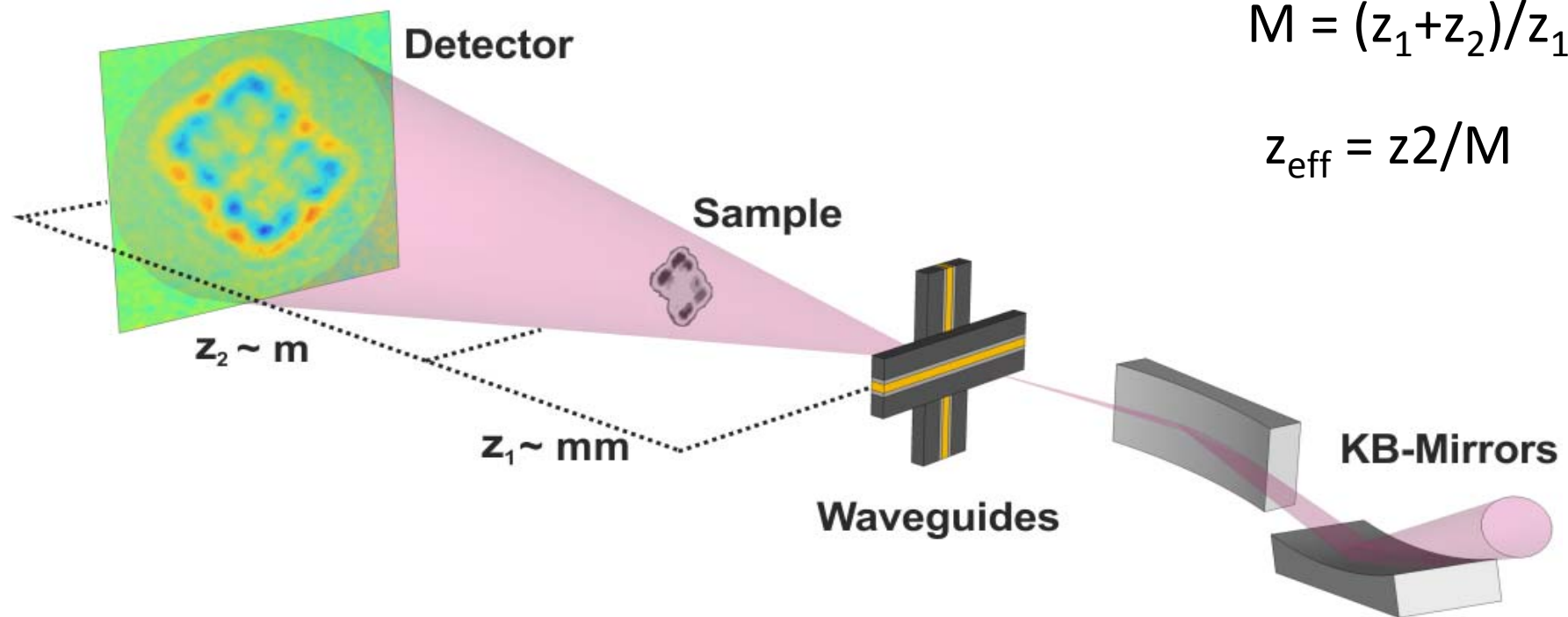
$$\tau \xrightarrow{D_z} \tilde{\tau} = D_z[\tau]$$

conjugated wave „twin image“

$$I(x, y) \propto |1 + \tilde{\tau}|^2 = 1 + \tilde{\tau} + \tilde{\tau}^* + |\tilde{\tau}|^2$$

$$\tau_{\text{recon}} = D_{-z}[1 + \tilde{\tau} + \tilde{\tau}^* + |\tilde{\tau}|^2] = 1 + \tau + \tau^* + D_{-z}[|\tilde{\tau}|^2]$$

Waveguide based propagation imaging schematic setup

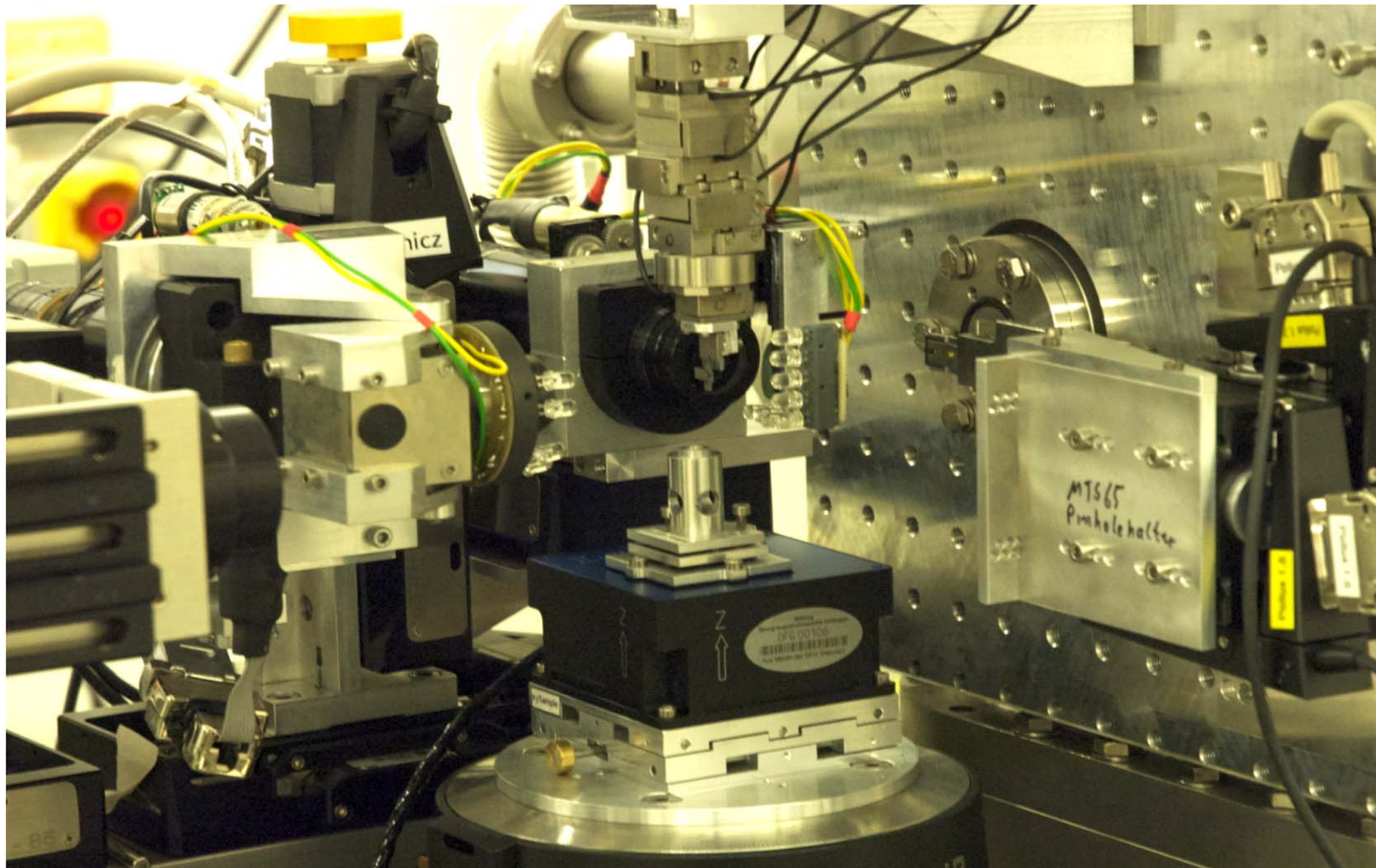


$$M = (z_1 + z_2) / z_1$$

$$z_{\text{eff}} = z_2 / M$$

1. Homogeneous signal level in detection plane
2. High dose efficiency
3. Less scanning overhead for tomography (full field)

Waveguide based propagation imaging setup – P10 at PETRA III



KB mirrors

mirror –precision polishing and metrology

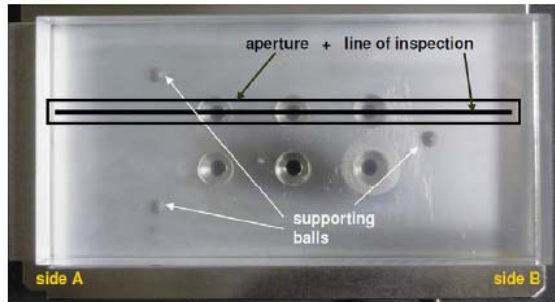


Fig. 3. Hard X-ray focusing mirror for the holography end-station of beamline P10 at PETRA-III at the alignment set with three steel balls. The 10 mm thick substrate was finished on a 10 mm × 5 mm long aperture section by EEM-finishing technology.

Table 1
Shape parameter of an elliptical cylinder mirror, for hard X-ray focussing at PETRA-III, as measured using BESSY-NOM and a Micromap Promap interference microscope (using magnifications 2.5 ×, 20 × and 50 ×).

Parameter of ellipse	Specification	Measurement results
Source distance r (mm)	85 500	85 500
Focus distance r (mm)	200	200
Incidence angle θ (mrad)	4.0	4.0499
Mirror pole x_m (mm)	Not defined	42 648.2
Residual slope error		0.13 μ rad rms
Residual figure error	3 nm pv	1.0 nm rms/3.1 nm pv
Roughness	≤ 0.15 nm rms	$S_q = 0.135\text{--}0.164$ nm rms (2.5 ×) $= 0.107\text{--}0.122$ nm rms (20 ×) $= 0.101\text{--}0.122$ nm rms (50 ×) $S_a = 0.106\text{--}0.126$ nm rms (2.5 ×) $= 0.082\text{--}0.096$ nm rms (20 ×) $= 0.079\text{--}0.093$ nm rms (50 ×)

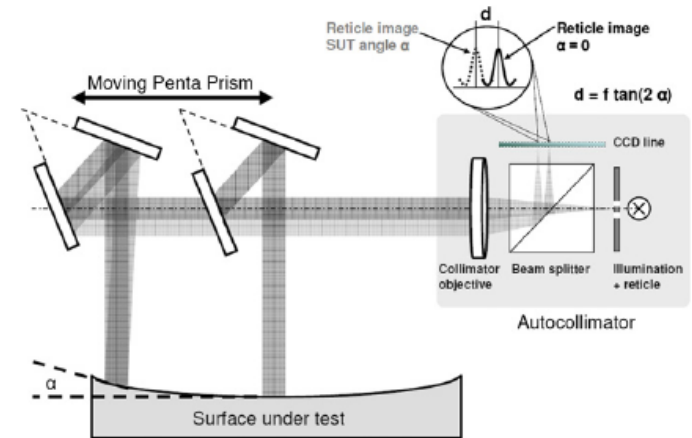


Fig. 1. Principal set-up of a mirror based moving penta-prism slope measuring profiler as realized for BESSY-NOM.

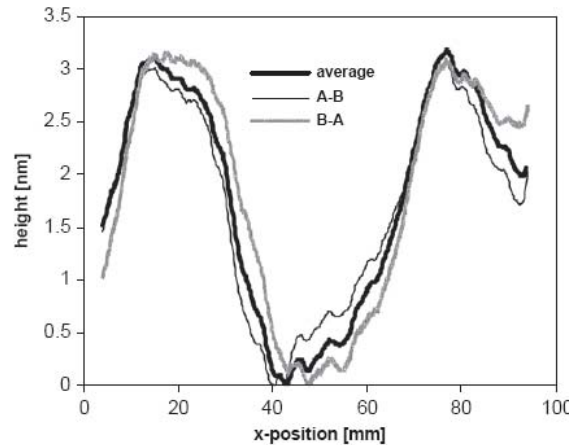
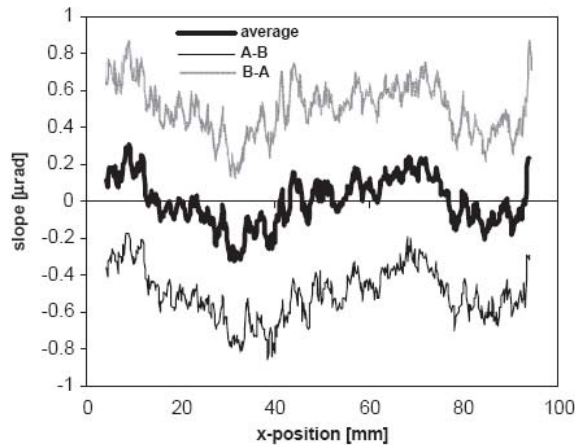
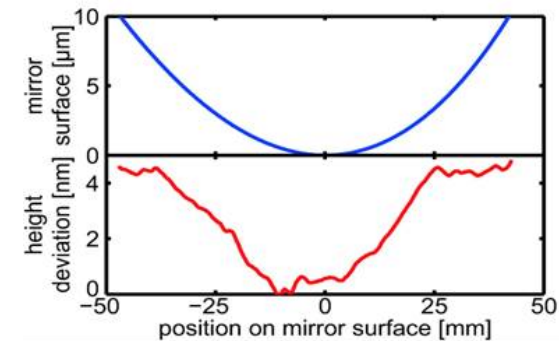
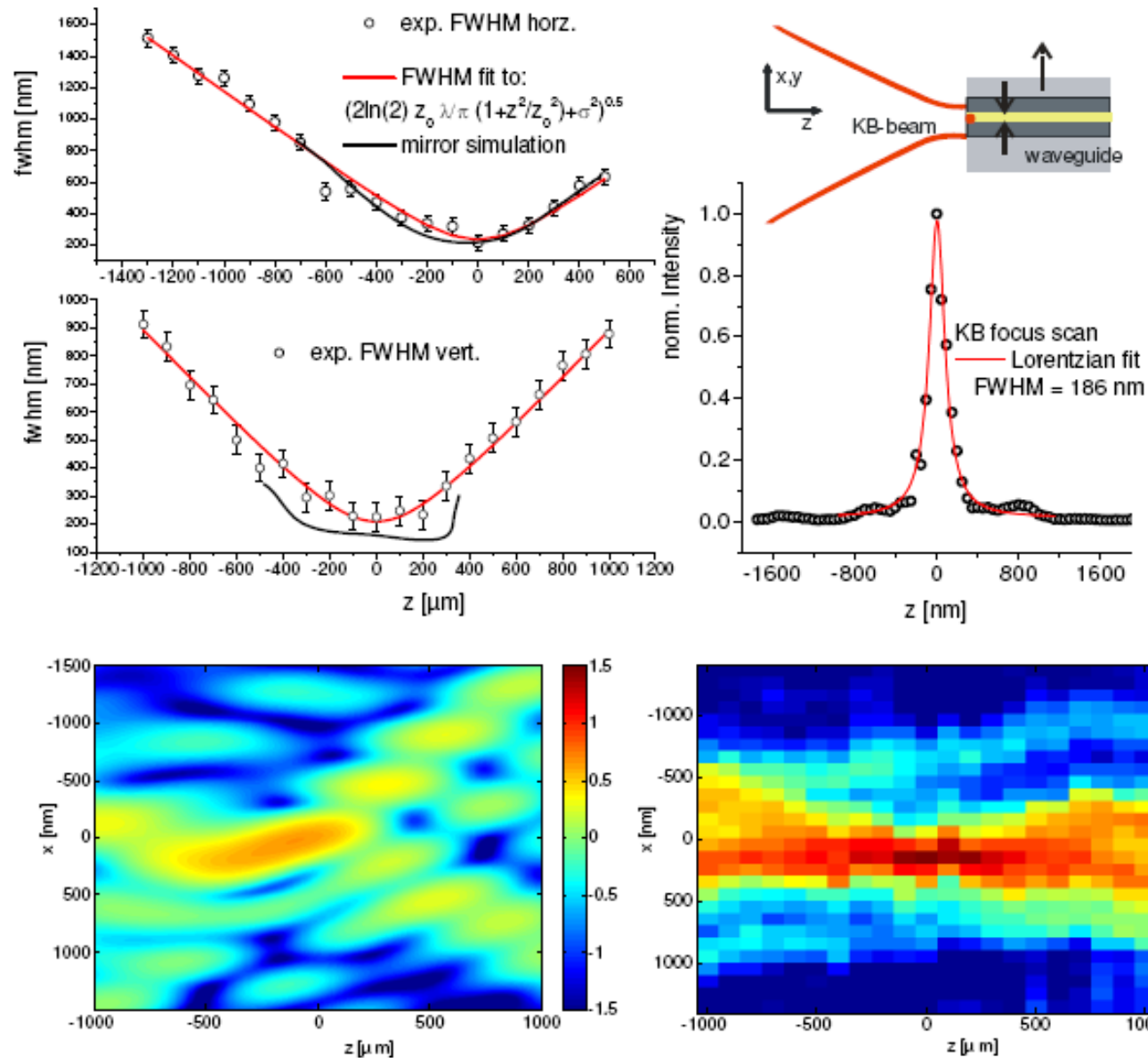


Fig. 4. Hard X-ray focusing mirror for the holography end-station of beamline P10 at PETRA-III. Left—profile of residual slope measured at two different alignment conditions from side A to B and after a 180° rotation from side B to A. For better visualization a shift of 0.2 μ rad was added to the profiles. Right—the corresponding profiles of residual height, gained by integration of the slope data.

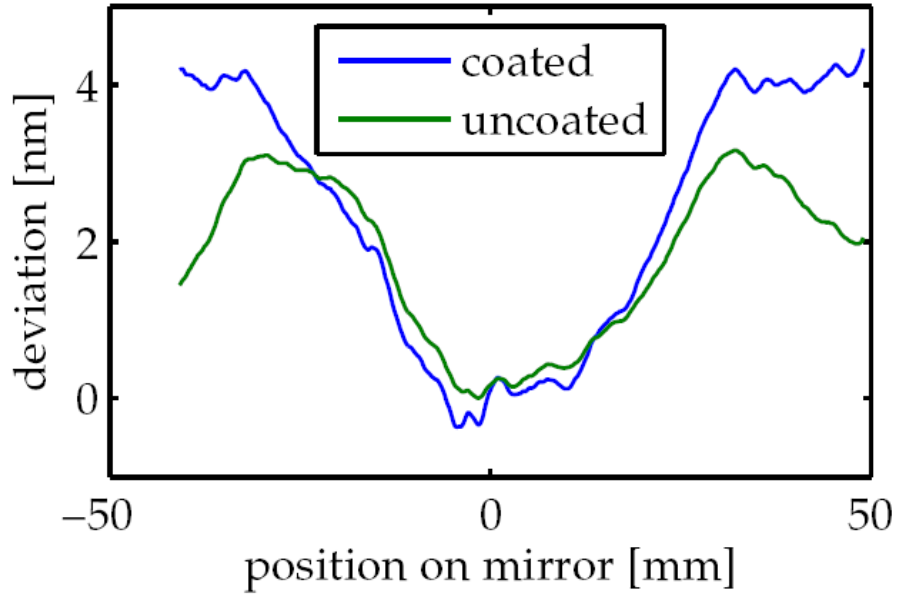


measured intensity distribution compared to simulation

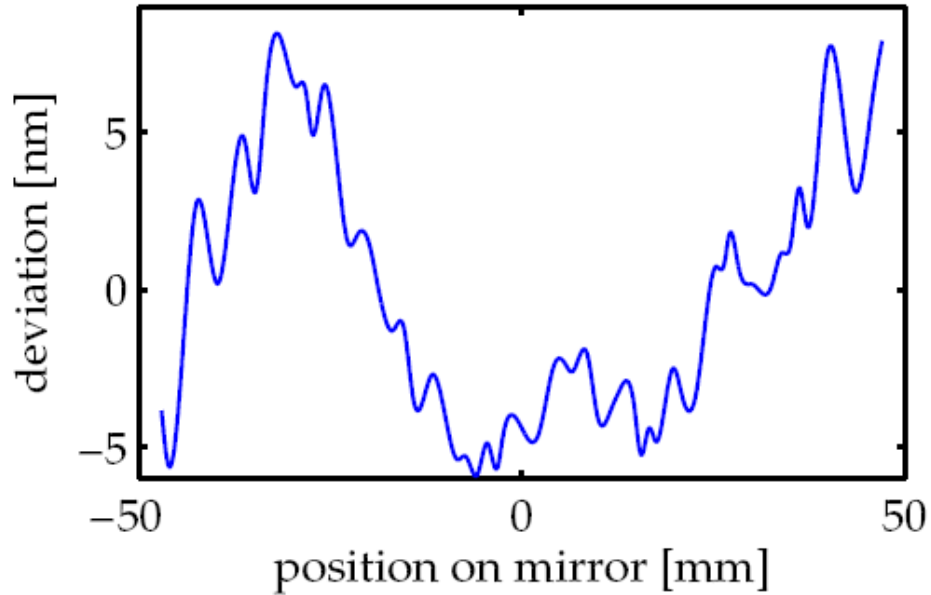


KB mirror system

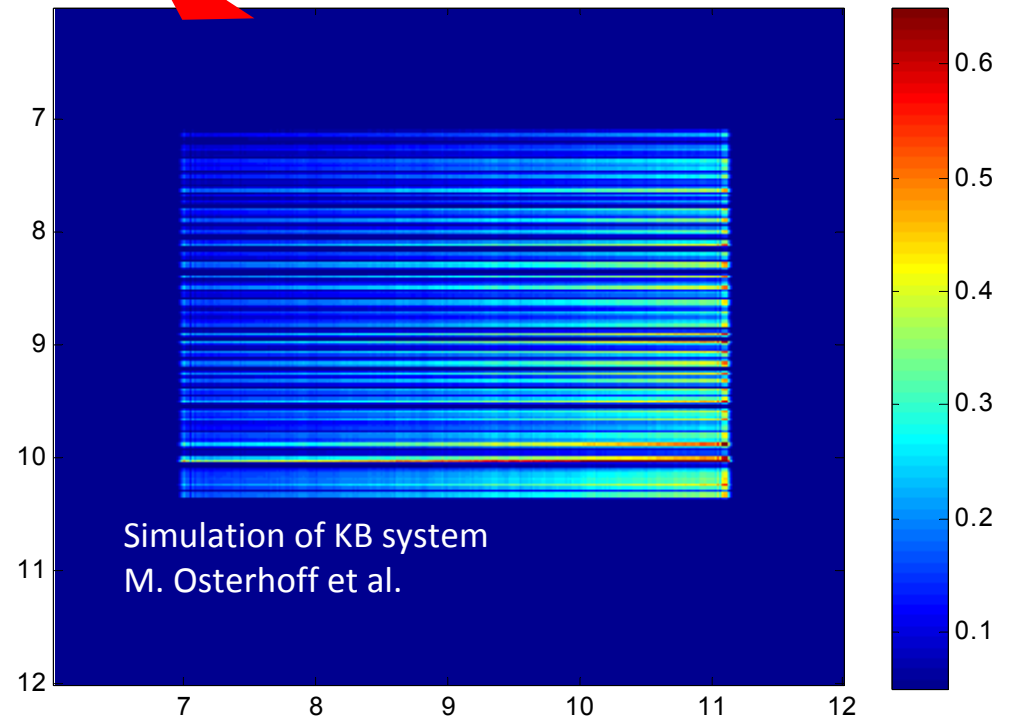
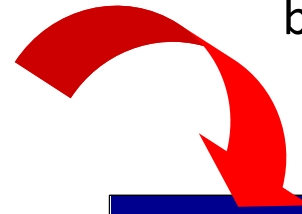
height profile JTEC mirror

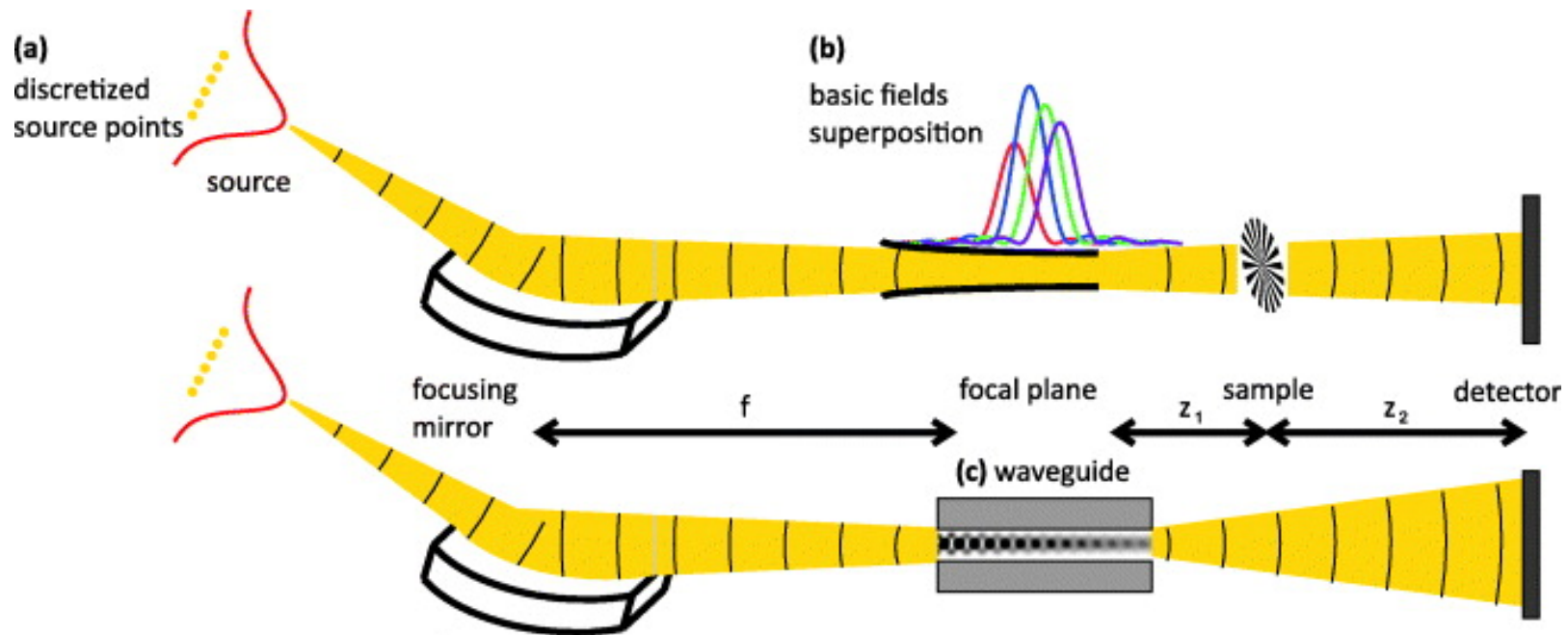


height profile WINLIGHT mirror



Simulated farfield pattern based on measured height data





stochastic superposition:

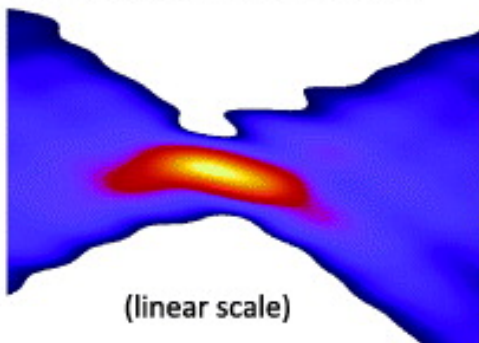
$$U(x) = \sum_n w_n c_n u_n(x)$$

Gaussian envelope
stochastic phase
pre-calculated fields

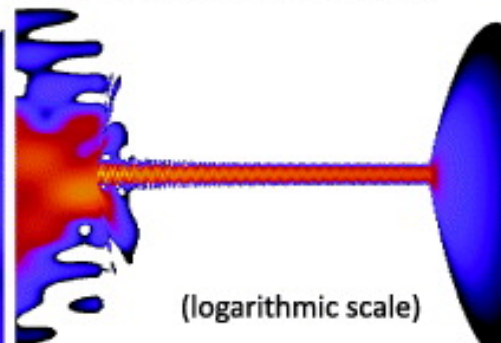
ensemble average of mutual intensity:

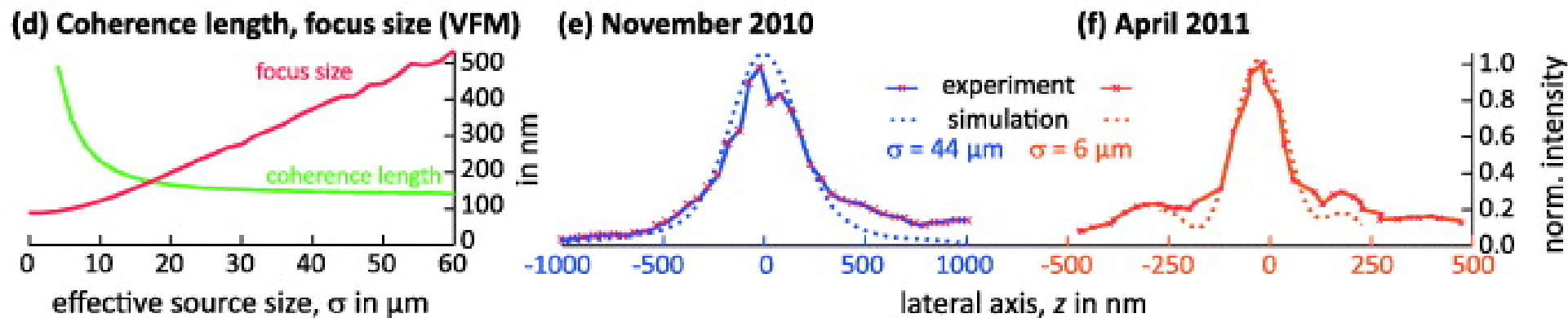
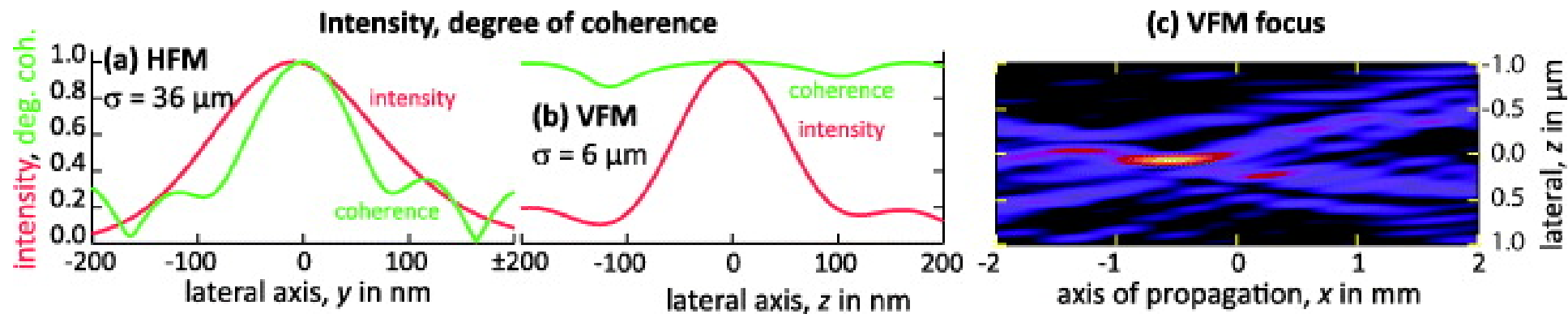
$$J_{1,2} = \langle U(x_1) U(x_2)^* \rangle$$

(d) 1 realization of mirror focus

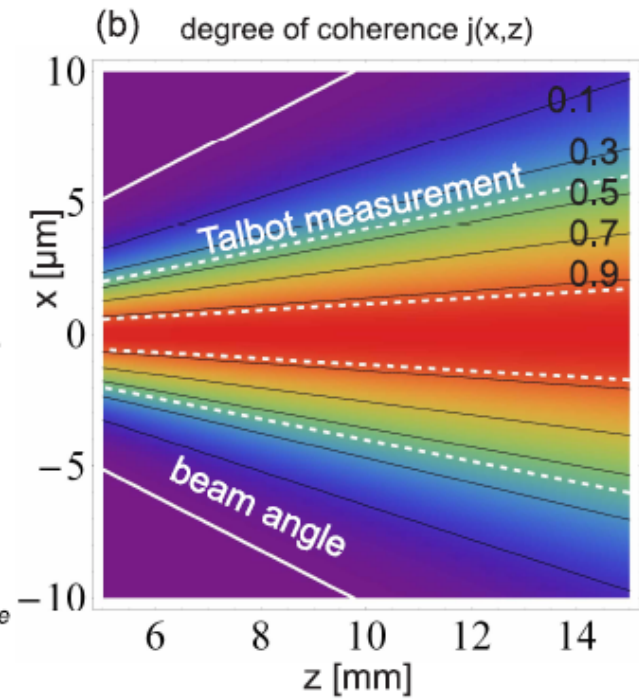
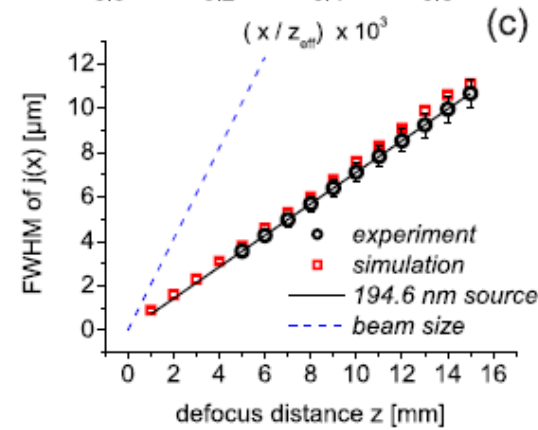
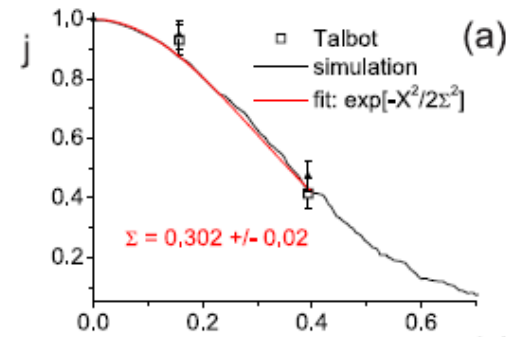
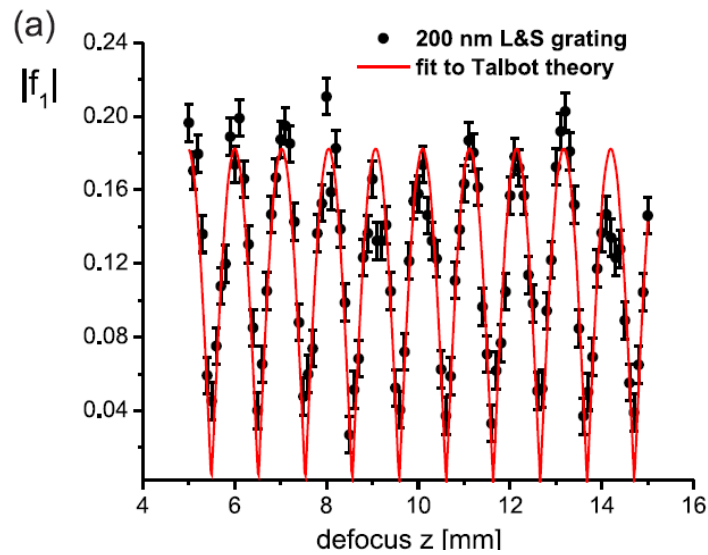
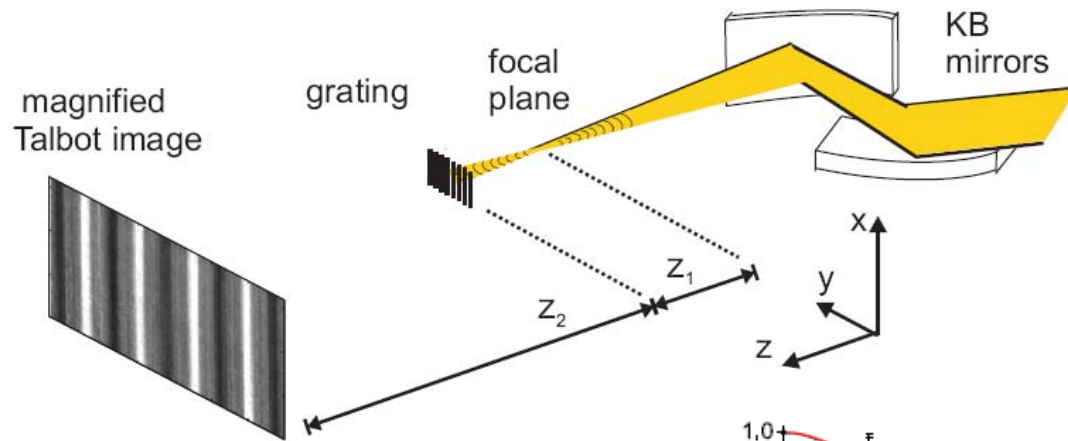


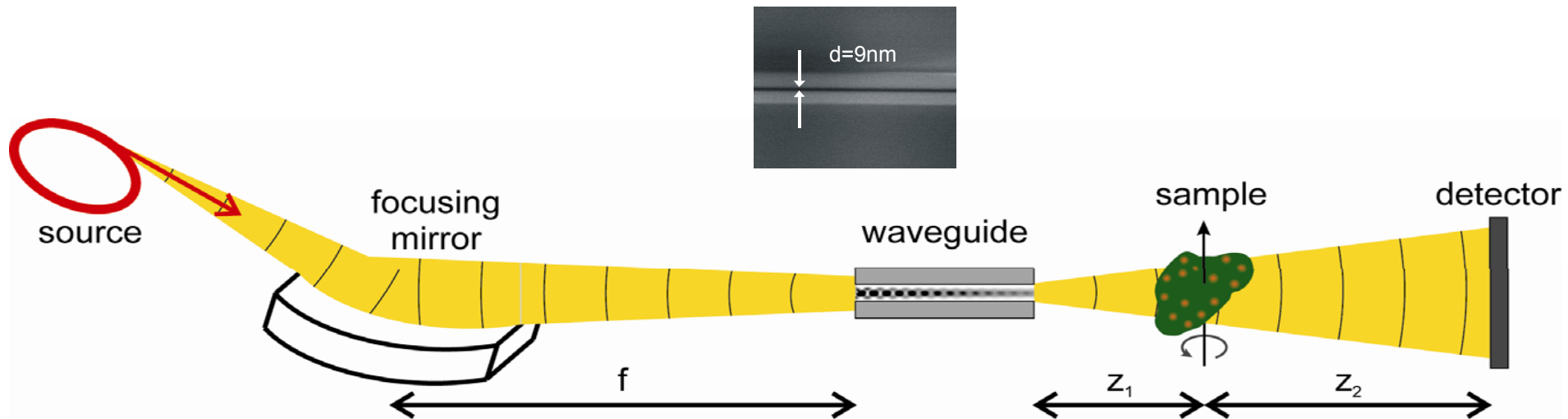
(e) 1 realization of WG filtering



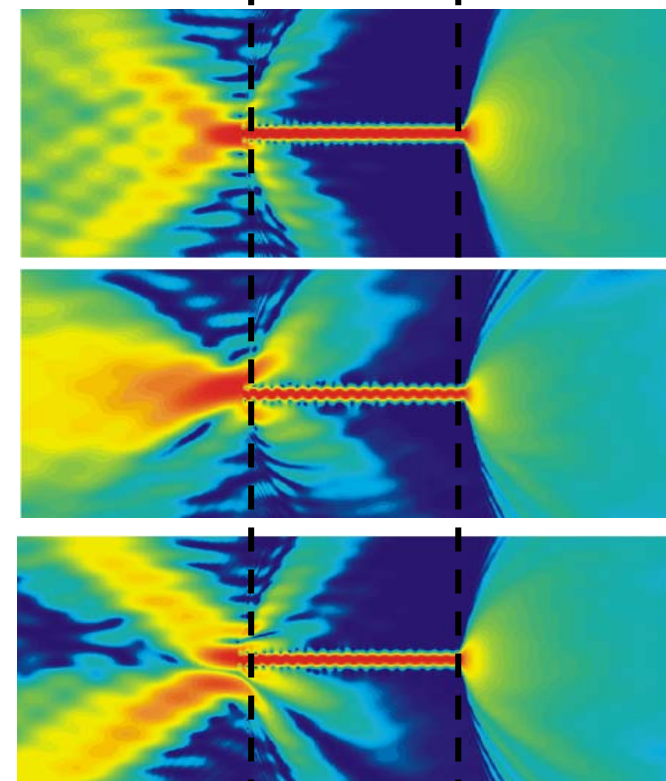
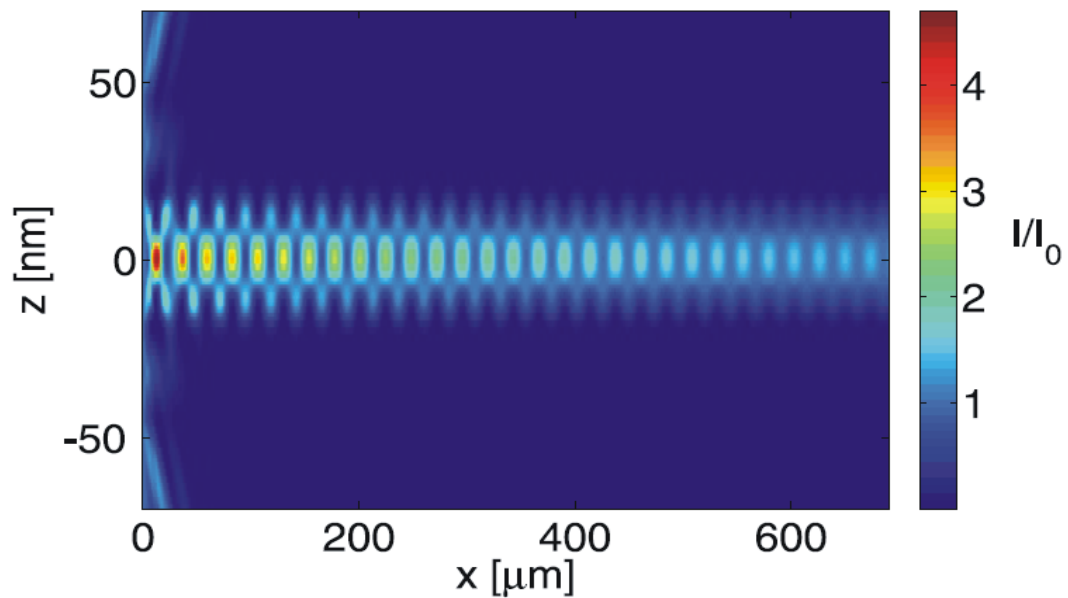


measured coherence function in good agreement with simulation

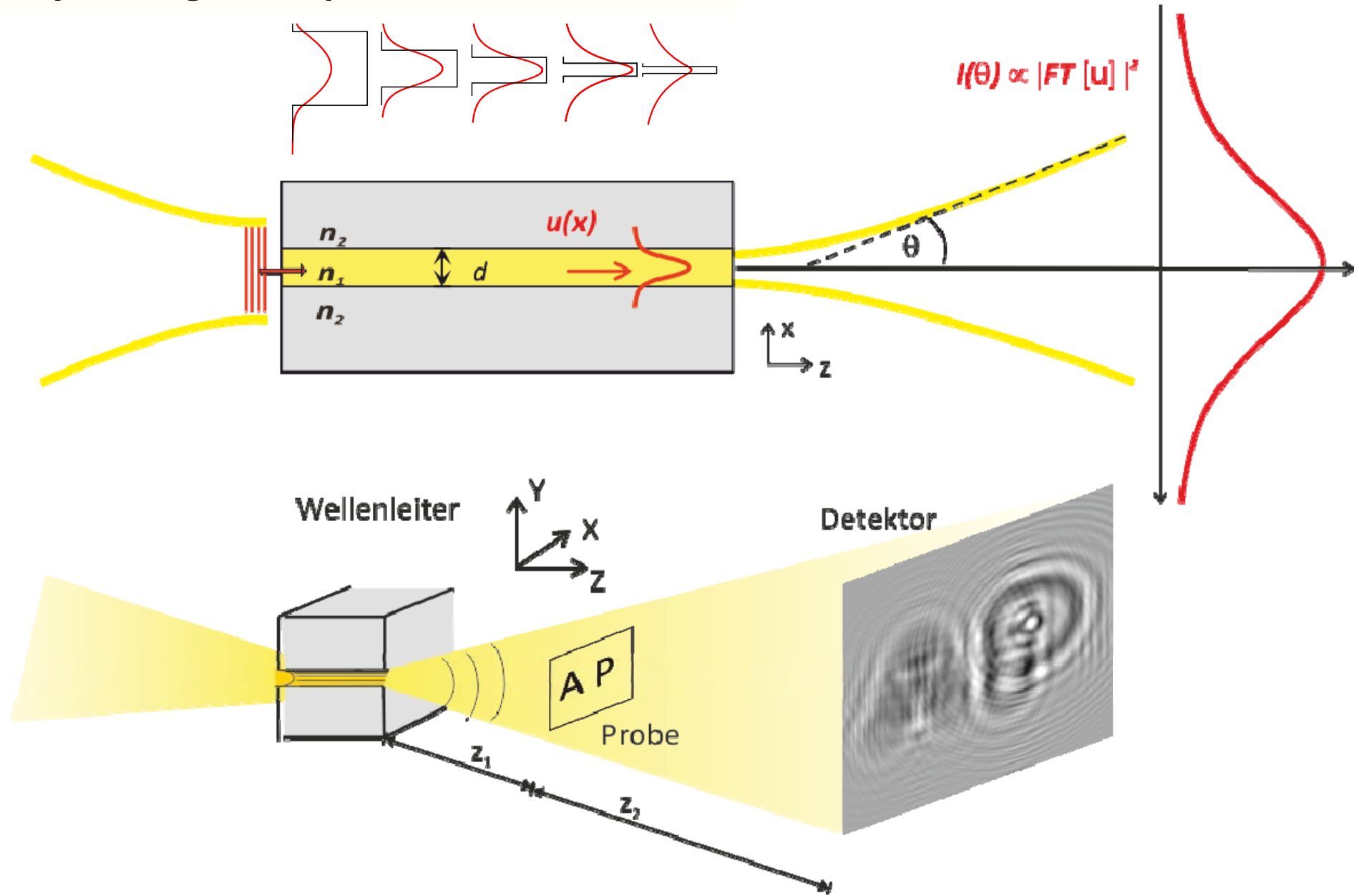


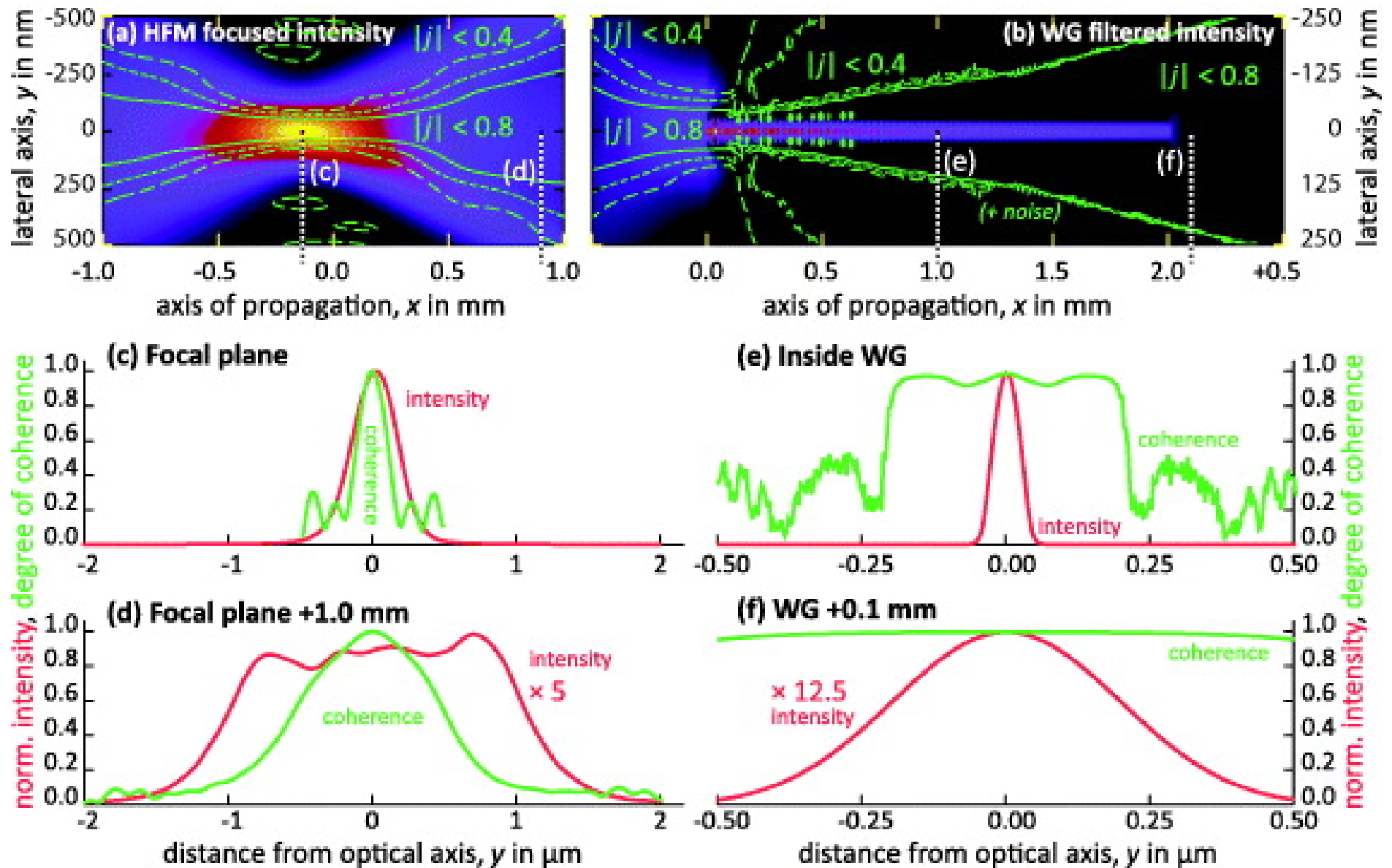


Coupling of mirrors beam into waveguide ...

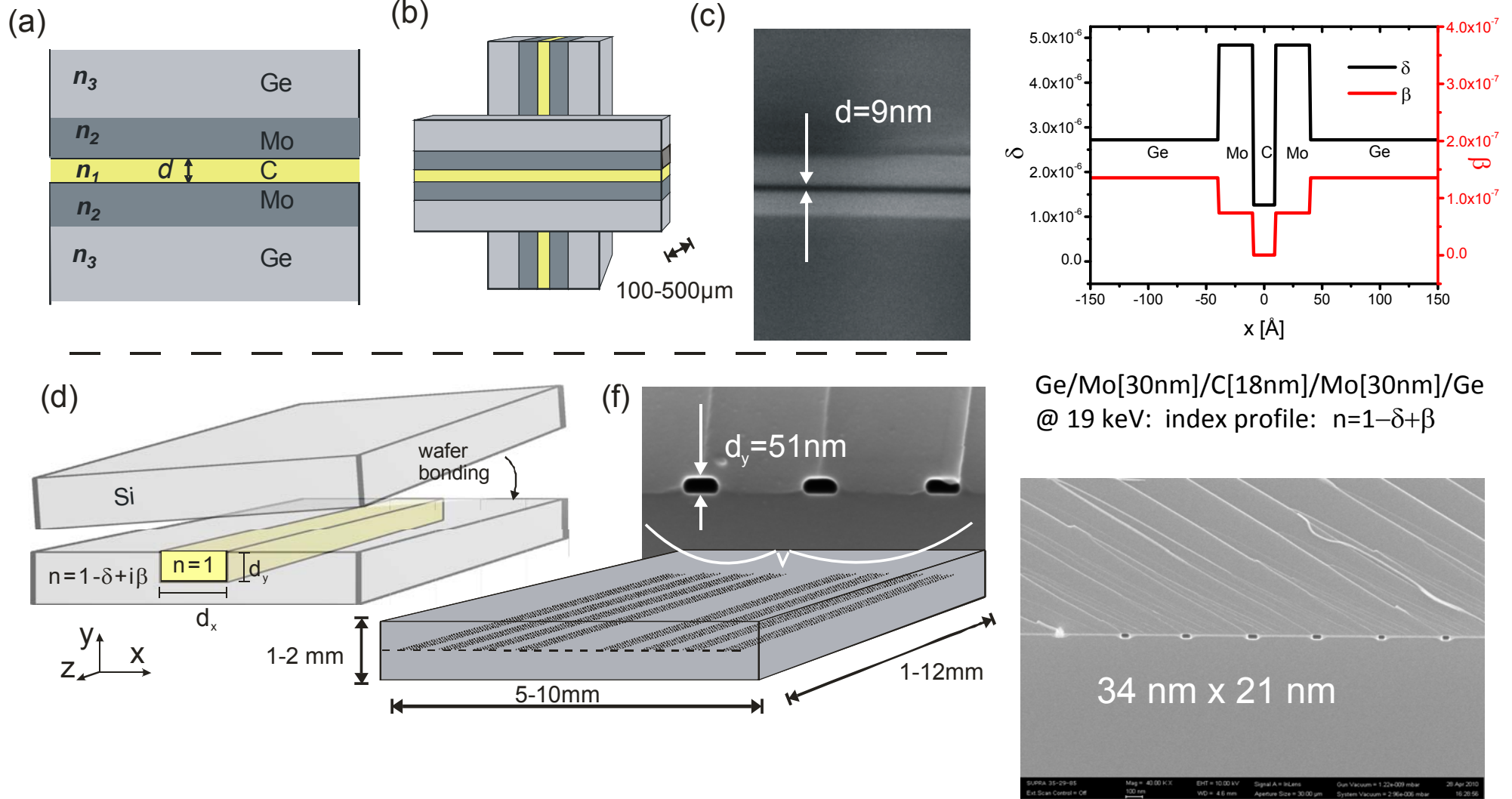


X-ray waveguide optics



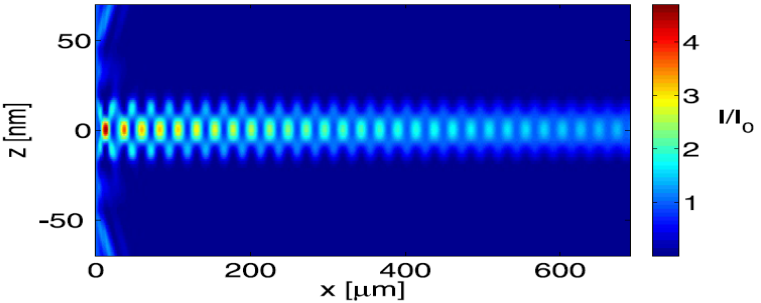
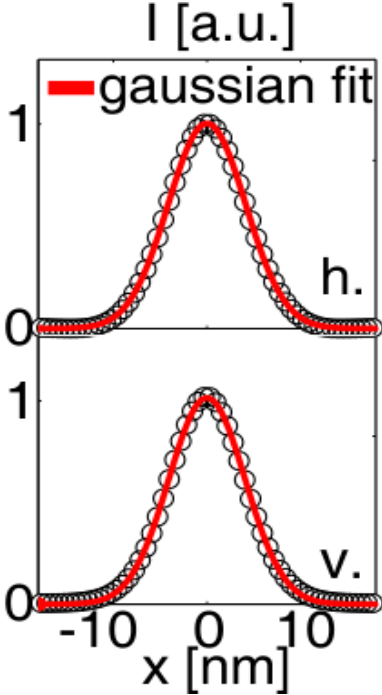
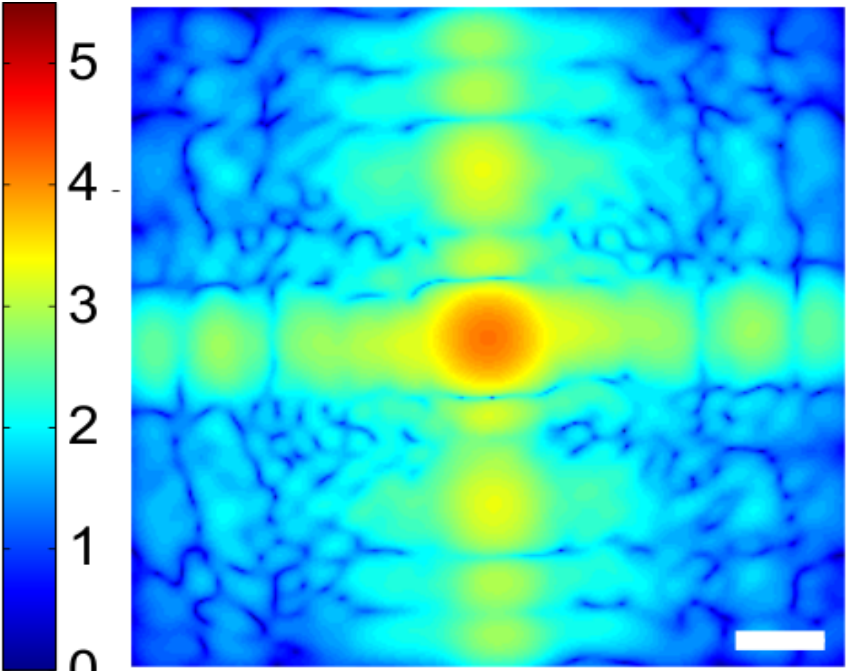
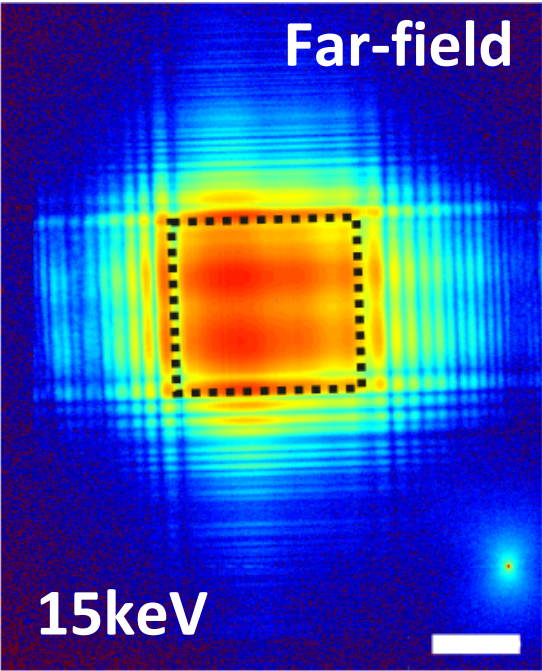


New generations of x-ray waveguides: (a) crossed high transmission planar waveguides (b) lithographic channels in Si sealed by wafer bonding



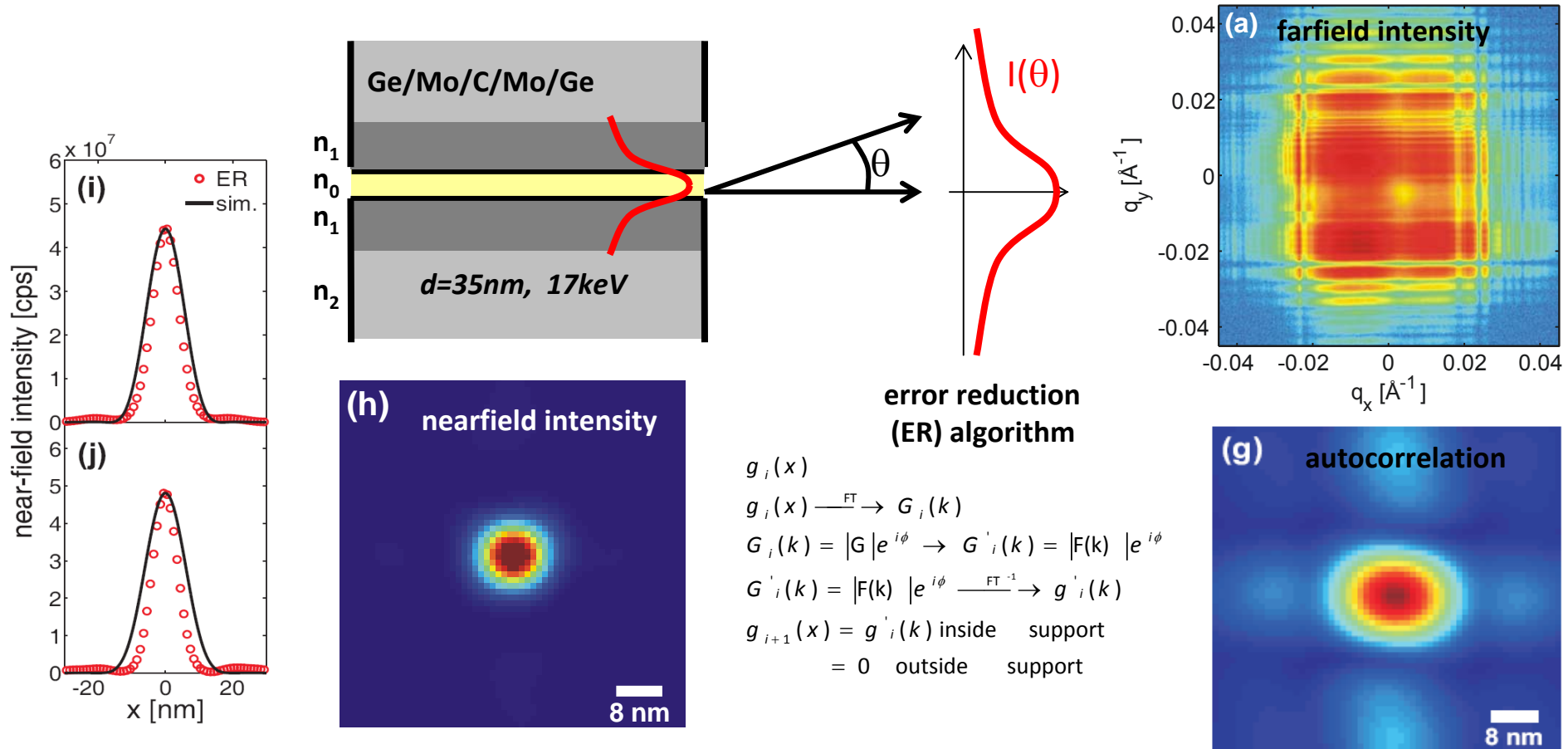
Waveguide based propagation imaging

Waveguide system



Effective focal plane
10 nm x 9.8 nm (FWHM)
1e7 cps

Calculation of near-field intensity distribution from farfield diffraction pattern: *sub 15 nm beam size in two dimensions*

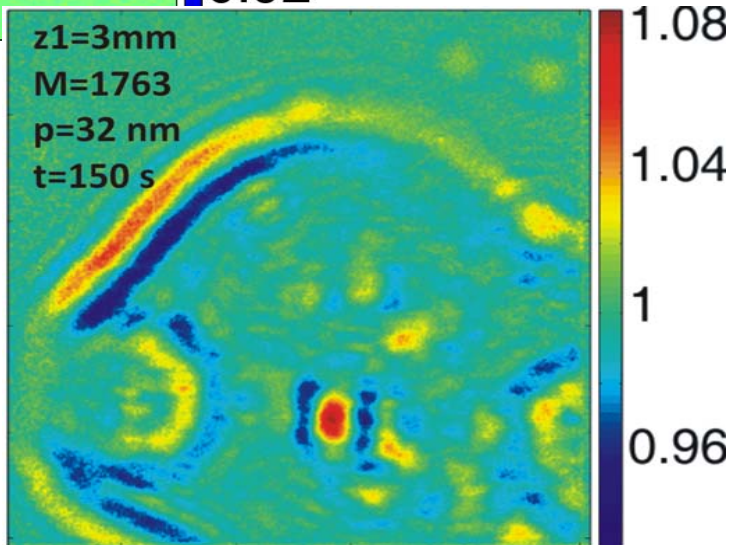
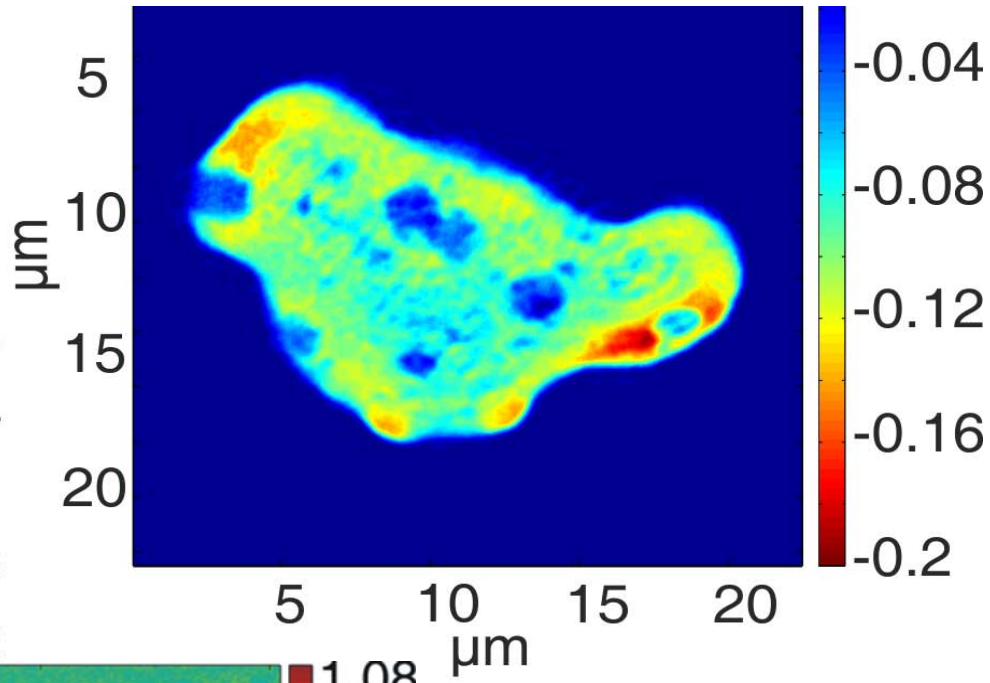
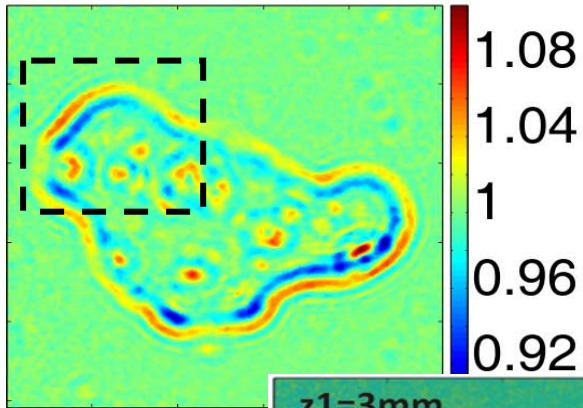


beam size (FWHM vert x horz)
reconstruction: 9.2nm x 9.6 nm
simulation: 12.5nm x 13.6 nm
autocorrelation: 14.2nm x 17.9 nm

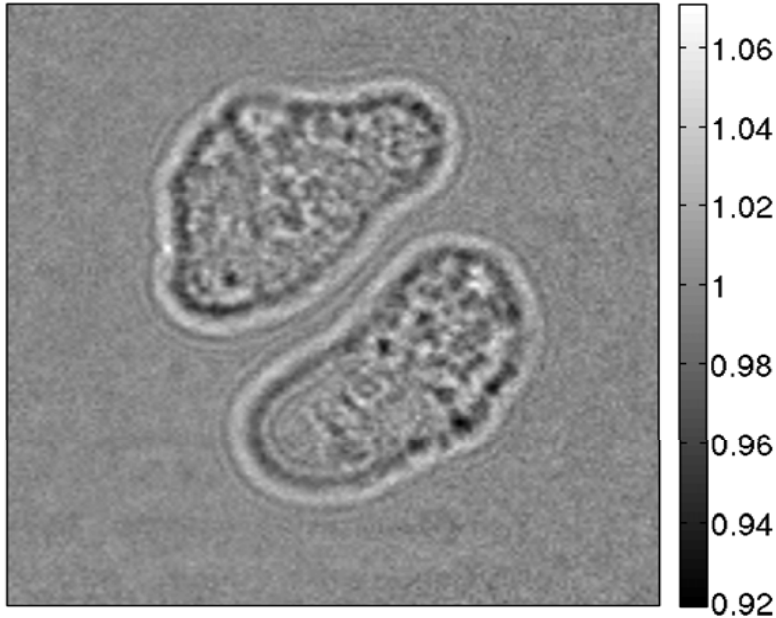
world record in one-dimension: 7nm focus
 by EEM polished mirror @1km long beamline 29 Spring8
 (Yamauchi group, Osaka Univ.)

H. Mimura *et al.*, Nature Physics, 2010
Breaking the 10 nm barrier in hard x-ray focusing

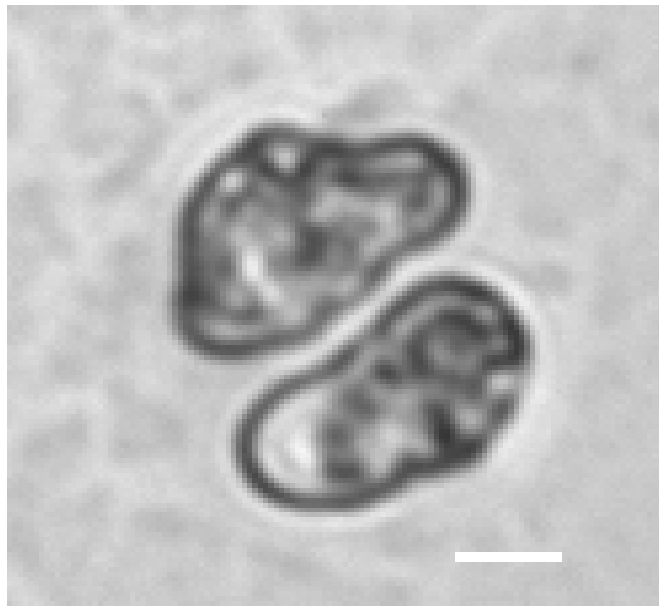
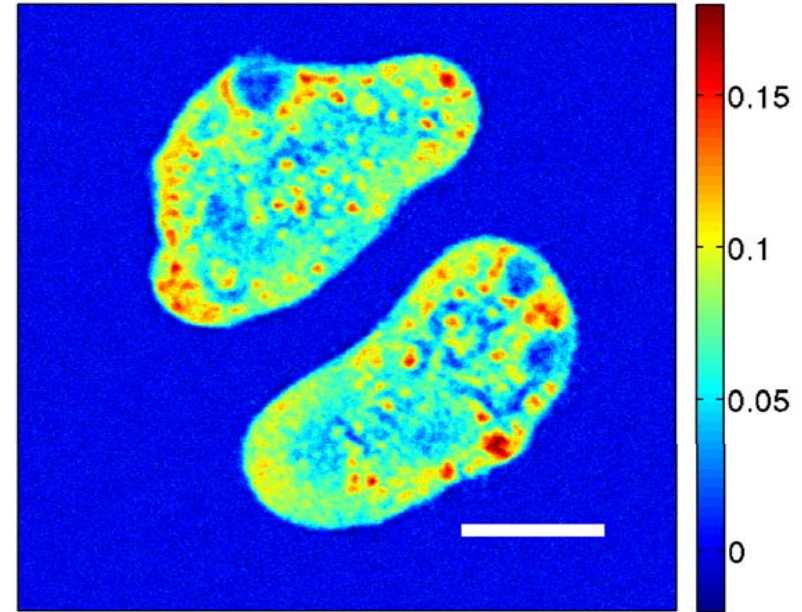
X-ray imaging of cells: *Dictyostelium Discoideum*



Waveguide flux = $1e8$ ph/s
t = 60 x 0.5 sec = 30 sec



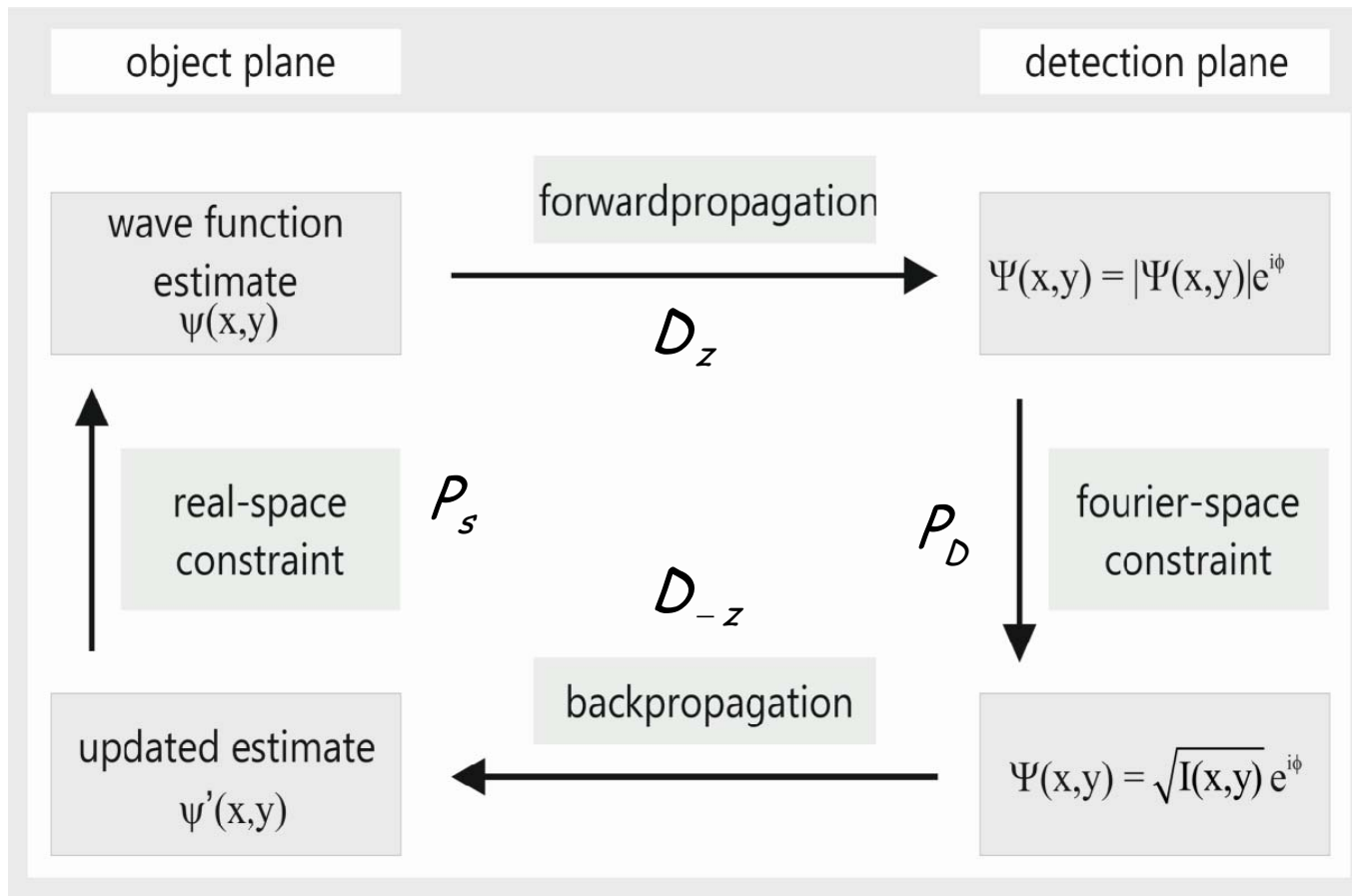
ID 22NI, 17.5 keV
 35 x 35 nm crossed WG
 8.3 mm defocus



Zellen (*Dictyostelium Discoideum*, cryo. fixiert & gefrier getrocknet)

- Phaseninformation durch Referenzwelle
- quantitativer Dichtekontrast
- iterative Rekonstruktion
- Lösung des Zwillingsbildes (hologr. Artefakt)

K. Giewekemeyer, S. Krüger, S. Kalbfleisch,
 M. Bartels, C. Beta, T. Salditt, Physical Review A, 2011



Propagator $D_z = FFT^{-1} \exp[iz \sqrt{k^2 - k_x^2 - k_y^2}] FFT$

P_s : projector in sample plane

$$|\chi_{n+1}(x,y)| = |\chi_n(x,y)| - \beta (|\chi_n(x,y)| - 1)$$

$$\arg(\chi_{n+1}(x,y)) = \begin{cases} \arg(\chi_n) - \gamma \arg(\chi_n') & \forall (x,y) \notin S \\ \min(\arg(\chi_n'), 0) & \forall (x,y) \in S \end{cases}$$

S support (from holographic reconstruction)

P_D : 'projector' in detector plane

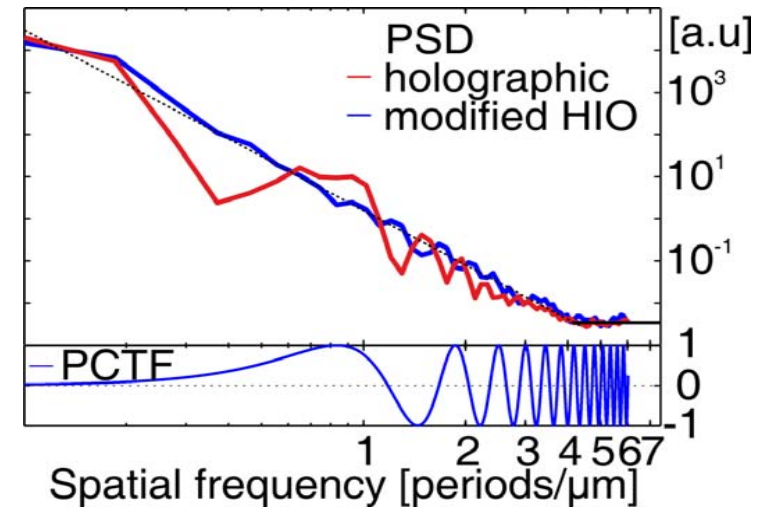
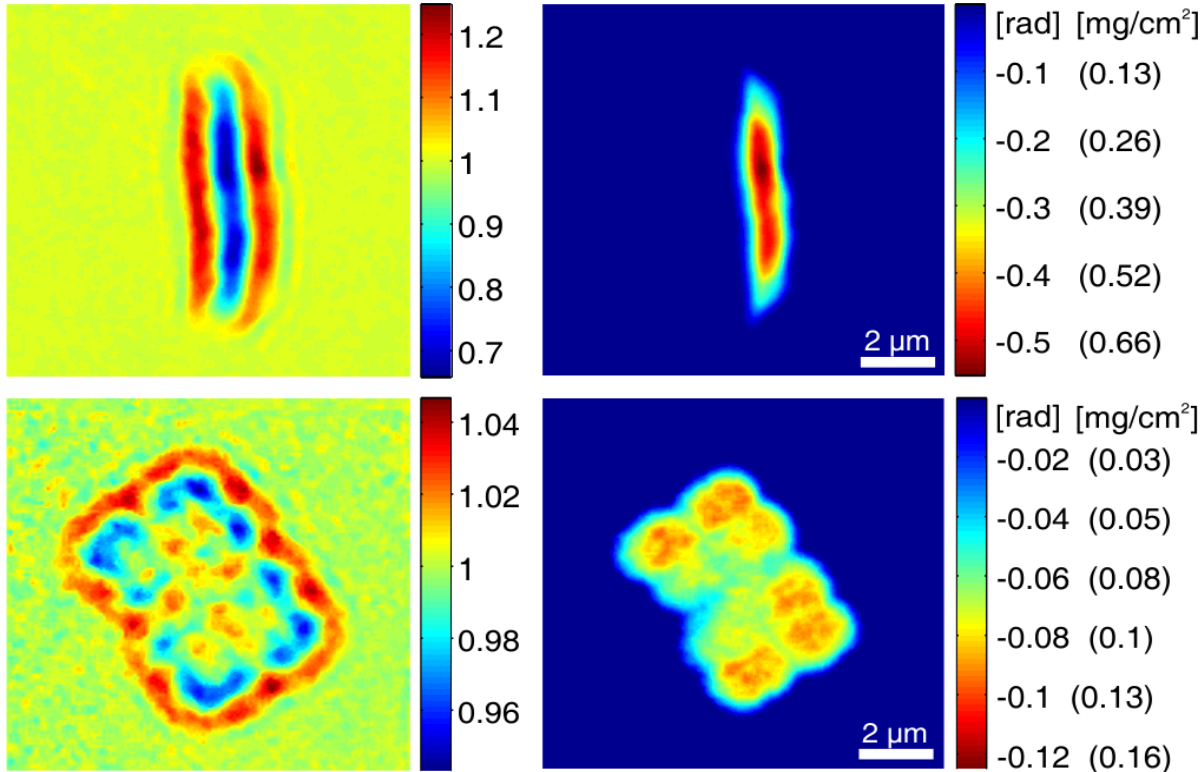
$$|\tilde{\chi}_n'(x,y)|^2 = (1 - \frac{D}{d}) \bar{I}(x,y) + \frac{D}{d} |\tilde{\chi}_n(x,y)|^2$$

$$d^2 = \frac{1}{N} \sum_{x,y} (|\tilde{\chi}_n(x,y)|^2 - \bar{I}(x,y))^2$$

$$D = \sqrt{2 / \langle I_0 \rangle} \text{ noise}$$

X-ray imaging of bacterial cells

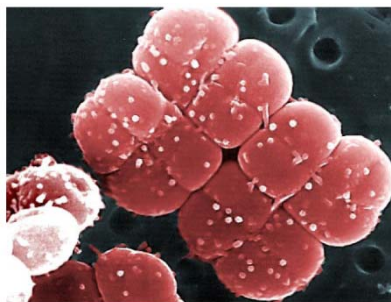
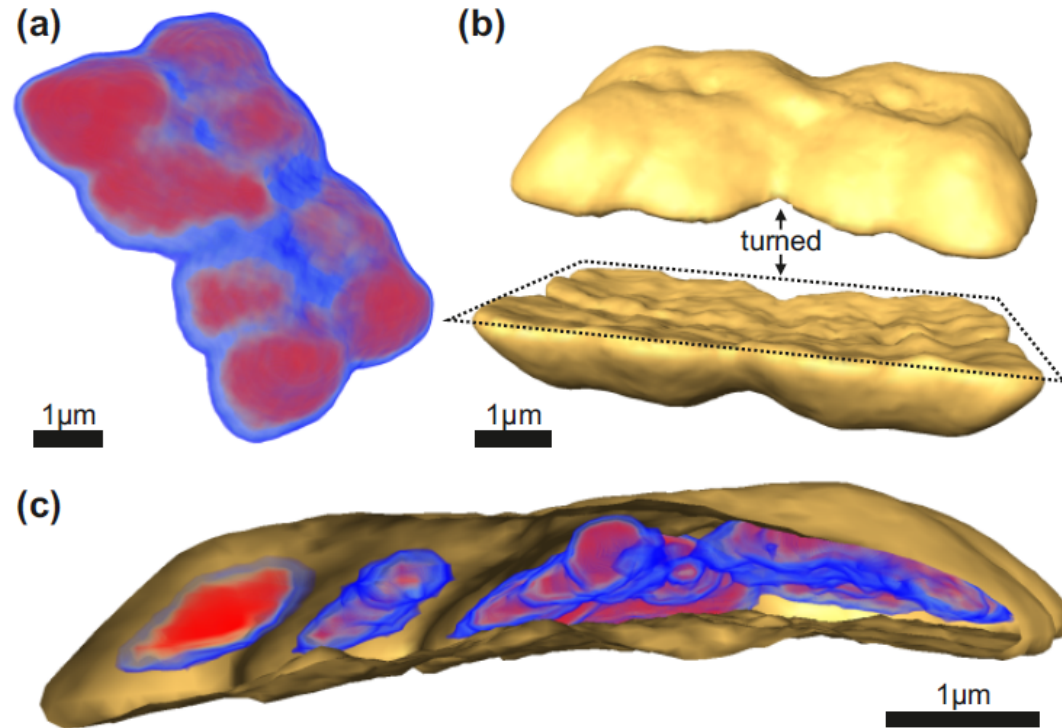
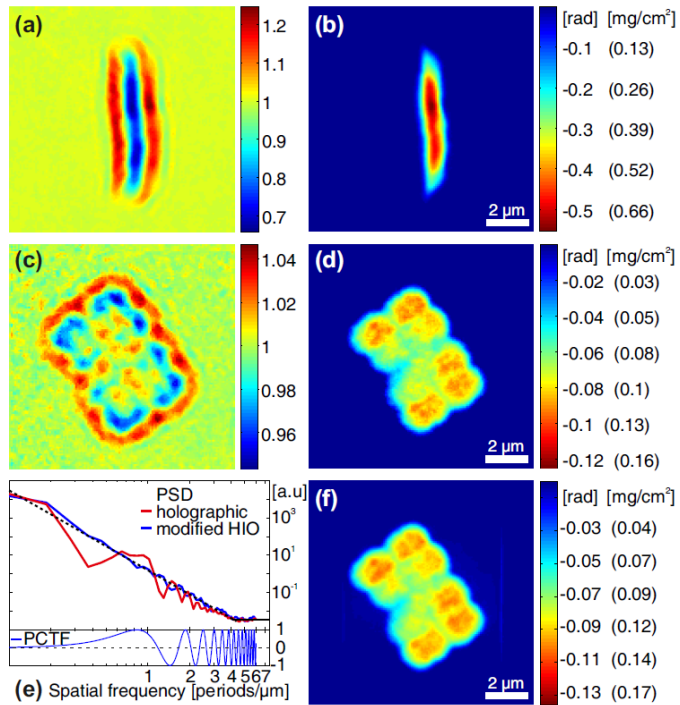
Deinococcus Radiodurans



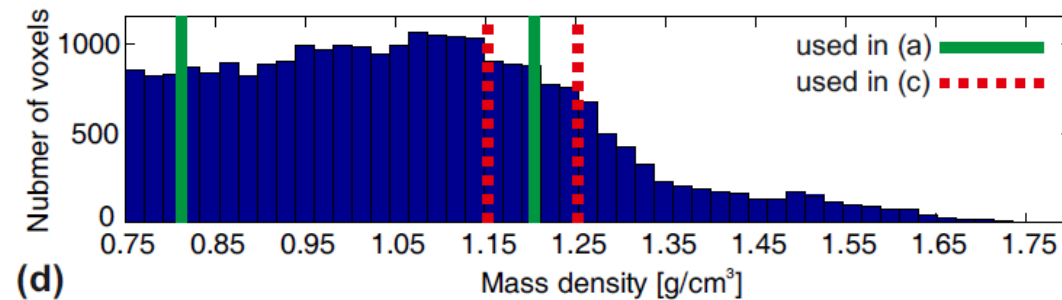
E=13.8 keV
z1=8 mm
z2=5.3 m
M=660
P=55 μm
p=83 nm
t=10 min
F=2.6e5 ph/μm²
D=110 Gy
r=125 nm

DNA packing in nucleoids: Tomography of *Deinococcus Radiodurans*

- Among most radiationresistant organisms on earth, can survive 15 kGy of ionizing radiation
- Very effective DNA repair mechanism, DNA packing debated



2x3 μm size, tetrad morphology
4 identical copies of the genome



Three-Dimensional Visualization of a Human Chromosome Using Coherent X-Ray Diffraction

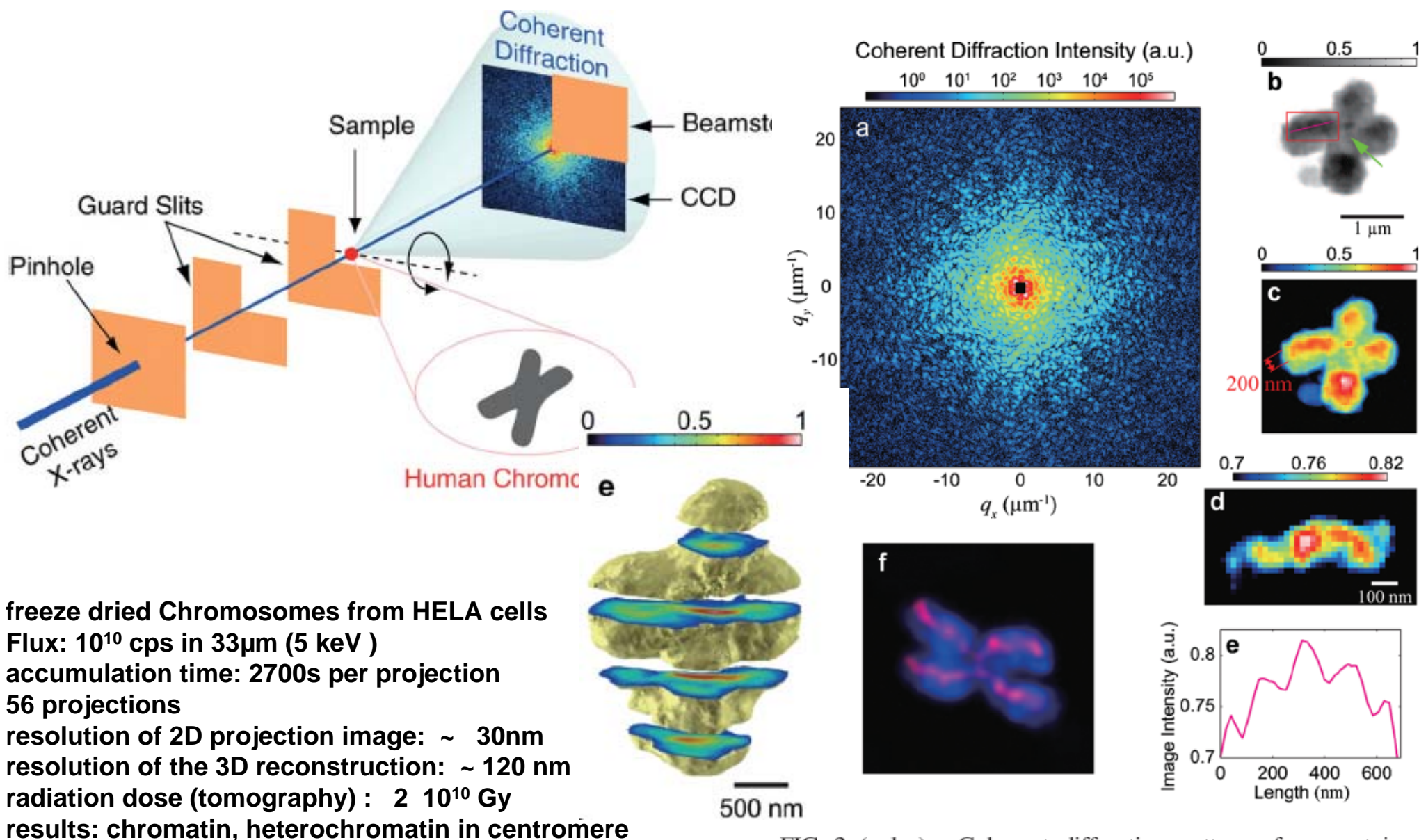
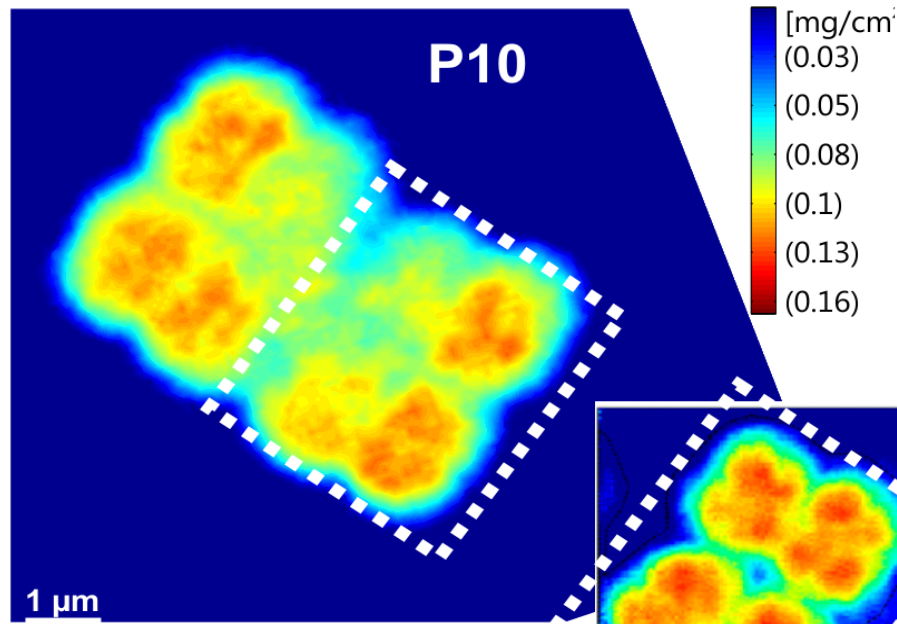


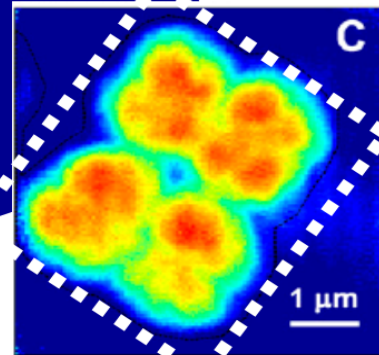
FIG. 2 (color). Coherent diffraction pattern of an unstained human chromosome and its reconstructed projection image. The

X-ray propagation imaging

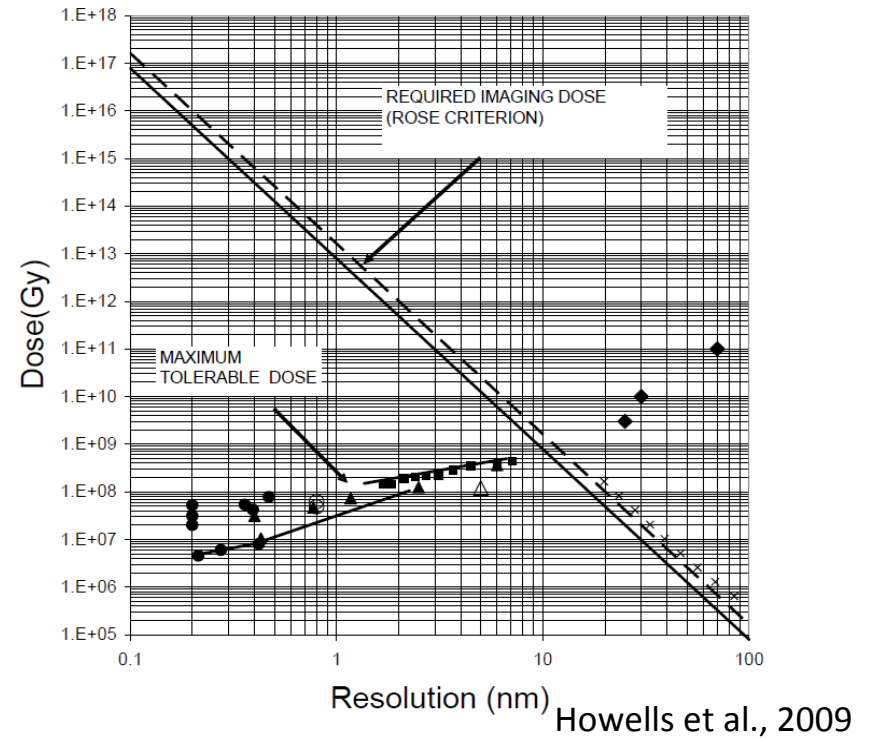
Dose efficiency



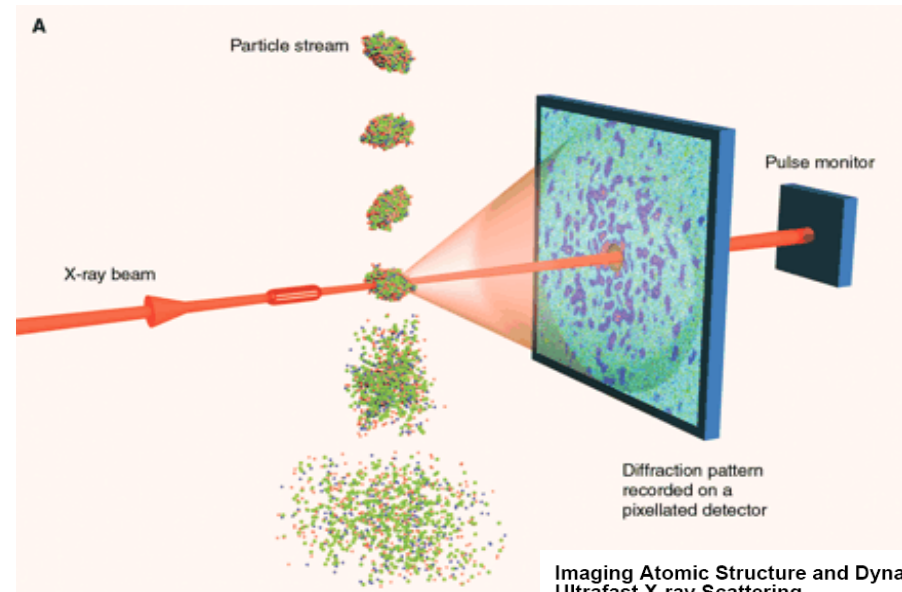
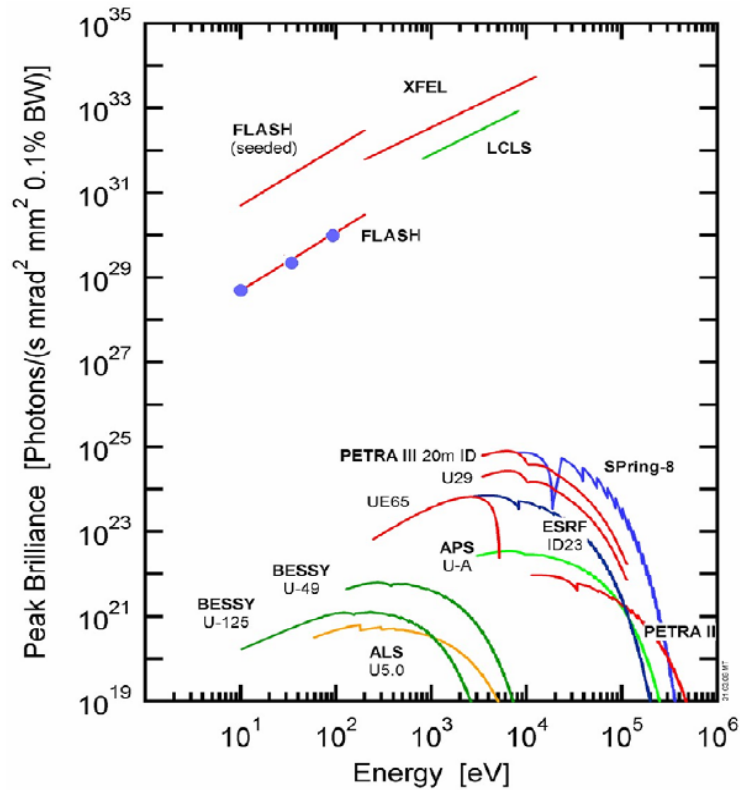
Propagation Imaging
 110 Gy
 4 µm⁻¹



Ptychography*
 1.3e5 Gy
 5.9 µm⁻¹



The advent of x-ray free electron lasers 9 orders in peak brilliance !



Imaging Atomic Structure and Dynamics with Ultrafast X-ray Scattering
K. J. Gaffney, et al.
Science 316, 1444 (2007);

Figure 1. Peak brilliance of storage ring and FEL sources.

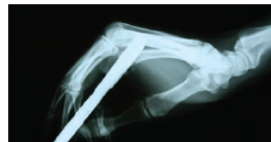
editorial

X-ray vision

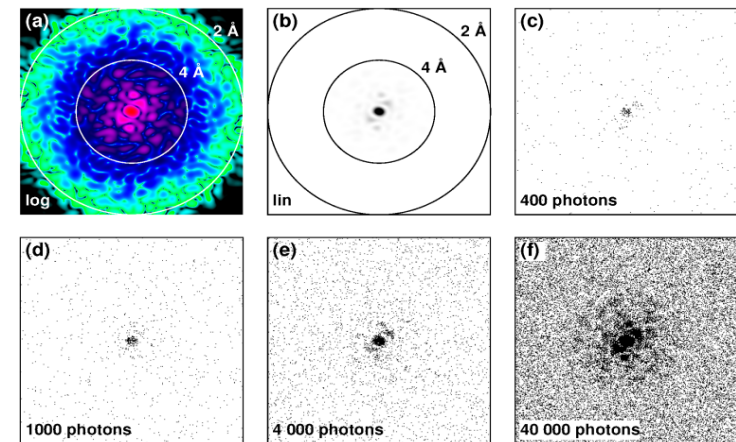
The century-old field of X-ray physics is being rejuvenated by new forms of ultrabright sources based on laser technology, promising a revolution in imaging capabilities.

This month *Nature Photonics* presents a special Focus Issue dedicated to the latest advances in X-ray optics, a field that has a long and rich history.

"I have seen my death," exclaimed Anna Röntgen in mid-November, 1895. She had just seen the first ever human X-ray image — a picture of her own hand revealing the bones beneath the flesh.



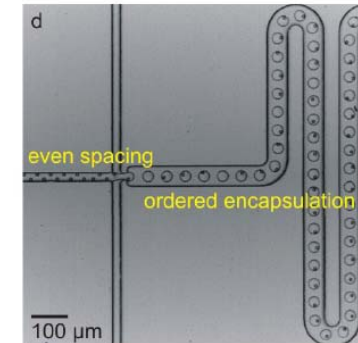
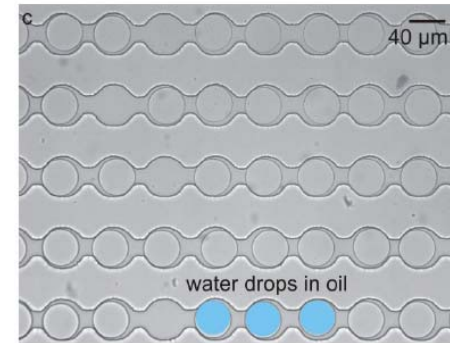
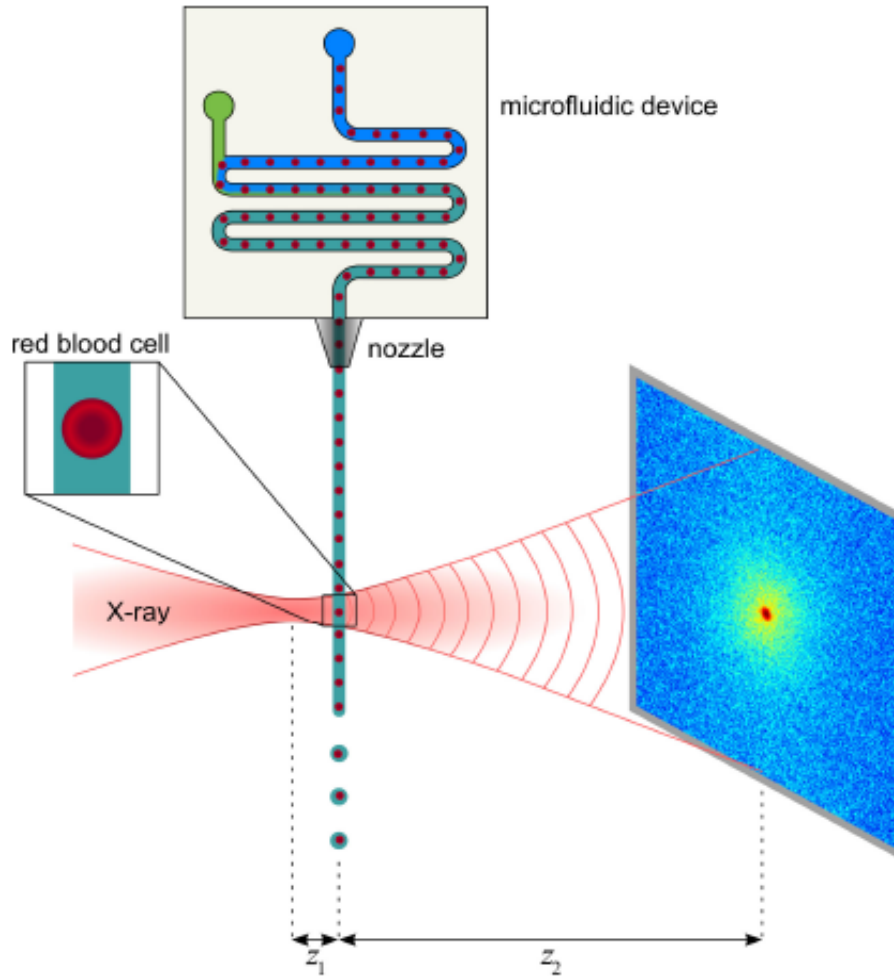
setting, using either high-harmonic generation, laser wakefield or various types of plasma sources. This is in stark contrast with the immobile nature of synchrotrons, in which most high-resolution work has been done so far. X-ray imaging schemes generally utilize soft X-rays or high-spatial-resolution hard X-rays, with or without lenses, in a modality that is



Simulated diffraction images of a single molecule in different representations (a)+(b) and at different intensities (c)-(f).

C10 (Salditt /Köster)

Single pulse cellular imaging (high throughput)



$$N_0 = 10^{12} \text{ photons / pulse}$$

$$\text{assume } N_c = 10^5 \text{ per resolution element } r$$

$$\rightarrow 3000 \times 3000 \text{ pixel in field of view } V$$

$$\lambda = 0.1 \text{ nm}, V = 10 \mu\text{m}, z_1 = 10 \text{ mm}, r = 3 \text{ nm}$$

$$\text{focus } \Delta = 100 \text{ nm}$$

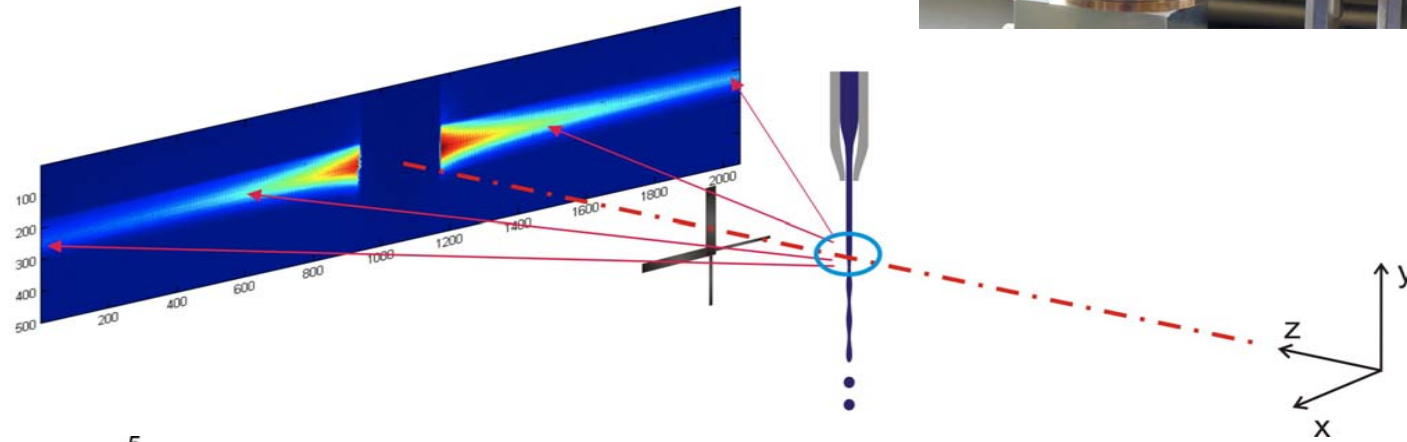
$$\text{fluence at defocus } N_0 \lambda^2 \Delta^2 / z_1^2$$

3D information from anlylography ?

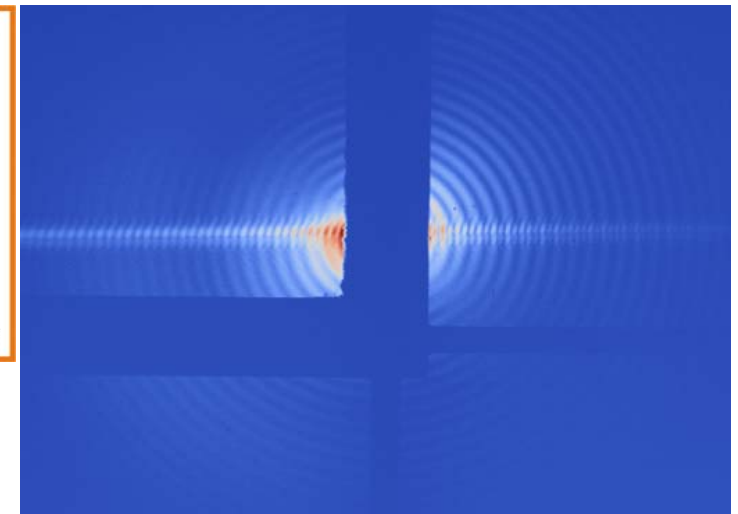
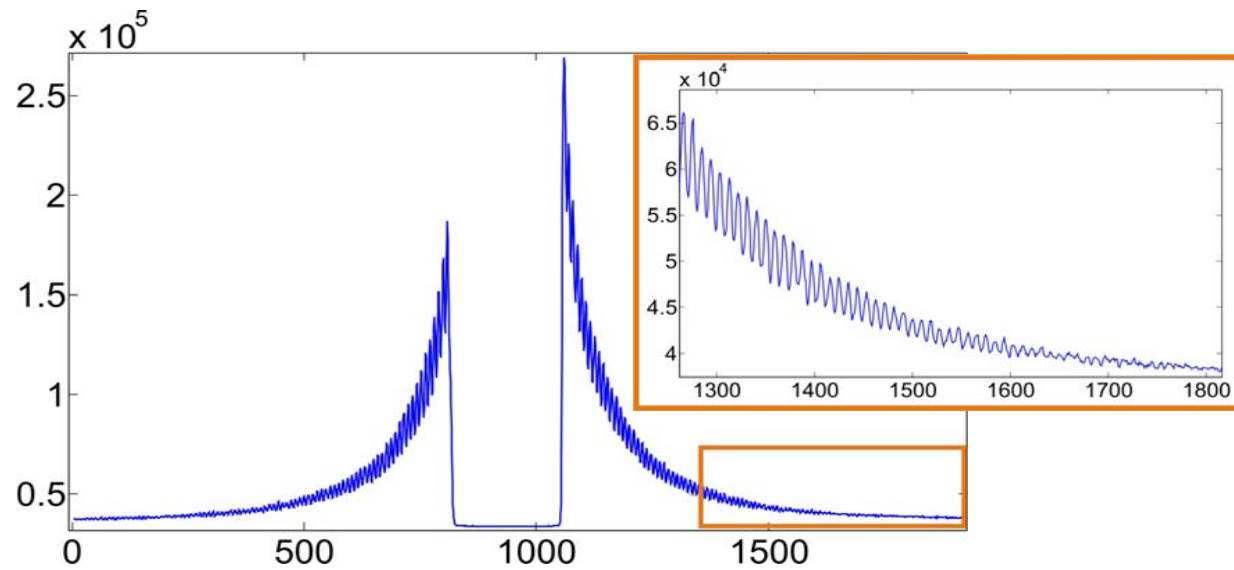
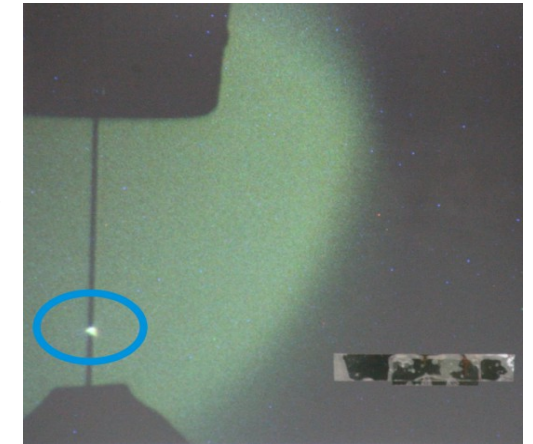
$$\rightarrow @ 10^8 \text{ W / cm}^2 :$$

100mV transmembrane Voltage

FEL – Liquid Jet



FEL



the team / collaborations: acknowledgements

Matthias Bartels *waveguide holography, tomography, neural cells and tissues*
Robin Wilke, *phase reconstruction algorithms, ptychography*
Klaus Giewekemeier *phase reconstruction algorithms, ptychography, cellular imaging*
Marius Priebe *cellular imaging and diffraction*
Christian Oldendrowitz *multicellular organisms*
Sebastian Kalbfleisch *waveguide microscope*
Henrike Neubauer, Sven Krüger *waveguide optics and fabrication*
Markus Osterhoff *numerical optics, focusing, mirror design*
Don-Du Mai, Jörg Hallmann, Tobias Reusch *FLASH experiments*

S. Köster, B. Weinhausen Institut für Röntgenphysik
T. Hohage, R. Luke Angew. Mathematik

A. Rosenhahn, U. Heidelberg
M. Sprung, I. Vartanyants, S. Düsterer, R. Treusch DESY
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