

Signal processing algorithms for wireless connected hearing devices

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Outline

- Use of multiple microphones in hearing aids
 - o Monaural \rightarrow Binaural \rightarrow external microphones
- Binaural signal processing
 - o Objective: noise reduction and binaural cue preservation
 - o Algorithms: binaural beamforming, time-frequency masking, Multi-channel Wiener filter
 - o Experimental results
 - o Bandwidth reduction: iterative distributed MWF
- Wireless acoustic sensor networks
 - o Algorithms: extension of distributed MWF
 - o Effect of bitrate on performance
- Conclusions and future work



- Introduction
- Binaural processing
- Acoustic sensor networks
- Conclusion

Hearing aids

- Problems: background noise, directional hearing
 - o signal processing to selectively enhance useful speech signal and improve speech intelligibility
 - o signal processing to preserve directional hearing (binaural auditory cues) and spatial awareness
 - o robustness important due to small inter-microphone distance
- Binaural auditory cues
 - Interaural Time Difference (ITD) Interaural Level Difference (ILD)
 Interaural Coherence (IC)
 - o Binaural cues, in addition to spectral and temporal cues, play an important role in binaural noise reduction and sound localisation
 - o ITD: f < 1500Hz, ILD: f > 2000Hz





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Hearing aids - Algorithms

- Cochlear loss:
 - o Frequency-specific amplification
 - o Dynamic range compression
- Binaural and central loss:
 - o Noise reduction
 - o Binaural Algorithms
- "Technical" requirements
 - o Feedback control
 - o Occlusion effect / 'own voice' detection
 - o Classification of acoustic environment
 - o (fully digital, 1V supply from very small battery, 5-6d battery time, wireless binaural link)





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Hearing aids - Algorithms

- Digital hearing instruments allow for advanced acoustical signal pre-processing
 - o multiple microphones available \rightarrow spectral + spatial processing
 - o noise reduction (beamforming), computational auditory scene analysis (source localisation, environment classification, ...)



Monaural (2-3)

Binaural

External microphones



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- Signal acquisition in **adverse acoustic environments**:
 - o Microphones at large distance from speaker \rightarrow background noise and reverberation

Acoustic sensor networks:

- o Network of a large number of spatially distributed nodes (each with one or multiple microphones)
- o Wireless data transmission
- o More information about spatial noise field (microphones with higher SNR, higher direct-to-reverberant ratio)
- Objectives:
 - o speech enhancement
 - o source localisation
 - o CASA



Subset of sensors closer to target signal





Binaural processing





- Binaural processing
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Bilateral vs. Binaural

Bilateral system Hearing aid user $Y_{1,0}(\omega)\cdots Y_{1,M_1-1}(\omega)$ $Y_{0,0}(\omega)\cdots Y_{0,M_0-1}(\omega)$ $\mathbf{W}_0(\omega)$ $W_1(\omega)$ $Z_0(\omega)$ $Z_1(\omega)$

Hearing aid user $Y_{0,0}(\omega)\cdots Y_{0,M_0-1}(\omega)$ $Y_{1,0}(\omega)\cdots Y_{1,M_1-1}(\omega)$ $\mathbf{W}_0(\omega)$ $W_1(\omega)$ $Z_0(\omega)$ $Z_1(\omega)$

Binaural system

 Independent left/right processing: Preservation of binaural cues (ILD/ITD) for localisation ?

- Hore microphones:
 - \rightarrow better performance ?
 - \rightarrow preservation of binaural cues ?





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Bilateral vs. Binaural

Bilateral system:

- o Independent processing of left and right hearing aid
- o Negative effect on localisation cues and intelligibility through binaural hearing advantage [Van den Bogaert, 2006; Keidser, 2009]



RMS error per loudspeaker when accumulating all responses of the different test conditions (NH = normal hearing, NO = hearing impaired without hearing aids, O = omnidirectional configuration, A = adaptive directional microphone)



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Bilateral vs. Binaural

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[Bronkhorst and Plomp, 1988]

[Beutelmann and Brand, 2006] 10



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Bilateral vs. Binaural

Bilateral system

- o Independent processing of left and right hearing aid
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• Binaural system

- o Cooperation between left and right hearing aid (e.g. wireless link) \rightarrow **centralised** vs. **distributed** processing
- o Bandwidth constraint and latency of wireless link

Objectives/requirements for binaural algorithm:

- 1. SNR improvement: noise reduction, limit speech distortion
- 2. Preservation of binaural cues (all sources) to exploit binaural hearing advantage
- 3. No assumption about position of speech source and microphones



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Binaural noise reduction techniques

• Configuration: microphone array with *M* microphones at left and right hearing aid, communication between hearing aids

$$Y_{0,m}(\omega) = X_{0,m}(\omega) + V_{0,m}(\omega), \quad m = 0...M_0 - 1$$

speech noise

• Use all microphone signals to compute output signal at both ears

$$Z_0(\boldsymbol{\omega}) = \mathbf{W}_0^H(\boldsymbol{\omega})\mathbf{Y}(\boldsymbol{\omega}), \quad Z_1(\boldsymbol{\omega}) = \mathbf{W}_1^H(\boldsymbol{\omega})\mathbf{Y}(\boldsymbol{\omega})$$





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Binaural noise reduction techniques

- Time-frequency post-processing/masking:
 - o Computation and application of **real-valued** binaural mask/weight based on binaural and temporal/spectral cues
 - o Can be merged with MVDR-beamformer or ICA-based processing
 - Good preservation of binaural cues for **all** sources
 - Single-microphone spectral enhancement" artefacts at low SNRs





Beamformer: $\mathbf{W}_{b} = \frac{\Gamma^{-1}\mathbf{d}}{\mathbf{d}^{H}\Gamma^{-1}\mathbf{d}} \Rightarrow Y' = \mathbf{W}_{b}^{H}\mathbf{Y}$ Post-Filter: $H_{p} = \frac{\left(|d_{0}|^{2} + |d_{1}|^{2}\right)|Y'|^{2}}{|Y_{0}|^{2} + |Y_{1}|^{2}} \Rightarrow Z = H_{p}\begin{bmatrix}Y_{0}\\Y_{1}\end{bmatrix}$

[Rohdenburg 2009, Reindl 2010, Saruwatari 2010]



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Binaural noise reduction techniques

- Beamforming: spatial selectivity + binaural speech cues
 - o Maximize directivity index while restricting speech ITD error [Desloge, 1997]
 - o Superdirective beamformer using HRTFs [Lotter, 2004]
 - o Adaptive beamforming based on GSC [Welker, 1997]
 - low computational complexity
 - Iimited performance, known geometry, only speech cues may be preserved (in ideal situations)





[Welker, 1997]



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[S. Doclo, S. Gannot, M. Moonen, A. Spriet, Handbook on Array Processing and Sensor Networks, Wiley, 2010.]

[B. Cornelis, S. Doclo, T. Van den Bogaert, J. Wouters, M. Moonen, IEEE Trans. Audio, Speech and Language Processing, Feb. 2010.]

[S. Doclo, T.J. Klasen, M. Moonen, T. Van den Bogaert, J. Wouters, R.P. Derleth, S. Korl, US2010002886.]

Binaural noise reduction techniques

Binaural multi-channel Wiener filter: estimate of speech component in microphone signal at both ears (usually front mic) + trade-off between noise reduction and speech distortion

$$V(\mathbf{W}) = E \left\{ \begin{bmatrix} X_{0,r_0} & \mathbf{W}_0^H \mathbf{X} \\ X_{1,r_1} & \mathbf{W}_1^H \mathbf{X} \end{bmatrix}^2 + \mu \begin{bmatrix} \mathbf{W}_0^H \mathbf{V} \\ \mathbf{W}_1^H \mathbf{V} \end{bmatrix}^2 \right\} \implies \mathbf{W}_{SDW} = \mathbf{R}^{-1} \mathbf{r}$$

speech component
in from Princhopistoria noise reduction
$$\mathbf{R} = \begin{bmatrix} \mathbf{R}_x + \mu \mathbf{R}_v & \mathbf{0}_M \\ \mathbf{0}_M & \mathbf{R}_x + \mu \mathbf{R}_v \end{bmatrix}, \quad \mathbf{r} = \begin{bmatrix} \mathbf{r}_{x0} \\ \mathbf{r}_{x1} \end{bmatrix}, \quad \mathbf{R}_x = \mathbf{R}_y - \mathbf{R}_y$$

- o Estimate \mathbf{R}_{y} during speech-dominated time-frequency segments, estimate \mathbf{R}_{v} during noise-dominated segments, requiring robust voice activity detection (VAD) mechanism
- o No assumptions about positions of microphones and sources
- o Different implementations:
 - Batch (off-line) vs. adaptive (update correlation matrices)
 - Using spatial prediction (SP) between speech components



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Binaural noise reduction techniques

- Binaural multi-channel Wiener filter:
 - o Preservation of binaural cues (ITD-ILD)
 - Speech cues are preserved, no a-priori assumptions
 - Noise cues are distorted
 - o **Extensions** in order to preserve binaural cues of both speech and noise sources, without substantially compromising noise reduction
 - Partial noise estimation (MWFv)
 - Extension with Interaural Transfer Function (MWF-ITF) or Interaural Coherence (MWF-IC) of noise source



$$J_{SDW\eta}(\mathbf{W}) = E\left\{ \left\| \begin{bmatrix} X_L - \mathbf{W}_L^H \mathbf{X} \\ X_R - \mathbf{W}_R^H \mathbf{X} \end{bmatrix} \right\|^2 + \mu \left\| \begin{bmatrix} \eta V_L - \mathbf{W}_L^H \mathbf{V} \\ \eta V_R - \mathbf{W}_R^H \mathbf{V} \end{bmatrix} \right\|^2 \right\}, \quad 0 \le \eta \le 1$$

$$J_{MWF-ITF} = J_{MWF} + \delta \mathcal{E} \left\{ \left| \mathbf{W}_{0}^{H} \mathbf{V} - IT F_{v}^{des} \mathbf{W}_{1}^{H} \mathbf{V} \right|^{2} \right\}$$

$$J_{MWF-IC} = J_{MWF} + \delta \left| \frac{\mathcal{E} \left\{ \mathbf{W}_{0}^{H} \mathbf{V} \mathbf{V}^{H} \mathbf{W}_{1}^{H} \right\}}{\sqrt{\mathcal{E} \left\{ \left| \mathbf{W}_{0}^{H} \mathbf{V} \right|^{2} \right\} \mathcal{E} \left\{ \left| \mathbf{W}_{1}^{H} \mathbf{V} \right|^{2} \right\}}} - IC_{v}^{des} \right|^{2}$$



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Experimental results (1)

Identification of HRTFs

- o Binaural recordings on CORTEX MK2 artificial head
- o 2 omni-directional microphones on each hearing aid (d=1cm)
- o $LS = -90^{\circ}:15^{\circ}:90^{\circ}, 90^{\circ}:30^{\circ}:270^{\circ}, 1m$ from head
- o Conditions: T_{60} =510 ms, f_s=16 kHz





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Audio demo

- Speech and noise material:
 - o HINT sentences, speech source in front (0°)
 - o Multi-talker babble noise at 60°
 - o SNR=0 dB, f_s=16 kHz, FFT-size N=256, μ =1, α =0

	Noisy	Speech	Noise
Input			
Output (β=0)			
Output (β=0.05)			



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Perceptual evaluation: SRT

- SRT measurements (headphone presentation, 10 NH)
- Speech sentences + babble noise
- Algorithms: state-of-the art bilateral (ADM), MWF, MWFv (η=0.2)
- Conditions: S_0N_{60} , $S_{90}N_{270}$ and $S_0N_{90/180/270}$

	$S_0 N_{60}$			S ₉₀ N ₂₇₀			S ₀ N _{90/180/270}		
Bilat/bin Δ SRT (dB)	Perceptual	Left	Right	Perceptual	Left	Right	Perceptual	Left	Right
ADM	2.1 ± 1.9	2.7	2.8	$-4.3 \pm 1.3^{*}$	4.3	-3.2	1.3 ± 1.4	6.0	5.9
MWF ₂₊₂	$4.3 \pm 1.5*$	4.9	9.6	0.7 ± 1.4	10.0	2.5	$4.6 \pm 0.8 *$	7.1	7.2
MWF ₂₊₁	$3.8 \pm 1.6^{*}$	4.0	6.2	0.3 ± 2.0	9.6	2.1	$4.0 \pm 1.5^{*}$	6.6	6.0
MWF ₂₊₀	$1.0 \pm 0.7*$	1.9	3.3	-1.2 ± 1.6	3.8	1.0	$2.8 \pm 1.3^{*}$	5.1	4.9
MWF ₂₊₂ -N _{0.2}	$3.6 \pm 1.4^{*}$	3.3	5.4	$2.0 \pm 1.4^{*}$	4.3	1.9	$3.2 \pm 0.8^{*}$	4.1	4.2
MWF ₂₊₁ -N _{0.2}	$2.7 \pm 1.3*$	2.6	3.0	1.5 ± 1.6	3.9	1.6	$3.4 \pm 0.8*$	3.7	3.3
$MWF_{2+0}-N_{0.2}$	1.0 ± 2.1	1.1	0.9	0.0 ± 1.5	1.0	0.7	$2.3 \pm 1.4*$	2.8	2.6
[T. Van den Bogaert, S. Doclo, J. Wouters, M.									



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Perceptual evaluation: SRT

• SRT measurements (10 NH, 8 HI)



FIG. 7. (Color online) Average SRT results of ten normal hearing subjects (NH) and eight hearing aid users (HA) for the $S_0N_{90/180/270}$ scenario. Standard deviations are indicated by error bars. Algorithms which significantly improve the SRT for both groups, compared to the unprocessed (REF) condition, are marked by an "*" above the graph.



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Perceptual evaluation: localisation

- Algorithms: unprocessed, state-of-the art bilateral, MWF, MWFv (η =0.2)
- Conditions: S_0N_{60} , $S_{45}N_{315}$ and $S_{90}N_{270}$



[T. Van den Bogaert, S. Doclo, J. Wouters, M. Moonen, Journal of the Acoustical Society of America, Jan. 2009.]



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Experimental results (2)

Acoustic environment



- Cafeteria with recorded babble noise and simulated speaker at position B
- Binaural hearing aid with 3 microphones
- German sentences taken from OLSA speech material
- Speech in continuous babble noise
 - f_s: 16 kHz, WOLA, FFT-size: 256 samples, Overlap: 75%

http://medi.uni-oldenburg.de/hrir/ [Kayser et al. 2009]



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Experimental results

Subjective Evaluation

- o Improvement of Speech Reception Threshold (SRT)
- o Oldenburg Sentence Test (10 NH subjects)
- o Binaural presentation using headphones



[D. Marquardt, V. Hohmann, S. Doclo, DAGA 2011]



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[S. Doclo, T. Van den Bogaert, M. Moonen, J. Wouters, IEEE Trans. Audio, Speech and Language Processing, Jan. 2009.]

Distributed MWF

Binaural MWF

- o **all** microphone signals are transmitted over wireless link
- Reduce bandwidth requirement of wireless link by transmitting one signal from contralateral ear
 - o Raw microphone signal (e.g. front)
 - o Output of fixed (e.g. superdirective) beamformer
 - o MWF-estimate using only contralateral microphone signals
 - o Iterative distributed binaural MWF scheme (DB-MWF)





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Distributed MWF

Iterative procedure

o In each iteration \mathbf{F}_{10} is equal to \mathbf{W}_{00} from previous iteration, and \mathbf{F}_{01} is equal to \mathbf{W}_{11} from previous iteration





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• Now consider more than 2 sensor nodes...

• Challenges:

- o *Dynamic array configuration*: large number of microphones at unknown positions, dynamic subset selection
- o *Distributed and collaborative algorithms:* power and complexity constraints, effect of limited bandwidth
- o Calibration and synchronisation issues: same time basis
- Prototype applications:
 - o Hearing aids using extra microphones (room, other HA, ...)
 - o Video-conferencing using all microphones on laptops / room
 - o Surveillance





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- Recently has become quite a hot research topic
 - Distributed MWF: extension to multiple sensor arrays and multiple desired sources (DANSE) [Bertrand 2010]
 - o Distributed MVDR/LCMV-beamformer [Golan 2010, Bertrand 2011]
 - Performance analysis of a randomly spaced wireless microphone array, statistical performance of MWF [Golan 2011, Lawin-Ore 2012]
 - Dynamic signal combining (no synchronisation required)
 [Matheja 2011, Srinivasan 2011, Stenger 2011]







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Experimental results



 $T_{60} = 0,22 s$

[Bertrand 2009]



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Rate constraints

Investigate effect of capacity of wireless link → encode signal(s) at finite bit-rate *R* before transmission



- **Rate-distortion:** $R(\lambda) = \frac{1}{4\pi} \int_{-\infty}^{\infty} \max\left(0, \log_2 \frac{\Phi_Y^{01}(\omega)}{\lambda}\right) d\omega$ $D(\lambda) = \frac{1}{2\pi} \int_{-\infty}^{\infty} \min\left(\lambda, \Phi_Y^{01}(\omega)\right) d\omega,$ PSD of transmitted signal
- Upper bound on achievable performance can be calculated using forward channel representation



$$B = \max\left(0, \frac{\Phi_Y^{01} - \lambda}{\Phi_Y^{01}}\right)$$

$$\Phi_W = \max\left(0, \lambda \frac{\Phi_Y^{01} - \lambda}{\Phi_Y^{01}}\right)$$



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Rate constraints

- Effect on performance of distributed MWF (DANSE)
 - o **Case 2:** spread iterations over subsequent frames (stationarity)



DANSE scheme converges after i=2 iterations, moreover achieving highest performance gain



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• Future work/challenges:

- Speech enhancement algorithms:
 - Dynamic subset selection for time-varying situations
 - Theoretical performance analysis (statistical room acoustics) \rightarrow optimal microphone configuration
- o Computational auditory scene analysis:
 - E.g. multi-source localisation by merging energy- and correlationbased techniques
- o Calibration and synchronisation techniques:
 - With and without reference signals
- o (Perceptual) coding of transmitted signals







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Conclusions

- Speech enhancement algorithms in hearing instruments
 - o More and more microphones: monaural \rightarrow binaural \rightarrow acoustic sensor networks
 - o Algorithms: beamforming, post-processing, MWF
- Bandwidth reduction by transmitting filtered combination of microphone signals
 - o D-MWF: iterative procedure, converging to centralized MWF
- Effect of bit-rate on performance using rate-distortion theory
 - o D-MWF achieves highest performance gain, when iterations can be spread over subsequent frames
- Remaining challenges in acoustic sensor networks:
 - o **Algorithms**: robustness, dynamic subset selection, distributed algorithms, optimal microphone configuration
 - o (Perceptual) coding of transmitted signal
 - o Technical issues of wireless link: latency, synchronisation



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Questions ?



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