

Acoustically transparent sound presentation in hearing devices: algorithms, devices and models

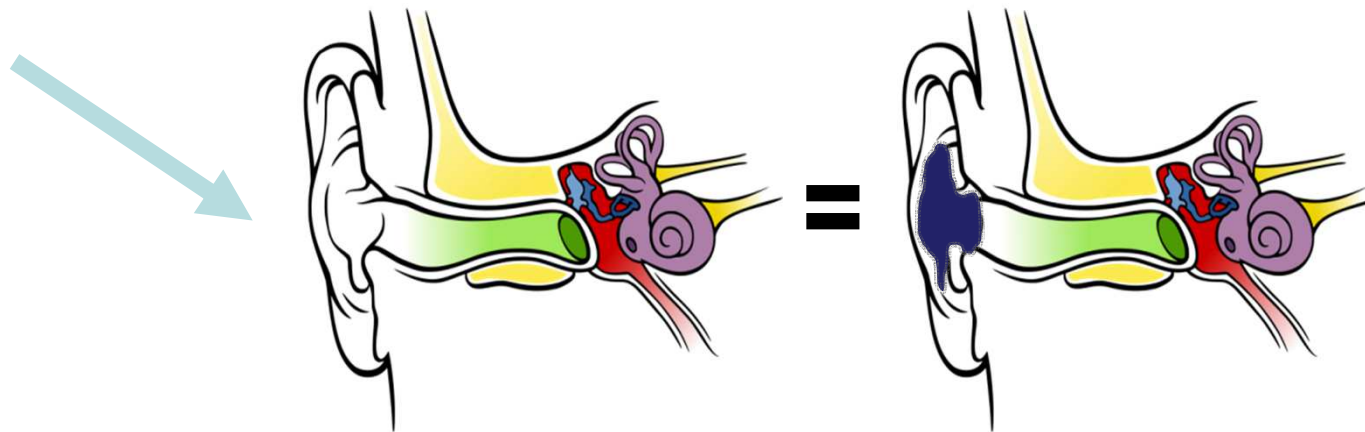
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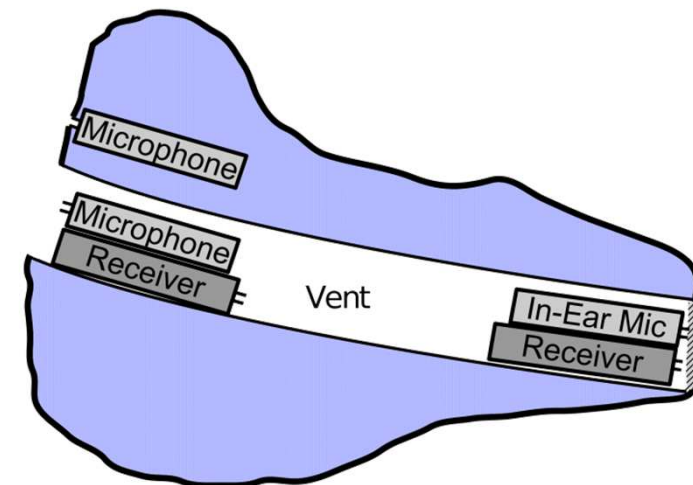
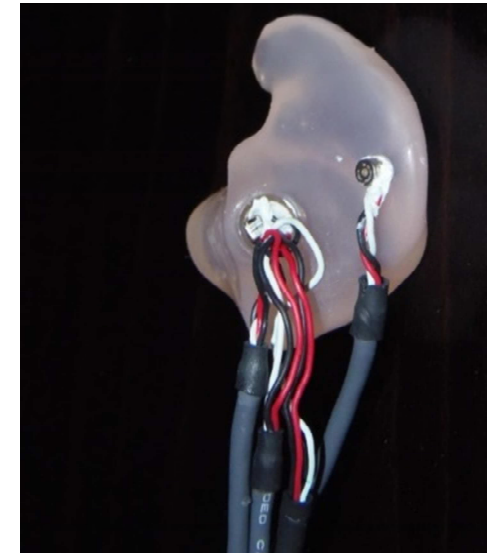
Acoustically Transparent Earpiece

- Current hearing devices: **sound quality still limited** (e.g., distortion, non-individualized, own voice, spatial impression)
- **Acoustic transparency:** enable hearing comparable to the open ear while providing desired sound enhancement (e.g., amplification, dynamic range compression, noise reduction)



Acoustically Transparent Earpiece

- **Custom in-the-ear earpiece** with multiple integrated microphones and receivers and relatively open acoustics
 - Vent/core: **2 microphones and 2 receivers** (woofer/tweeter)
 - Concha: **1 microphone**
- Insertion into individual silicone ear mould or generic earplugs



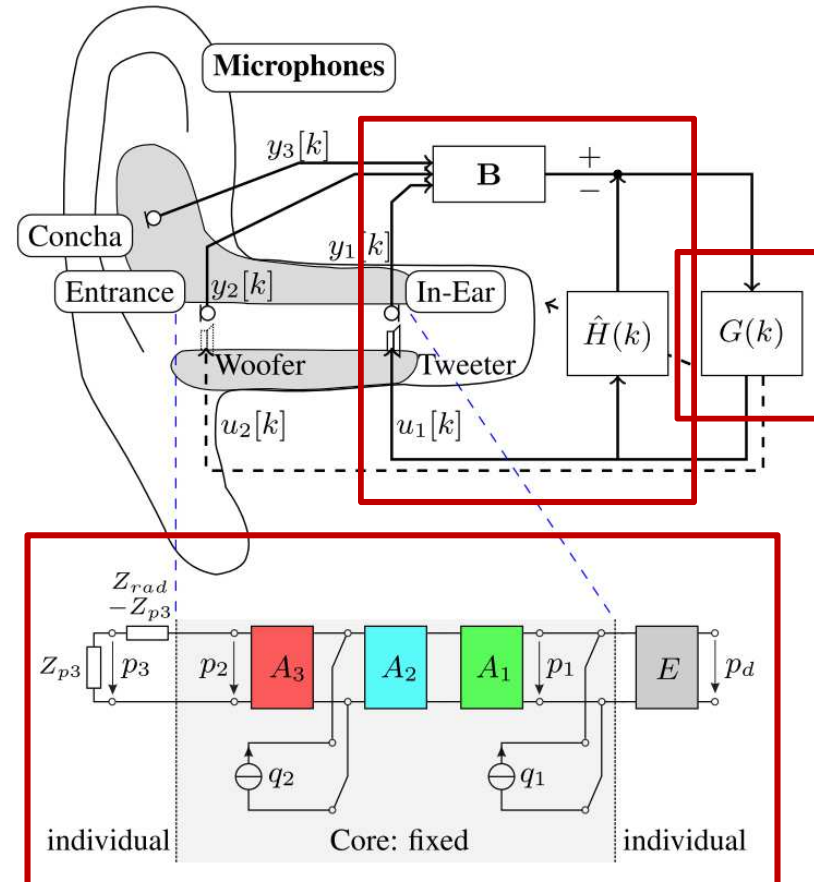
Acoustically Transparent Earpiece

1. Transparent sound presentation:

- Natural sound quality by equalizing to open-ear target response at eardrum (using single/multiple receivers)

2. Individualized Electro-Acoustic Model:

- Better understand acoustics
- Predict sound pressure and transfer functions (eardrum)



3. Acoustic Feedback cancellation

- Exploit multiple microphones to steer null towards position of receiver
- Exploit multiple receivers

4. Hearing support:

- Amplification and dynamic range compression
- Noise reduction (active/passive)
- Occlusion management

1. Transparent sound presentation

• Single-loudspeaker Equalization

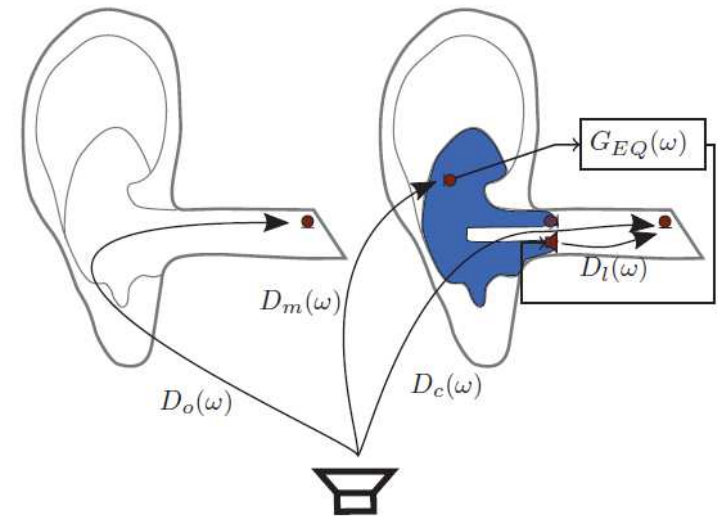
- **Goal:** Achieve target sound pressure at aided ear that is (physically or perceptually) equivalent to pressure at open ear (i.e. individual HRTF)

$$\begin{aligned}\hat{D}_o(\omega) &= D_{aided}(\omega) \\ &= D_m(\omega)G_{EQ}^{(opt)}(\omega)D_l(\omega) + D_c(\omega),\end{aligned}$$

$$G_{EQ}^{(opt)}(\omega) = \frac{\hat{D}_o(\omega) - D_c(\omega)}{D_m(\omega)D_l(\omega)}$$

1. **Estimate target pressure** based on outer microphone(s), e.g., frequency-dependent gain
2. **Equalization with hearing device:** adjust filter G such that direct sound + device output = target

- **In-Situ calibration routine,** assuming that pressure at eardrum is known using in-ear microphone



1. Transparent sound presentation

- **Single-loudspeaker Equalization**

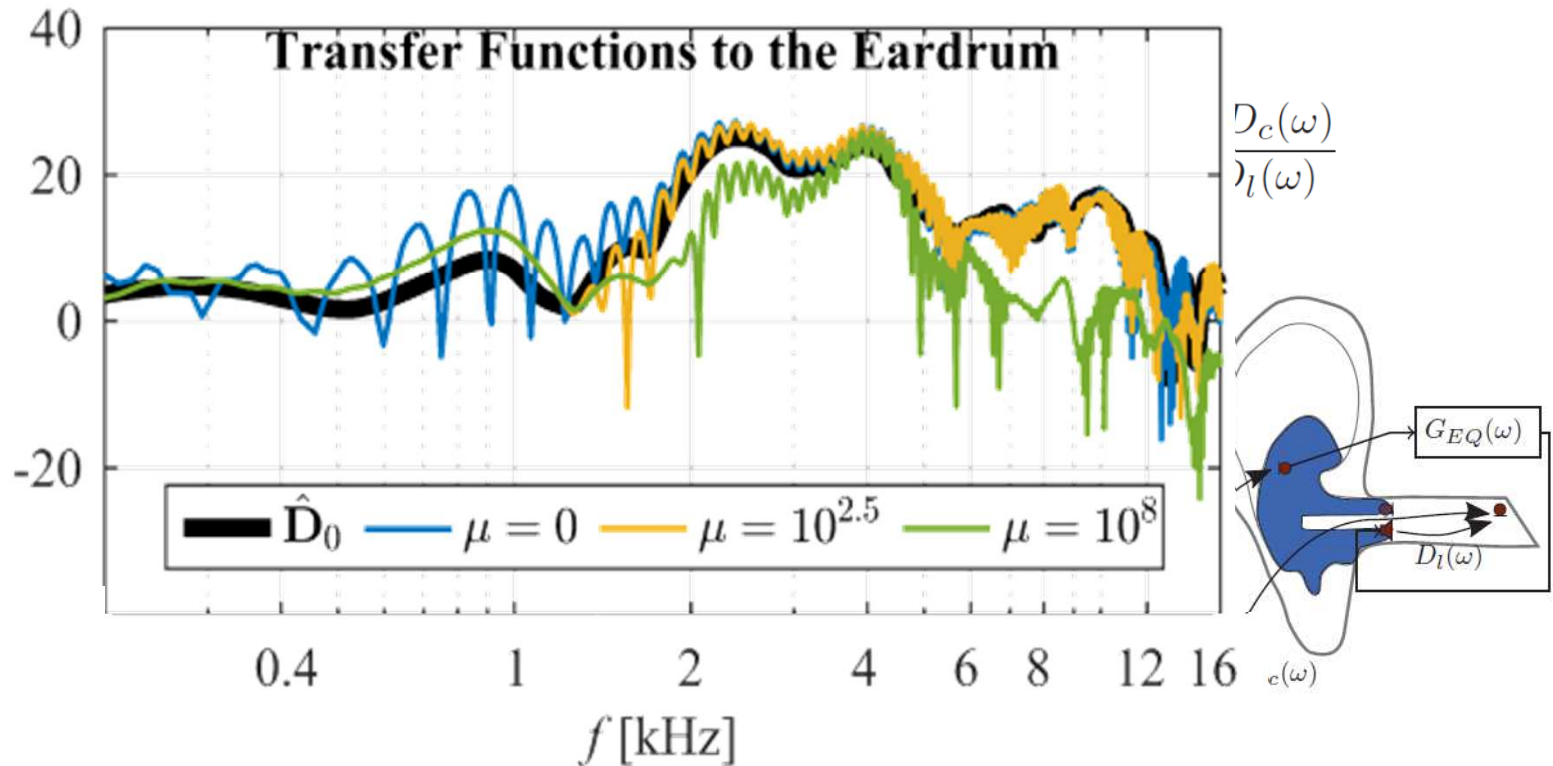
- **Goal:** Achieve target sound pressure at aided ear that is (physically or perceptually) equi

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1.

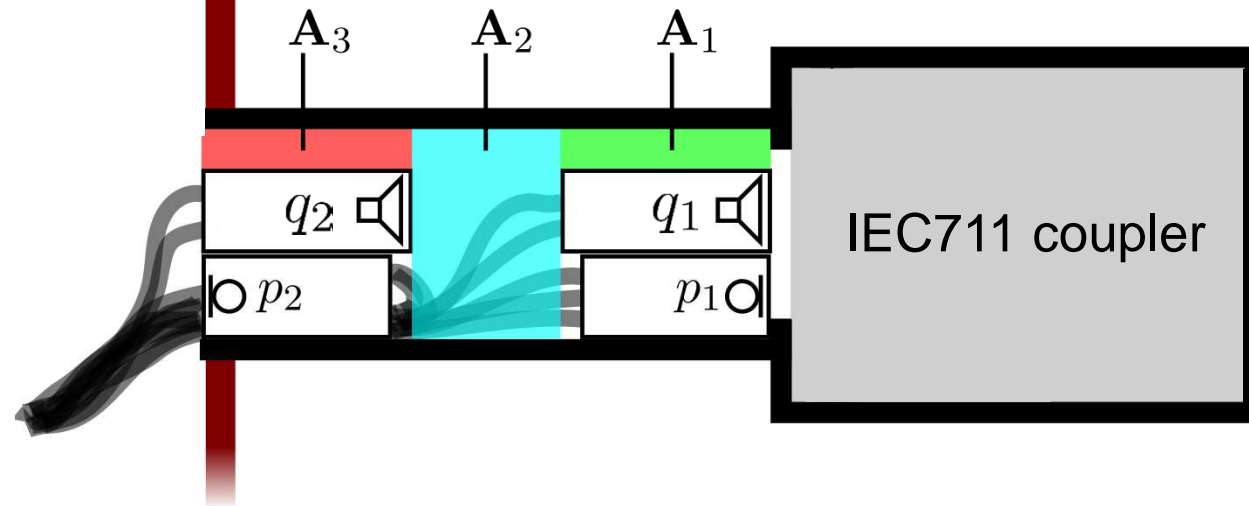
2.

- **In-Situ**
 assumin
 eardrum
 microphone



2. Electro-acoustic model

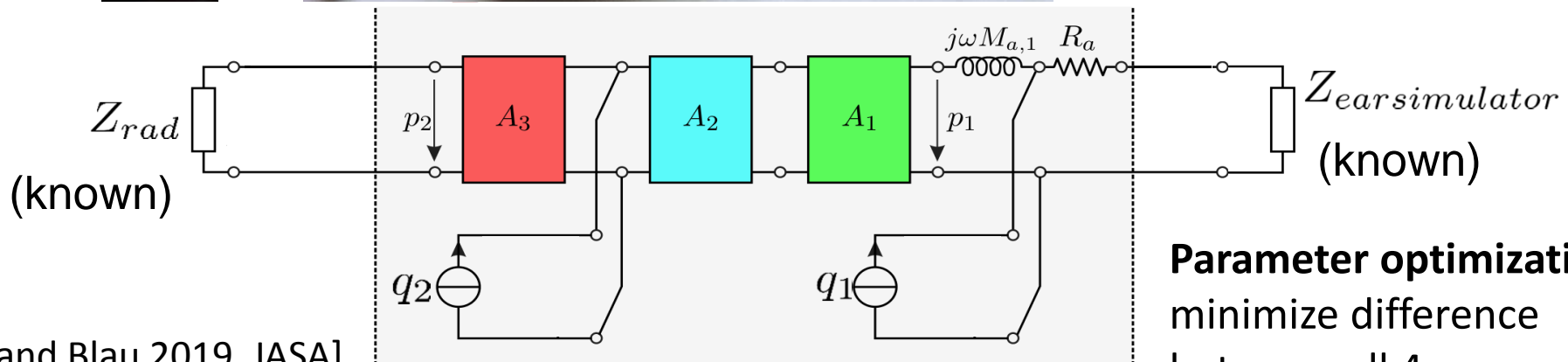
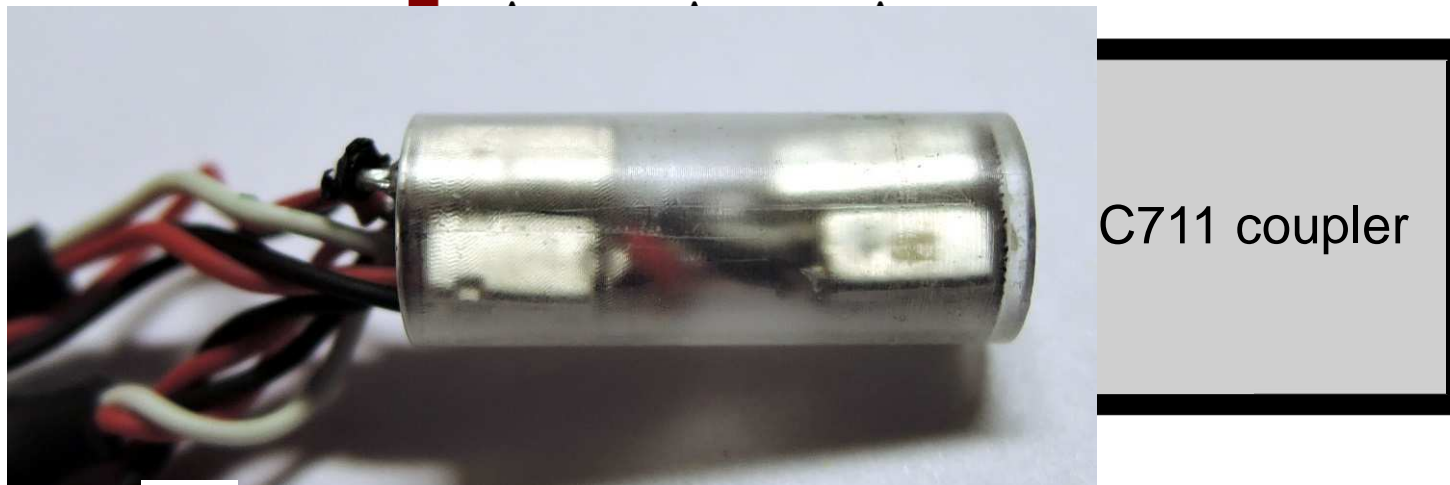
- Earpiece Model (Fixed)



[Vogl and Blau 2019, JASA]

2. Electro-acoustic model

- Earpiece Model (Fixed)

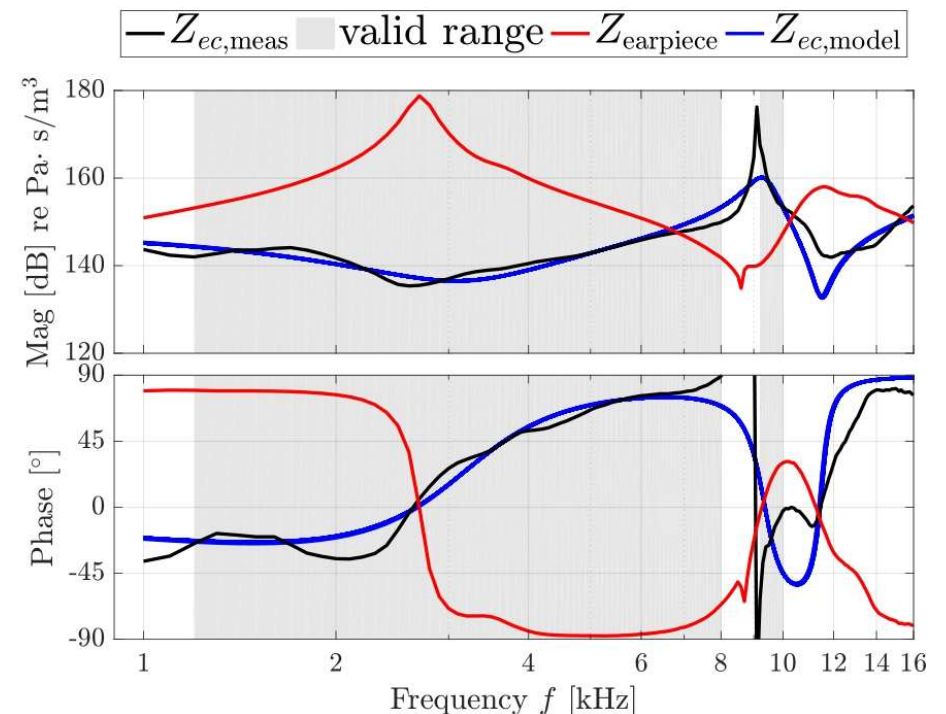
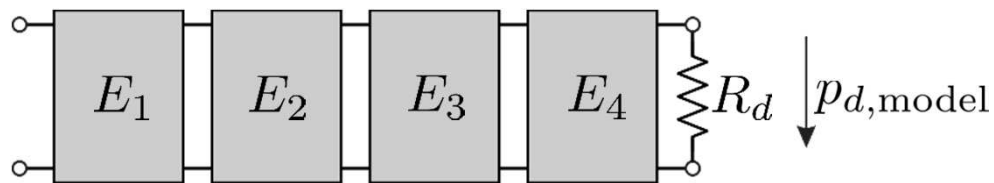


[Vogl and Blau 2019, JASA]

Parameter optimization:
minimize difference
between all 4 measured
and modeled transfer
functions

2. Electro-acoustic model

- Ear Canal Model (Individualized)



Parameter optimization (4 radii, 1 length, 1 resistive load) by minimizing the difference between measured and modeled ear canal (Nelder-Mead simplex optimization procedure):

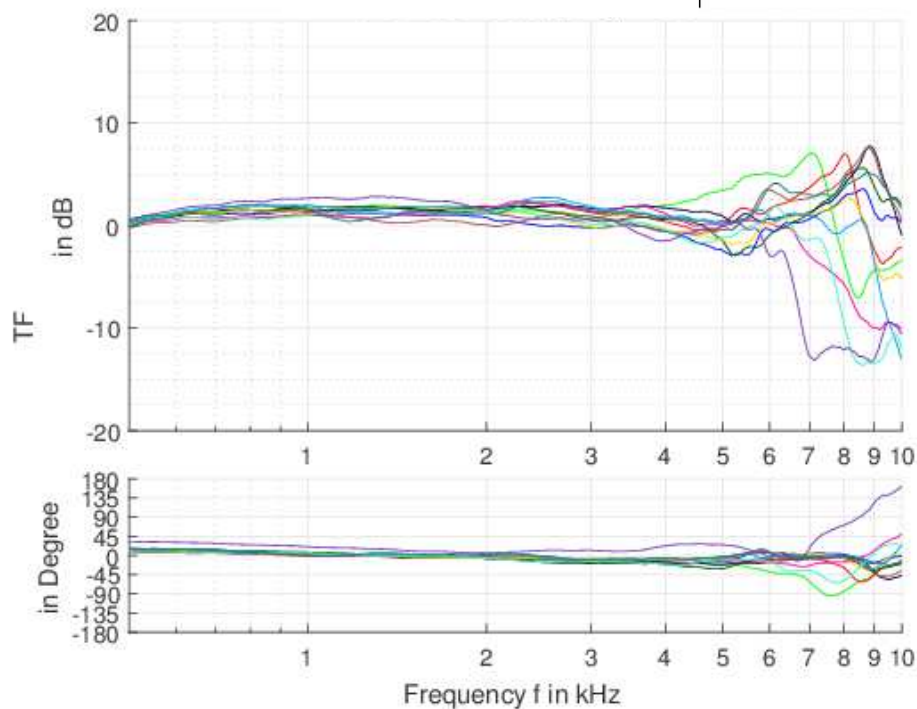
$$J(p) = \sum_{f_{\text{valid}}} (db(Z_{ec,\text{meas}}) - db(Z_{ec,\text{model}}(p)))^2 + 10 \cdot (\arg(Z_{ec,\text{meas}}) - \arg(Z_{ec,\text{model}}(p)))^2$$

2. Electro-acoustic model

- Evaluation (sound pressure at ear drum) for 12 subjects

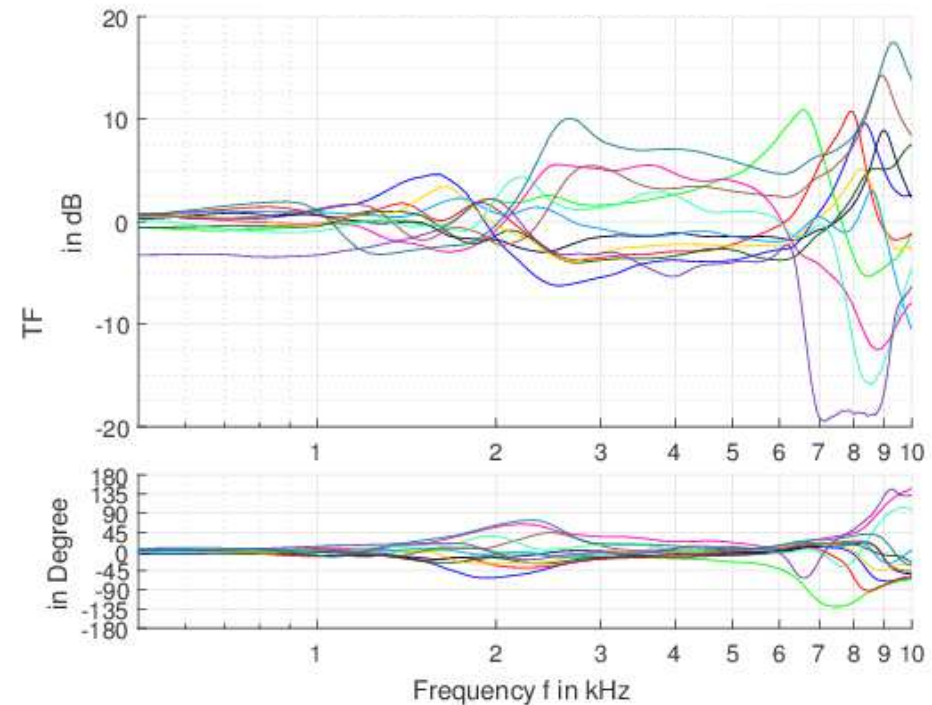
$p_{d,Model}$ (i.e. individualized)

$p_{d,Probe Tube Meas}$



$p_{d,from average correction of p1}$ (i.e. non-individualized)

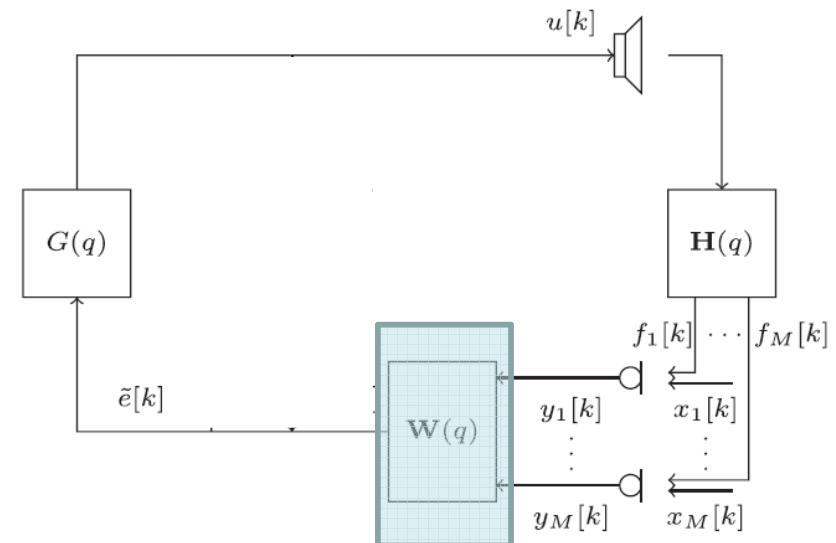
$p_{d,Probe Tube Meas}$



accurate prediction of sound pressure at ear drum possible using individualized electro-acoustic model up to about 6 kHz

3. Acoustic feedback cancellation

- **Several approaches** for acoustic feedback cancellation in hearing devices:
 1. Feedforward suppression
 2. Adaptive feedback cancellation (e.g., prediction error method)
 3. **Spatial filtering methods** exploiting multiple microphones
- **Approach:** fixed beamformer steering spatial null towards position of hearing aid receiver → theoretically perfect feedback cancellation possible
- Similar principle possible with **multiple receivers** (active feedback cancellation)



3. Acoustic feedback cancellation

- **Approach:** reduce acoustic feedback in the vent microphone by steering a (robust) spatial null towards the hearing aid receiver
- Perfect feedback cancellation if $\mathbf{H}^T(q)\mathbf{W}(q) = 0$
- **Different cost functions to design fixed beamformer:**
 - Requires (multiple) measurements of acoustic feedback paths
 - Additional constraint to preserve incoming signal

Optimization Criteria

- Residual feedback power (LS):

$$\min_{\mathbf{w}} \sum_{i=1}^I \|\mathbf{H}_i^T \mathbf{w}\|_2^2$$

- Maximum stable gain (MM):

$$\min_{\mathbf{w}} \max_{i, \omega_n} |\mathbf{H}_i^H(\omega_n)\mathbf{W}(\omega_n)|$$

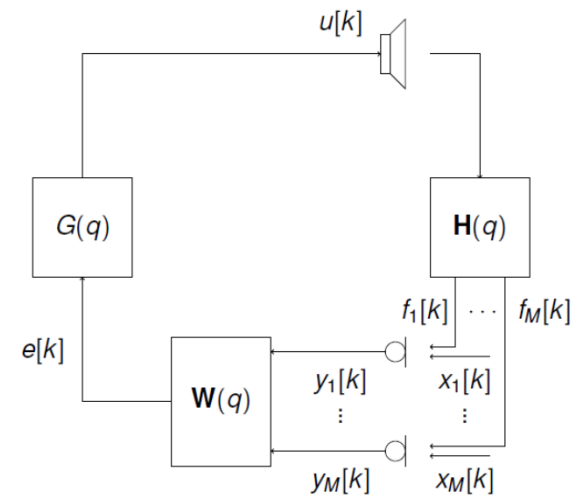
Constraints

- Fixed delay:

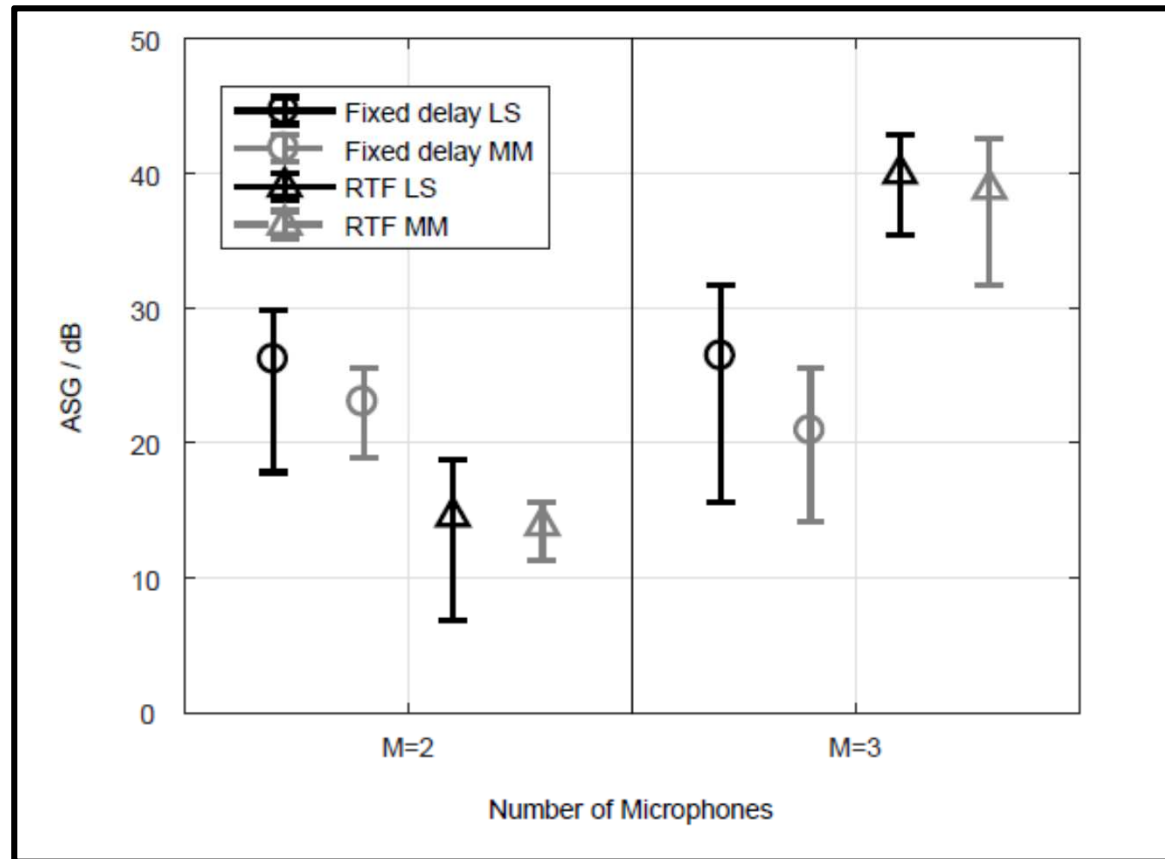
$$\mathbf{w}_{m_0} = [0 \dots 0 \ 1 \ 0 \dots 0]^T$$

- Relative transfer function (RTF):

$$\mathbf{D}_{m_0} \mathbf{w} = [1 \ 0 \dots 0]^T$$



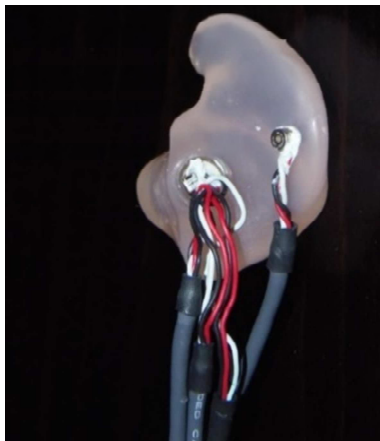
3. Acoustic feedback cancellation



Proposed fixed beamformer allows for robust reduction of acoustic feedback of up to 40dB

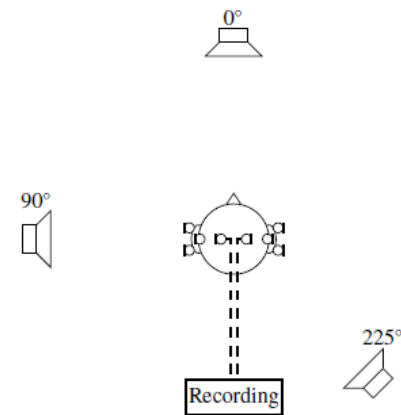
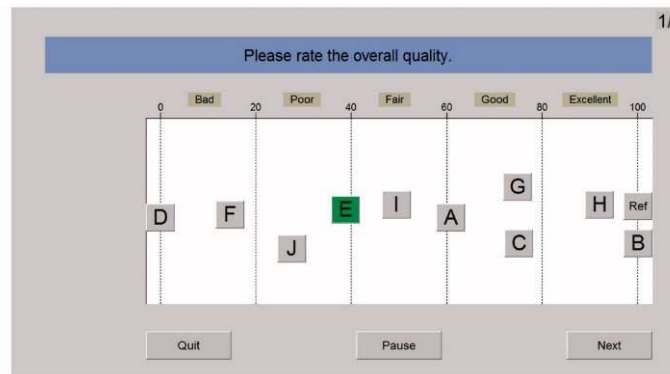
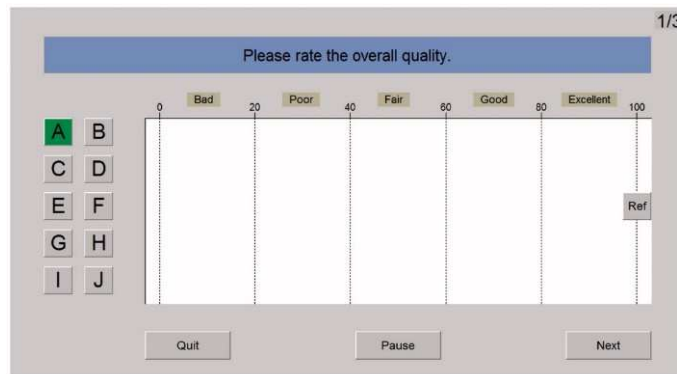
Real-time implementation

- Custom prototype
- RME Fireface UCX
- Algorithms implemented on Master Hearing Aid (MHA) run on Intel NUC PC
- Input-Output latency of 6.5 ms



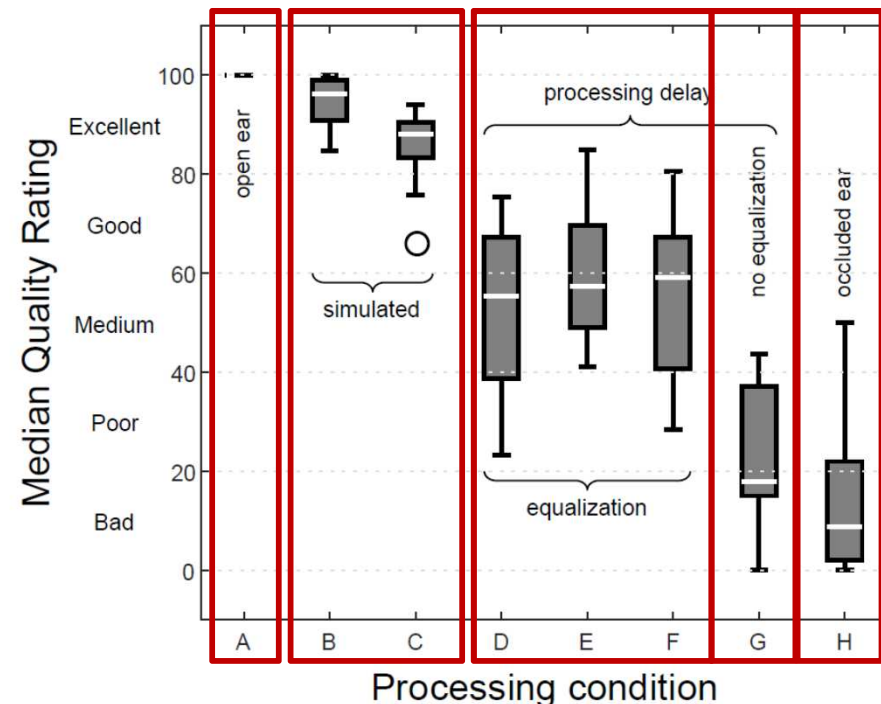
Subjective Quality Evaluation

- **Subjects:** N=15 self-reported normal-hearing
- **Task:** Evaluate overall quality compared to open ear in a MUSHRA-like framework
- **Stimuli:** Pre-recorded signals using KEMAR placed in varechoic lab presented over Sennheiser HD650 headphones



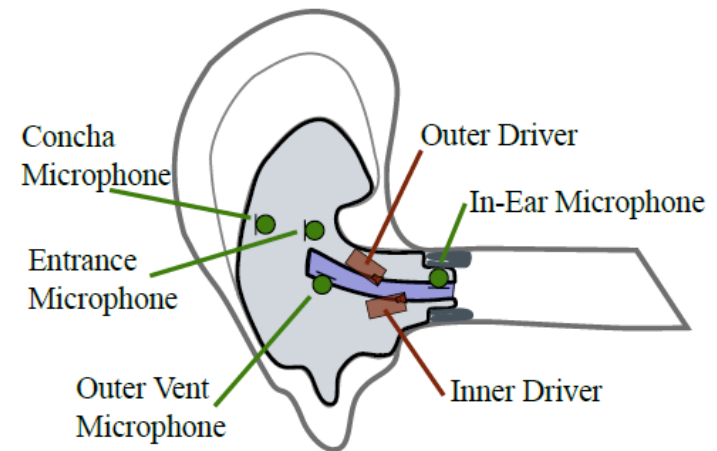
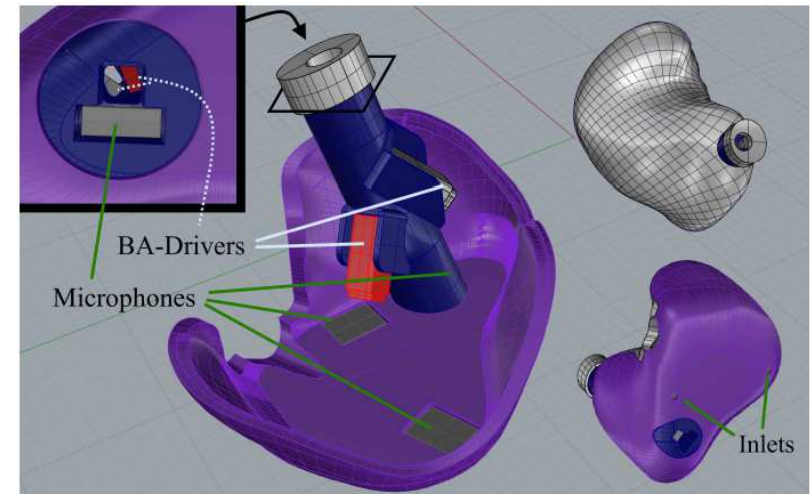
Subjective Quality Evaluation

- **Influence of Processing condition:**
 - Equalization significantly improves quality compared to no equalization
 - Target definition very similar quality compared to open ear
 - Processing delay is most crucial limiting factor (comb filtering effects)
 - Absolute ratings have to be interpreted with care (direct comparison with open ear in practice difficult)



Novel Hardware Design

- One-size-fits-all design: fits about 90% of human ears
- Vent: **2 microphones, 2 receivers**
- Concha: **2 microphones**
- Two versions: vented + closed
- **Available soon at InEar/Hoertech**



[Denk et al., AES Conference Headphone Technology, 2019]

Conclusion

- **Acoustically transparent hearing device:**
 - Custom earpiece with multiple integrated microphones and receivers
 - Allows for individualized sound pressure equalization and beamforming for acoustic feedback cancellation
 - **Transparency mode almost indistinguishable from open ear canal in blind comparison**
 - **Comb-filtering effects are the crucial limiting factors**
 - **Robust ASG improvement of up to 40 dB using fixed beamformer**
- **Real-time demonstrator available**

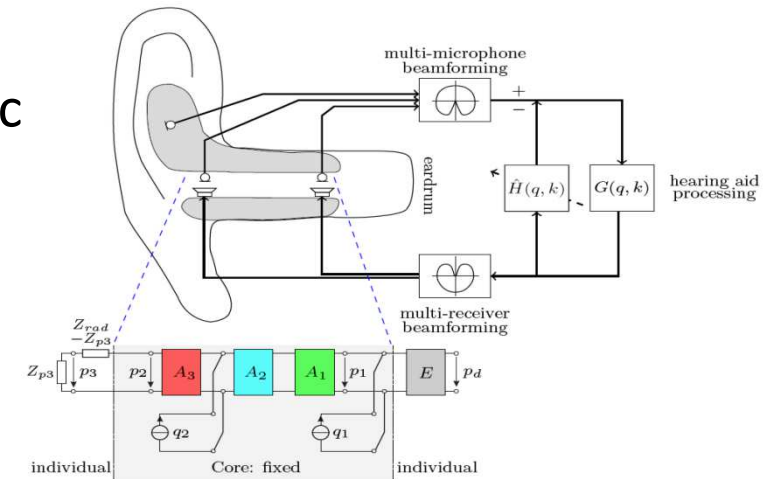


Current / Next steps

- **Sound pressure equalization:**
 - Integration of *individualized* electro-acoustic model (ear canal)
 - Improve calibration routine (not requiring additional equipment)
 - Reduce latency to avoid comb filtering

- **Combined solutions for equalization and feedback cancellation** (exploiting multiple microphones and receivers)

- Integration with **active noise and occlusion control**



Acknowledgments / references



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