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Treatment of Age-Related Hearing Loss Alters Audiovisual Integration and Resting-State Functional Connectivity: A Randomized Controlled Pilot Trial

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1 **1. Title: Treatment of age-related hearing loss alters audiovisual integration**
2 **and resting-state functional connectivity: A randomized controlled pilot**
3 **trial**

4
5 **2. Abbreviated Title:** Hearing aid fitting in age-related hearing loss

6
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21 Designed research: all authors contributed to the study design and experimental set-up

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51

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59

60 **Treatment of age-related hearing loss alters audiovisual integration**
61 **and resting-state functional connectivity: A randomized controlled**
62 **pilot trial**

63 **Abstract**

64 Untreated age-related hearing loss increases audiovisual integration and impacts resting state
65 functional brain connectivity. Further, there is a relation between crossmodal plasticity and
66 audiovisual integration strength in cochlear implant patients. However, it is currently unclear
67 whether amplification of the auditory input by hearing aids influences audiovisual integration and
68 resting state functional brain connectivity. We conducted a randomized controlled pilot study to
69 investigate how the McGurk illusion, a common measure for audiovisual integration, and resting
70 state functional brain connectivity of the auditory cortex are altered by six-month hearing aid use.
71 Thirty-two older participants with slight-to-moderate, symmetric, age-related hearing loss were
72 allocated to a treatment or waiting control group and measured one week before and six months
73 after hearing aid fitting with functional magnetic resonance imaging. Our results showed a statistical
74 trend for an increased McGurk illusion after six months of hearing aid use. We further demonstrated
75 that an increase in McGurk susceptibility is related to a decreased hearing aid benefit for auditory
76 speech intelligibility in noise. No significant interaction between group and time point was obtained
77 in the whole brain resting state analysis. However, a ROI-to-ROI analysis indicated that hearing aid
78 use of six months was associated with a decrease in resting state functional connectivity between the
79 auditory cortex and the fusiform gyrus and that this decrease was related to an increase of perceived
80 McGurk illusions. Our study, therefore, suggests that even short-term hearing aid use alters
81 audiovisual integration and functional brain connectivity between auditory and visual cortices.

82 **Significance Statement**

83 In this study we showed that first time hearing aid use of six months was related to a decrease in
84 resting state functional connectivity between the auditory cortex and the fusiform gyrus. The
85 decreased connectivity was associated with an increase in perceived McGurk illusions. Further, this
86 increase in McGurk illusions was correlated with decreased hearing aid benefit in auditory speech in
87 noise intelligibility. Our study therefore suggests that hearing aid fitting impacts functional
88 connectivity between auditory and visual regions and audio-visual integration (susceptibility to the
89 McGurk illusion). Further our results suggest, that an increased McGurk susceptibility seems to
90 inhibit the beneficial effect of the hearing aid when tested in auditory only conditions.

91 **Key words**

92 Hearing loss, Hearing aid use, fMRI, functional connectivity, McGurk illusion

93

94 **1. Introduction**

95 One of the most prevalent chronic disorders in older adults is age-related hearing loss (presbycusis) -
96 a form of bilateral sensorineural hearing loss that is caused by damage to the cochlea or the auditory
97 nerve and predominantly affects high frequencies. One of the primary treatments for presbycusis is
98 amplification of the auditory input through hearing aids. The use of hearing aids is associated with
99 self-reported improvements in communication due to increased speech clarity (Karawani et al.,
100 2018), improved speech perception and decreased listening effort (Sarant et al., 2020). Hence, there
101 is a growing interest on the beneficial effects of hearing aid use on brain and cognition in age-related
102 hearing loss (Amieva and Ouvrard, 2020; Lin, 2011). Randomized controlled studies with hearing aid
103 fittings are, however, limited.

104 Presbycusis is often associated with an increased cross-modal plasticity referring to an increased
105 neural activity in the auditory cortex when processing visual stimuli. Although mainly described in
106 deafness (e.g. Lambertz et al., 2005), crossmodal plasticity has also been shown in slight-to-
107 moderate age-related hearing loss (Campbell and Sharma, 2013; 2014). Furthermore, evidence for
108 increased functional coupling of the auditory cortex is provided by research in deaf and cochlear
109 implant patients (Chen et al., 2017; Kral et al., 2016) as well as in hard-of-hearing individuals
110 (Puschmann and Thiel, 2017). Shiell and colleagues (2015) found a decrease in audiovisual functional
111 connectivity with more years of hearing aid use in early-deaf individuals. Further, a reversal of
112 auditory cross-modal reorganization assessed by cortical visual evoked potentials (Glick and Sharma,
113 2020) and an increased frontal cortex resting state functional connectivity has recently been
114 identified after six months of hearing aid treatment (Ponticorvo et al., 2021).

115 Previous studies also revealed that hard-of-hearing participants perceived the McGurk illusion
116 significantly more often than normal-hearing individuals (Gieseler et al., 2020; Rosemann and Thiel,
117 2018; Stropahl and Debener, 2017). The McGurk illusion refers to an incongruent audiovisual
118 presentation of syllables (auditory 'ba' paired with visual 'ga') that may lead to the fused percept of a
119 third syllable ('da') and is often used to investigate audiovisual integration of speech sounds

120 (MacDonald and McGurk, 1978; McGurk & MacDonald, 1976). Increased McGurk illusion perception
121 in cochlear implant users was related to crossmodal plasticity in the auditory cortex (Stropahl and
122 Debener, 2017). Moreover, increased McGurk illusions were correlated with better audiovisual
123 speech in noise perception (Gieseler et al., 2020; Grant and Seitz, 1998), hence those changes seem
124 to be meaningful for speech comprehension in age-related hearing loss. Thus, although crossmodal
125 plasticity was mostly seen as maladaptive as it might interfere with the clinical benefit of a cochlear
126 implant or a hearing aid (Sandmann et al., 2012), there seem to be adaptive processes aiding in
127 speech perception in cochlear implant patients as well (Stropahl and Debener, 2017).

128 Increased task-modulated functional connectivity between auditory and visual cortex – when
129 comparing incongruent (McGurk) with congruent audiovisual stimuli – was found in hard-of-hearing
130 compared to normal-hearing participants (Rosemann et al., 2020). Moreover, increased McGurk
131 illusions were correlated with decreased resting state functional connectivity between auditory and
132 motor regions in mild to severe hard-of-hearing individuals (Schulte et al., 2020). Thus, previous
133 research provided evidence for changed audiovisual integration abilities in age-related hearing loss,
134 and functional connectivity alterations in the auditory cortex associated with the McGurk illusion.
135 However, how hearing aid fitting affects, or even reverses, these changes has not been investigated
136 so far.

137 Therefore, the aim of the current study was to investigate how the McGurk illusion and resting state
138 functional connectivity are altered by hearing aid use in age-related hearing loss. For this purpose,
139 we conducted a pilot randomized controlled hearing aid fitting study in which 16 hard-of-hearing
140 participants were measured one week before and six months after first fitting of a hearing aid
141 (treatment group). The other 16 hard-of-hearing participants were not equipped with a hearing aid
142 and were measured twice at an interval of six months as well (waiting control group). We expected a
143 decrease in the number of McGurk illusions in the treatment compared to the control group
144 (Gieseler et al., 2020; Rosemann and Thiel, 2018; Stropahl and Debener, 2017). Moreover, we
145 hypothesized a decrease in functional coupling of the auditory cortex to visual areas after hearing aid

146 fitting (Chen et al., 2017; Kral et al., 2016; Puschmann and Thiel, 2017; Shiell et al., 2015). We further
147 expected changes in McGurk illusion perception to be related to changes in functional connectivity
148 between auditory cortex and visual as well as motor brain regions (Rosemann et al., 2020; Schulte et
149 al., 2020).

150 **2. Methods**

151 **2.1 Participants**

152 We screened n=163 participants between 60 and 80 years of age with self-reported hearing loss and
153 no prior hearing aid experience. Inclusion criteria were a slight-to-moderate, symmetric, age-related
154 hearing loss defined as better-ear pure-tone averages (PTA) across the frequencies 0.5, 1, 2 and 4
155 kHz between 18 and 56 dB HL (cf. WHO) with PTA differences between left and right ear smaller than
156 15 dB HL and air-bone gaps no larger than 10 dB HL. In addition, participants had to be right-handed,
157 German native speakers, have normal or corrected-to-normal vision and no current or previous self-
158 reported neurological or psychiatric disorders, including tinnitus. Furthermore, participants were
159 screened for dementia and excluded in case of suspected dementia (age normed DemTect scores of
160 > 8; Kalbe et al., 2004). Seventy-one participants were initially included in the study, of whom n=58
161 completed behavioral testing. Subjects with no MRI contraindications were invited for an additional
162 MRI scan. In this paper, we report data of n=32 participants with complete behavioral and MRI data.
163 Of those, n=16 participants were allocated to the treatment group and n=16 to the waiting control
164 group.

165 Approval for the study was obtained from the local ethics committee of the University of Oldenburg
166 (no 25/2018) and the study was carried out in accordance with the Declaration of Helsinki as well as
167 the EU General Data protection Regulation. All subjects signed a written informed consent form and
168 were paid for participation.

169 **2.2 Treatment and Control Group**

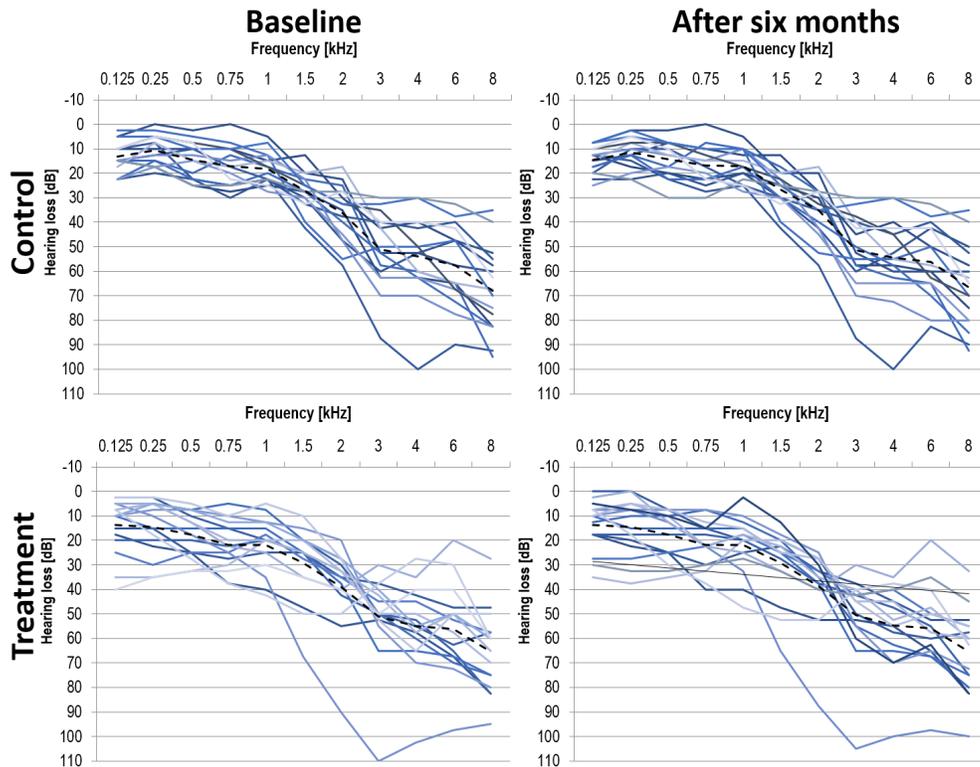
170 Treatment and control group were stratified with respect to hearing impairment (PTA), age and
171 cognitive performance (as assessed by the dementia screening test DemTect; Kalbe et al., 2004). The
172 mean age and hearing impairment of the participants at screening was 71.2 ± 5.1 years and $28.5 \pm$
173 9.6 dB HL (range 20.0-56.3 dB HL) in the treatment group and 70.0 ± 4.7 years and 27.2 ± 7.5 dB HL
174 (range 17.5-45.0 dB HL) in the control group, respectively.

175 Participants in the treatment group were fitted with bilateral Signia Pure 7Nx/px hearing aids with M-
176 receivers and click dome (semi-) open coupling by trained acousticians at the Hörzentrum Oldenburg
177 GmbH. For the fitting formula, NAL-NL2 with fixed pinna-preserving Omni-Mode and default noise
178 reduction was set as default. For all fittings, in-situ measurements were done. If the participants
179 were uncomfortable with the default setting, the acousticians allowed for little fine-tuning to avoid
180 drop-outs (as much as needed, as little as possible) starting with the simplest approach by i) trying to
181 master gain, ii) frequency-dependent gain, iii) compression and iv) allowing for additional noisy-
182 environment program only if the subject explicitly required it. All changes were documented. The
183 participants were instructed to wear their hearing aids daily for at least 6 hours and gave their
184 written consent to log the data of the hearing aid. The waiting control group was offered a hearing
185 aid fitting by the Hörzentrum Oldenburg GmbH after the study was completed.

186 **2.3 Experimental Procedure**

187 All participants underwent behavioral and MRI measurements one week prior and six months after
188 potential hearing aid fitting. Participants in the treatment group were additionally assessed one
189 month after the fitting (data not reported).

190 The individual pure-tone audiograms for the baseline and six-month post assessment are shown in
191 Figure 1. Note that there were no changes in the PTA for neither the control nor the treatment group
192 after six months.



193

194 **Figure 1:** Individual pure-tone audiograms for participants in the control group (top panels) and
195 treatment group (bottom panels) at baseline (left panels) and after six months (right panels). Mean
196 across both ears as well as group averages (dashed line)

197

198

199 **2.4 Behavioral measurements**

200 Behavioral measurements included a pure-tone audiometry, cognitive screening (Montreal Cognitive
201 Assessment: MOCA, Nasreddine et al., 2005; DemTect, Kalbe et al., 2004) and audiovisual tasks
202 (McGurk task, sound induced flash illusion, audiovisual speech in noise intelligibility task described in
203 Llorach et al., 2019). We focused only on the McGurk task, the audio-visual speech in noise
204 intelligibility task and resting state measurements.

205 Pure tone audiometry was performed in a soundproof chamber using air conduction pure-tone
206 audiometry for the frequencies 125, 250, 500, 1000, 2000, 4000, 6000 and 8000 Hz.

207 The McGurk task was performed in a soundproof chamber, approximately 60 cm in front of the
208 screen. The stimuli were presented on a 17" Iiyama ProLite T 1731 SR-B1 monitor (spatial resolution:
209 1280 × 1024 pixels; luminance: 200 cd/m²; refresh rate: 60 Hz) and via Sennheiser HDA200
210 headphones delivered by the USB audio interface RME Fireface UC ([http://www.rme-](http://www.rme-audio.de/en/products/fireface_uc.php)
211 [audio.de/en/products/fireface_uc.php](http://www.rme-audio.de/en/products/fireface_uc.php)). Stimulus presentation was controlled by Presentation®
212 software (Version 18.2, Neurobehavioral Systems, Inc., Berkeley, CA, www.neurobs.com). The task
213 consisted of typical McGurk syllables that were presented as either auditory-only, visual-only,
214 audiovisual congruent or audiovisual incongruent conditions (the McGurk illusion). We used the
215 syllables 'ga' and 'ba', that commonly lead to the fused percept 'da' when presented as incongruent
216 stimuli (visual 'ga' with auditory 'ba'). These stimuli were a subset of syllables that were recorded in
217 the Department of Media Production at the University of Oldenburg and consisted of video and
218 audio files of a male speaker articulating the different syllables in front of a dark grey background
219 (Rosemann and Thiel, 2018). The syllables 'ga' and 'ba' were presented in either auditory-only or
220 visual-only as well as audiovisual congruent conditions in addition to the incongruent presentation of
221 the McGurk illusion condition. The audiovisual conditions (both congruent and incongruent) were
222 presented either synchronously (stimulus onset asynchrony (SOA) of 0 ms) or asynchronously (SOAs
223 of 70-420 ms in steps of 50 ms). The different SOAs were used to assess the temporal domain in
224 which the McGurk illusion is most likely perceived. In these asynchronous presentations, the auditory
225 stimulus followed the visual stimulus. Each SOA was repeated ten times and unimodal conditions
226 were presented five times. Each trial started with a 1000 ms blank screen followed by a jittering 600–
227 800 ms black fixation cross on a white background. Then, the video/audio files were presented. Last,
228 the response display with the syllables ('ba', 'ga', 'da') as response options (labeled as 1, 2, 3; three-
229 alternative forced choice) was presented. Participants were instructed to report what they heard.
230 The response (respective number from the response display) was given orally to the experimenter

231 and the next trial only started after the experimenter had entered the response. The total duration
232 of the McGurk task was 20 minutes. The auditory stimuli in the McGurk task were presented via
233 headphones and the loudness was adjusted individually for each participant prior to the test and
234 training session (in steps of 1 dB to medium loudness starting at 65 dB SPL). The mean medium
235 loudness level of the auditory stimuli was 68 dB for the baseline measurement and 69 dB for the six
236 months re-test measurement in the control group and 69 dB and 71 dB in the treatment group,
237 respectively. Importantly, the participants of the treatment group were measured unaided, i.e.,
238 without their hearing aids, at the re-test assessment to assess potential general changes that are not
239 associated with specific hearing aid settings.

240 The auditory and audiovisual speech intelligibility tasks were the Oldenburg Sentence Test
241 (Oldenburger Satztest, OLSA; Wagener et al., 1999a, b, c) and the corresponding audiovisual version
242 of it (please find a detailed description in Llorach et al., 2019). The OLSA consists of five-word
243 sentences and the task for the participants is to repeat what they heard. Each testing condition
244 involved 20 sentences each in fluctuating background noise (ICRA4-250). The presentation of the
245 conditions was randomized (auditory only and audiovisual conditions as well as aided and unaided
246 conditions after 6 months in the treatment group). Before the testing, each participant conducted a
247 training of ten sentences in each condition. For each condition, the corresponding 80%-speech
248 reception thresholds were determined, referring to the signal-to-noise ratio that yields 80%
249 intelligibility based on performance (word scoring). An adaptive procedure was applied (fixed
250 background noise presentation level at 65 dB SPL; the target speech was adaptively varied based on
251 the previous answer, starting at 0dB SNR).

252 **2.5 MRI measurements**

253 The MRI measurements took place on a separate day in close proximity to the behavioral
254 assessment. Imaging data were acquired on a 3T whole-body Siemens Magnetom Prisma MRI
255 machine with a 20-channel head coil. Resting state fMRI data were recorded with an ascending echo

256 planar imaging sequence (320 T2*-weighted volumes, TR = 1500 ms, TE = 30 ms, voxel size = 2.2 x 2.2
257 x 3 mm, 25 slices). Participants had to fixate a white fixation dot that was presented on a black
258 screen. The fixation dot was presented with the Presentation® software (Version 18.3,
259 Neurobehavioral Systems, Inc., Berkeley, CA, www.neurobs.com) via a projector behind the bore of
260 the MRI (DATAPixx2, VPixx Technologies Inc.). Anatomical images were acquired with a 3-D T1-
261 weighted sequence (MP-RAGE, TR = 2000, TE = 2.07, flip angle = 9 °, voxel size = 0.75mm, field of
262 view =240x240, 224 sagittal slices).

263 **2.6 Analysis of Behavioral Data**

264 To assess general task performance in the McGurk task, we computed mean performance measures
265 (% correct) for audiovisual congruent conditions (across all SOAs), auditory-only and visual-only
266 conditions for each participant. Potential differences in general task performance between groups at
267 baseline and after six months were assessed by repeated-measures GLM on the percent of correctly
268 identified syllables with condition (audiovisual congruent/auditory/visual) as within-subject factor
269 and group (treatment/control) as between-subject factor.

270 To assess audiovisual integration, the incongruent McGurk (illusion) trials underwent a detailed
271 analysis to investigate potential group differences in the susceptibility to the McGurk illusion (defined
272 as fusion reports 'da'). Since the response options in the incongruent condition can be either the
273 auditorily-presented syllable ('ba'), the visually-presented syllable ('ga') or the fused illusion percept
274 ('da'), a first analysis focused on the percent for each response option across SOAs using a repeated-
275 measures GLM with group as between- and response as within-subject factors (for baseline and after
276 six months). A second analysis focused on the fused percept as a function of SOA using a repeated-
277 measures GLM with group as between- and SOAs within-subject factors (for baseline and after six
278 months).

279 Two post-hoc correlation analyses were performed to investigate i) whether the McGurk
280 susceptibility is a valid measure of audiovisual integration (correlation of McGurk illusions with

281 audiovisual speech intelligibility) and ii) whether the change in the McGurk susceptibility is a positive
282 or negative outcome for speech intelligibility (correlation of the change in McGurk susceptibility
283 between baseline and retest assessment with benefit of aided versus unaided speech intelligibility).

284 **2.7 Analysis of MRI Data**

285 Resting state functional connectivity data were analyzed with the Statistical Parametric Mapping
286 software package (SPM12, Wellcome Department of Imaging Neuroscience, London, UK) based on
287 Matlab 2016b and the CONN toolbox (Whitfield-Gabrieli and Nieto-Castanon, 2012). Images were
288 pre-processed in SPM including spatial realignment estimation, slice timing correction and co-
289 registration. Next, a normalization to the Montreal Neurological Institute space using parameters
290 obtained from segmentation of the anatomical T1-weighted image and spatial smoothing using a
291 Gaussian kernel with a full width at half maximum of 8 mm was applied. After normalization, data
292 processing proceeded in CONN: remaining physiological and movement artefacts were removed by
293 linear regression. The BOLD signal from white matter and cerebrospinal fluid as well as realignment
294 parameters were used for denoising. Subsequently, a band-pass filter (0.008-0.9 Hz) and linear
295 detrending was applied. First-level analyses revealed Fisher-transformed correlation coefficients for
296 each subject. Individual connectivity maps were subsequently entered into two second level analyses
297 to identify treatment-dependent changes in resting state connectivity over time. The first analysis
298 was a whole brain analysis with seed in the auditory cortex (seed-to-voxel analysis), the second
299 analysis was a region of interest (ROI) analysis (ROI-to-ROI) focusing on connectivity changes
300 between 1) auditory cortex and fusiform face area and 2) the auditory cortex and M1 lip area).

301 The main seed in this study was positioned in the left and right Brodmann areas 41 and 42 (defined
302 using the Automated Anatomical Labeling (AAL) ROI-Library within the WFU Pickatlas). This pooled
303 seed was used for the whole-brain analysis and for the ROI-to-ROI analysis. The fusiform gyrus was
304 used as a ROI because of its involvement in face processing (Kanwisher and Yovel, 2006; Kanwisher et
305 al., 1997) and its neural activity during the presentation of McGurk syllables (Rosemann et al., 2020).

306 Further, coupling between auditory and visual areas was shown to be increased in deafness and
307 hearing impairment (Chen et al., 2017; Kral et al., 2016; Puschmann and Thiel, 2017; Shiell et al.,
308 2015). We further used the M1 lip area as a ROI because its neural activity was shown to be related
309 to the McGurk illusion in healthy volunteers (Murakami et al., 2018). Further, studies in age-related
310 hearing loss demonstrated increased neural activity in motor cortex but decreased coupling between
311 auditory and motor regions with increased McGurk illusion responses (Rosemann et al., 2020;
312 Schulte et al., 2020). The ROI in the left and right fusiform gyrus was provided by the atlas
313 implemented in CONN. The ROI in the left M1 lip area constitutes a sphere of 8 mm radius around
314 the coordinates ($x=-44$, $y=-11$, $z=34$) provided by Murakami et al. (2018).

315 In order to assess changes in functional resting state connectivity of the auditory cortex to the rest of
316 the brain after hearing aid fitting, we computed an interaction between group (treatment/control) x
317 measurement time point (baseline/after six months) with a height threshold of $p < 0.001$ and a
318 cluster corrected threshold of $pFWE < 0.05$. For the ROI analysis, connectivity values between 1) the
319 auditory cortex and the fusiform gyrus as well as 2) the auditory cortex and the M1 lip area (ROI-to-
320 ROI analyses) were extracted. Changes in connectivity values from auditory to fusiform and the M1
321 lip area between measurement time points were compared across groups (using repeated-measures
322 ANOVAs) and correlated with changes in the McGurk illusion (Pearson correlation). These analyses
323 were computed in JASP (JASP Team, 2020; Version 0.14.1).

324

325 **3. Results**

326 **3.1 Hearing aid use**

327 Although all participants were instructed to wear the hearing aid for at least 6 hours per day, the
328 average daily wearing period ranged from 1 hour to 12 hours, with a median of 7 hours. Given the
329 small number of subjects we refrained from excluding three subjects who had been wearing their

330 hearing aids for less than 5 hours per day as none of them had been detected as an outlier during the
331 analysis.

332 **3.2 Behavioral Results**

333 The mean performance values for both groups and measurements for audiovisual congruent,
334 auditory-only, and visual-only conditions are presented in Table 1. Individual data for all participants
335 is shown in Figure 2 (upper panel). The repeated-measures GLM revealed a significant main effect of
336 *condition* at both baseline and re-test assessment after six months [baseline: $F_{(2,60)}=34.49$, $p_{\text{adj}}<0.001$,
337 $GG_{\text{eps}}=0.76$, $\eta^2p=0.54$; after six months: $F_{(2,60)}=44.75$, $p_{\text{adj}}<0.001$, $GG_{\text{eps}}=0.78$, $\eta^2p=0.61$], whereas
338 neither the main effect of *group* nor the *group x condition* interaction yielded significance. Hence,
339 general task performance did not differ between the treatment and control group for neither
340 baseline nor re-test assessment. Post-hoc comparisons showed that both groups performed
341 significantly better in both the auditory-only and audiovisual congruent condition than in the visual-
342 only condition (all $p_{\text{adj}}<0.001$).

343

344 **Table 1: Mean values (\pm standard deviation) for performance in the McGurk task.** All conditions
 345 except the incongruent McGurk illusion condition are presented for the baseline as well as re-test
 346 (after six months) measurements

Condition	Measurement	Control group	Treatment group
Audiovisual congruent trials: % correct	Baseline	87.9 \pm 21.7	93.1 \pm 15.4
	After 6 months	90.9 \pm 16.6	97.9 \pm 3.3
Auditory-only trials: % correct	Baseline	84.4 \pm 18.6	85.6 \pm 19.3
	After 6 months	93.1 \pm 14.5	86.0 \pm 13.5
Visual-only trials: % correct	Baseline	65.0 \pm 22.8	70.0 \pm 15.5
	After 6 months	71.9 \pm 19.1	68.7 \pm 15.1

347

348 To assess changes in audiovisual integration we analysed the amount of McGurk illusions ('da'
 349 response), auditory ('ba') and visual ('ga') percepts in incongruent trials for each group at both
 350 measurement time points (response mean across SOAs shown in Table 2, individual data are shown
 351 in Figure 2, responses as a function of SOA shown in Figure 3). At baseline, the expected significant
 352 main effect of *response* was not accompanied by significant *group* - nor by significant *response x*
 353 *group* interaction effect. Across all SOAs, both groups perceived the audiovisual illusion and the
 354 auditory percept more often than the visual percept. Note, however, the large variability in both
 355 groups.

356 After six months, we again found a main effect of *response* together with a significant trend for a
 357 *response x group* interaction with a medium effect size [response: $F_{(2,60)}=23.47$, $p_{adj}<0.001$,
 358 $GG_{eps}=0.55$, $\eta^2p=0.45$; response x group: $F_{(2,60)}=2.96$, $p_{adj}=0.055$, $GG_{eps}=0.55$, $\eta^2p=0.092$]. As
 359 presented in Table 2 and visualized in Figure 2, the control group perceived the audiovisual illusion
 360 after six months almost equally often as in the baseline assessment, whereas the treatment group
 361 showed an increase in McGurk illusions after six months of hearing aid use.

362 The correlation between responses given at baseline and responses given after six months for all
 363 participants was significantly correlated for all three response options, while the correlation was
 364 stronger for the McGurk illusion ($r=0.797$, $p<.001$) and the auditory response ($r=0.778$, $p<.001$) than
 365 for the visual response ($r=0.366$, $p=0.043$).

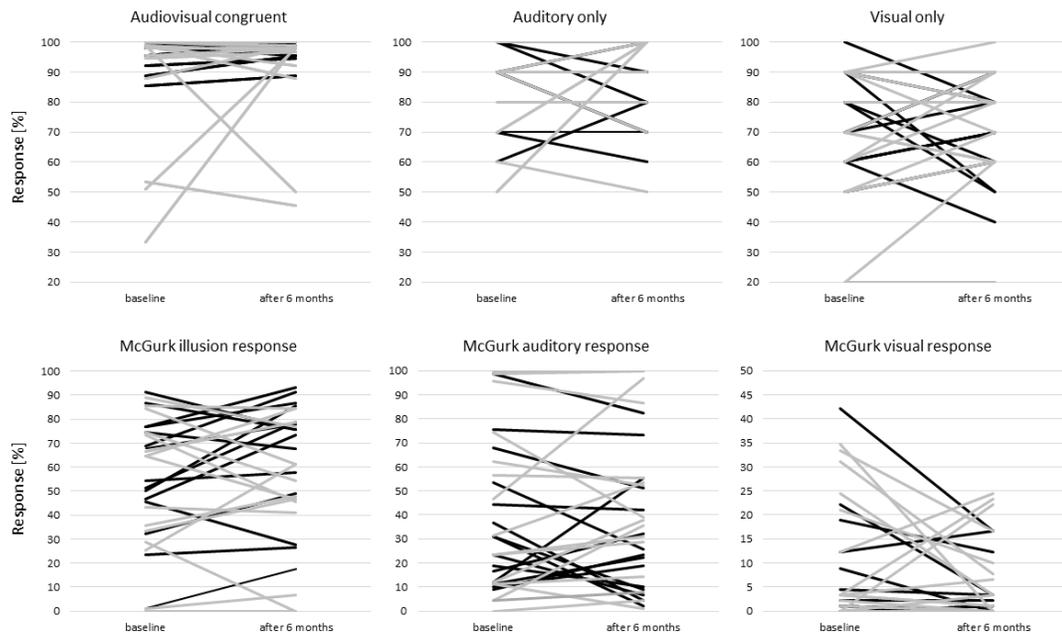
366 **Table 2: Mean values (\pm standard deviation) for performance in the McGurk audiovisual**
 367 **incongruent trials.** Percent values are shown for the three response options for the baseline as well
 368 as re-test (after 6 months) measurements [mean across all SOAs]

Condition	Measurement	Control group	Treatment group
Audiovisual incongruent trials: Illusion percept ('da')	Baseline	48.1 \pm 31.3	54.5 \pm 25.1
	Post 6 months	46.0 \pm 29.9	65.6 \pm 24.5
Audiovisual incongruent trials: Auditory percept ('ba')	Baseline	41.0 \pm 35.9	36.9 \pm 26.5
	Post 6 months	46.5 \pm 33.8	30.6 \pm 25.2
Audiovisual incongruent trials: Visual percept ('ga')	Baseline	10.9 \pm 13.3	8.6 \pm 12.4
	Post 6 months	7.5 \pm 9.1	3.8 \pm 6.1

369

370

371



372

373 **Figure 2: Individual McGurk data.** Correct responses (%) shown for the audiovisual congruent,
 374 auditory only and visual only conditions in the top panel (as in Table 1). Different responses (%) given
 375 in the McGurk illusion trials are shown in the lower panel (as in Table 2). The responses of subjects in
 376 the treatment group are shown in black and those in the control group in grey. [mean values for each
 377 participant]

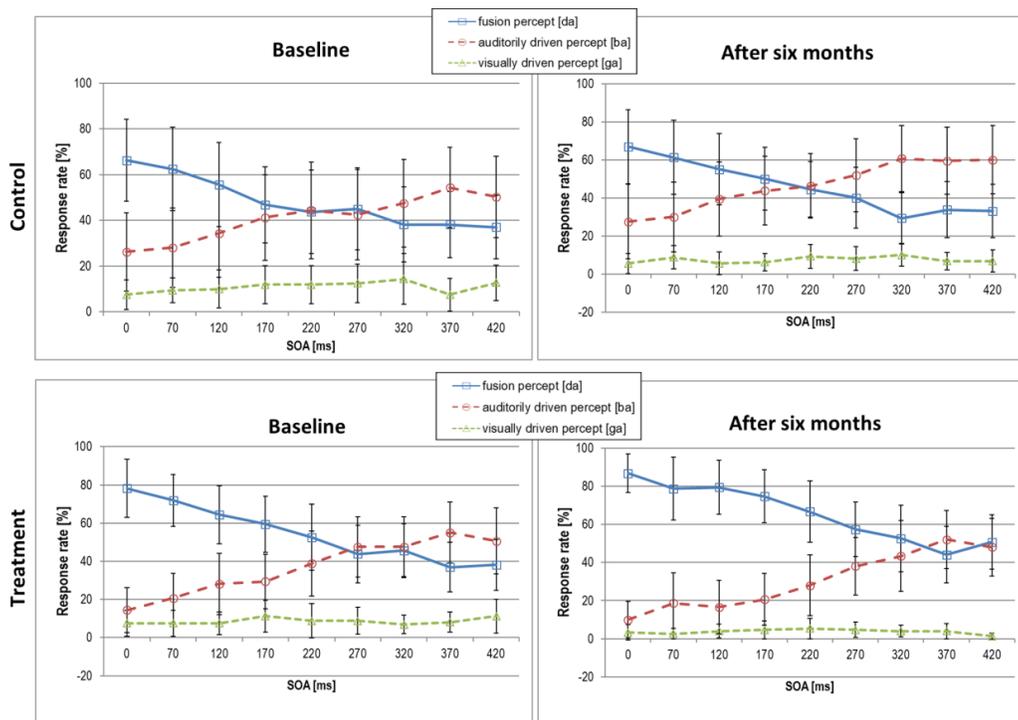
378

379 To assess potential group differences and changes in the McGurk illusion as a function of SOA, we
 380 first looked at the baseline assessment. As expected, the main effect of *SOA* was significant with
 381 decreasing illusion reports with increasing SOAs [$F_{(8,240)}=17.19$, $p_{adj}<0.001$, $GG_{eps}=0.52$ $\eta^2p=0.36$],
 382 whereas neither the main effect of *group* nor the *SOA x group* interaction were significant. Hence,
 383 although the treatment group showed slightly higher values in the amount of McGurk illusions at
 384 baseline, those differences were not statistically significant.

385 At the re-test assessment, we found a significant main effect of *SOA* together with a significant trend
 386 for a main *group* effect with a medium effect size [*SOA*: $F_{(8,240)}=18.07$, $p_{adj}<0.001$, $GG_{eps}=0.29$,

387 $\eta^2p=0.38$; group: $F_{(1,30)}=3.97$, $p=0.05$, $\eta^2p=0.12$]. The treatment group showed more McGurk illusions
 388 than the untreated peers.

389 Figure 3 shows how the amount of fusion percept decreases with increasing SOAs, i.e., the further
 390 the onsets of the lip movement and the tone are apart, the less likely they are integrated. Yet, it is
 391 not until 220 ms for the control group and 270 ms for the treatment group that the auditory percept
 392 is perceived more often than the fused percept. After six months, the treatment group shows an
 393 even more pronounced integration of visual and auditory information up to an SOAs of 320 ms.
 394 Importantly, in the treatment group, the performance in the McGurk task across the different
 395 conditions did not correlate with the mean daily wearing period of the hearing aid.



396
 397 **Figure 3: Response rate across SOAs in the audiovisual incongruent (illusion) condition of the**
 398 **McGurk task.** Data shown for the control (top panel) and treatment group (bottom panel) for the
 399 baseline assessment (right panels) and assessment after six months (left panels) [mean values \pm
 400 standard deviation]

401 Two post-hoc correlation analyses were performed to investigate i) whether the McGurk
 402 susceptibility is a valid measure of audiovisual integration and ii) whether the change in the McGurk
 403 susceptibility is a positive or negative outcome for speech intelligibility. The results for the speech
 404 intelligibility task can be seen in table 3. The treatment group was tested in an aided and unaided
 405 condition after six months. No significant differences between the two groups were obtained in the
 406 unaided measurement conditions ($p>0.1$).

407

408 **Table 3: Mean values (\pm standard deviation) for performance in speech intelligibility task in**
 409 **auditory (A only) and audiovisual (AV) conditions.** The treatment group was tested in aided and
 410 unaided conditions in the re-test measurement after six months [SNR at 80% speech intelligibility]

Condition	Measurement	Control group	Treatment Group
A only unaided	Baseline	-3.69 \pm 5.48	-3.98 \pm 6.06
	Post six months	-7.70 \pm 3.18	-7.54 \pm 3.98
AV unaided	Baseline	-10.65 \pm 5.03	-10.74 \pm 6.19
	Post six months	-14.42 \pm 3.75	-14.29 \pm 3.75
A only aided	Post six months	–	-9.21 \pm 3.83
AV aided	Post six months	–	-15.48 \pm 5.49

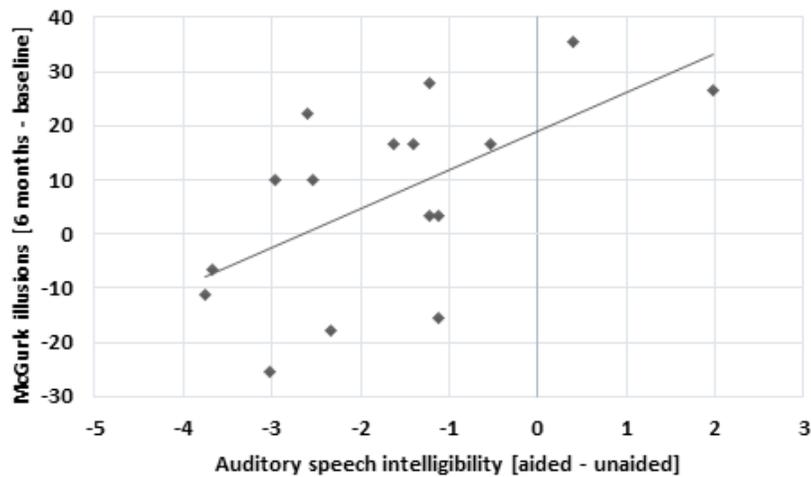
411

412 The correlational analysis between audiovisual speech intelligibility values and McGurk susceptibility
 413 at baseline showed a correlation at trend level (Pearson's $r=-0.457$, $p=0.075$), indicating better
 414 audiovisual speech intelligibility with higher number of McGurk illusions. The same correlation was
 415 not significant after six months (unaided condition, all participants). As a next step, we computed a
 416 correlational analysis for the treatment group only, evaluating the benefit of aided versus unaided
 417 measurement conditions and the change in McGurk susceptibility over time. While this analysis

418 showed a positive correlation for the auditory speech intelligibility (Pearson's $r=0.6$, $p=0.014$; Figure
419 4), this was not significant for the audiovisual speech intelligibility.

420

421 **Figure 4: Positive correlation between the difference in McGurk illusions (6 months – baseline) and**
422 **auditory speech intelligibility test conditions (aided – unaided) in the treatment group**



423

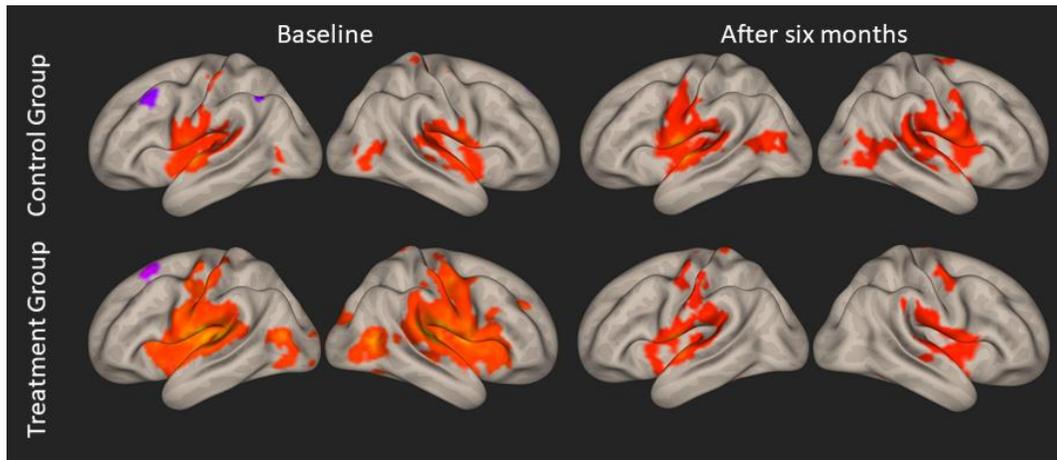
424

425 3.3 Neuroimaging Results

426 We conducted a functional connectivity analysis of the auditory cortex (left and right Brodmann
427 areas 41 and 42) to the whole brain at baseline and after six months (see Figure 5). The auditory
428 resting state network comprised areas in the occipital, temporal and parietal lobe as well as the
429 cingulate cortex and parts of the frontal cortex. Mostly, a positive correlation between neural activity
430 in these regions was obtained, however coupling with frontal areas (superior, middle and orbito-
431 frontal gyrus) and parts of the left parietal cortex (inferior parietal lobule) was negative. To assess the
432 changes in functional resting state coupling with hearing aid fitting, we computed the interaction
433 between group (treatment/control) x measurement time point (baseline/after six months). This

434 analysis did not reveal any significant results (even when the threshold was lowered to $p < 0.001$,
435 uncorrected for multiple comparisons).

436



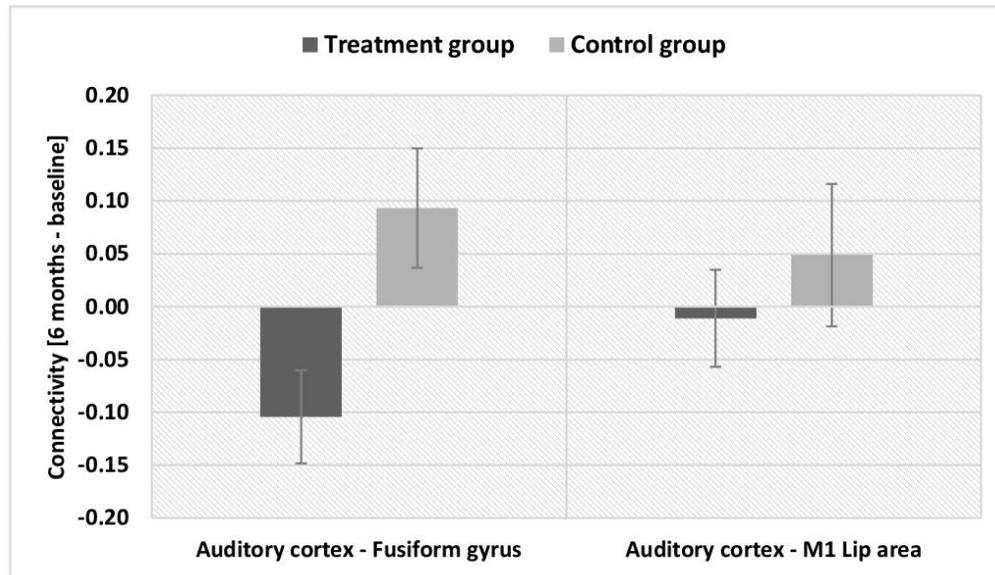
437
438

439 **Figure 5: Whole brain resting-state functional connectivity of the left and right auditory cortex (for**
440 **each measurement and each group).** Left and right hemispheres are presented on left and right side,
441 respectively. [$p < 0.05$; FWE corrected on the cluster level] Positive correlations are shown in red,
442 negative correlations are shown in purple

443

444 In the second step, we implemented a ROI analysis and extracted functional connectivity values
445 between the ROIs in the auditory cortex (left and right Brodmann areas 41 and 42) and the fusiform
446 gyrus as well as between the auditory cortex and the M1 lip area (ROI-to-ROI analysis) for each group
447 and measurement time point (baseline and after six months). The interaction between group and
448 measurement time point with respect to functional connectivity of the auditory cortex and the
449 fusiform gyrus was significant ($F_{(1,30)} = 7.566$, $p = 0.01$, $\eta^2 = 0.142$; Figure 6, left). The control group
450 showed a numeric increase coupling between auditory cortex and fusiform gyrus after six months
451 (which was however not significant), whilst the treatment group showed a significant decrease in

452 coupling between those areas. We did not obtain a significant interaction between group and
 453 measurement time point in the resting state connectivity of the auditory cortex and M1 lip area
 454 ($F_{(1,30)}=0.538$, $p=0.469$, $\eta^2=0.007$; Figure 6, right).



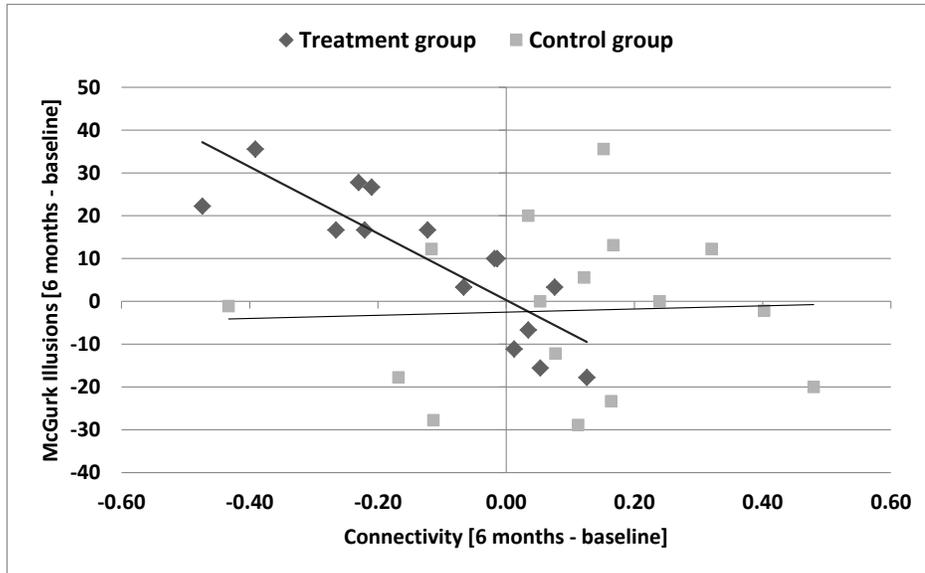
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456 **Figure 6: Change in resting-state functional connectivity between measurements at baseline and**
 457 **after six months for the two groups (ROI-to-ROI analysis).** Negative values refer to a decrease in
 458 connectivity between the respective regions after six months, positive values refer to an increase in
 459 connectivity after six months; ROIs were positioned in 1) left and right auditory cortex, 2) left and
 460 right fusiform gyrus, 3) left M1 lip area [mean values with standard error of the mean]

461

462 Importantly, this decrease in resting state functional connectivity between the auditory cortex and
 463 fusiform gyrus was correlated with an increase in reported fused McGurk percepts in the treatment
 464 group (Pearson's $r=-0.846$, $p<0.001$), but not in the control group (Pearson's $r=0.045$, $p=0.869$; Figure
 465 7). Hence, the increase in audiovisual integration after hearing aid fitting co-occurred with a
 466 reduction of functional brain connectivity between auditory and visual brain regions. The average

467 daily hearing aid use was not correlated with any of the connectivity measures obtained in the
 468 resting-state functional connectivity analysis.



469

470 **Figure 7: The relation between the change in resting-state functional connectivity between**
 471 **auditory cortex and fusiform gyrus and the change in percentage of perceived McGurk illusions [6**
 472 **months – baseline measurement]. Data were pooled over ROIs in left and right hemispheres.**

473

474 **4. Discussion**

475 This pilot randomized controlled study investigated the effect of hearing aid fitting on audiovisual
 476 integration abilities in slight-to-moderate age-related hearing loss. For this aim, one group of hard-of-
 477 hearing participants was measured one week before and six months after fitting and use of hearing
 478 aids. The waiting control group was measured twice with a duration of six months between
 479 measurements and was not equipped with a hearing aid during that time. Our results provide
 480 evidence that six months of hearing aid use is associated with a decrease in functional connectivity
 481 between the auditory cortex and fusiform gyrus that is correlated with an increase in perceived

482 McGurk illusions. Furthermore, the increase in perceived McGurk illusions was correlated with a
483 decreased hearing aid benefit in auditory speech intelligibility.

484

485 **4.1 The effect of hearing aid use on the McGurk illusion**

486 Audiovisual integration abilities in hard-of-hearing participants were assessed with the McGurk
487 illusion. We hypothesized a decrease in the number of perceived McGurk illusions in the treatment
488 group compared to the control group after six months, arguing that regular hearing aid use might
489 lead to a bias towards the auditory percept – as in normal-hearing participants – rather than the
490 integration of incongruent audiovisual information (Gieseler et al., 2020; Rosemann and Thiel, 2018;
491 Stropahl and Debener, 2017). Our results demonstrated a positive trend of hearing aid use on the
492 McGurk illusion. However, in contrast to our hypothesis, the treatment group showed an increase in
493 perceiving the McGurk illusion over time when compared to the control group.

494 Previous research using the McGurk illusion in untreated, hard-of-hearing individuals has
495 demonstrated that they perceive the McGurk illusion more often than normal-hearing individuals
496 (Gieseler et al., 2020; Rosemann and Thiel, 2018; Stropahl and Debener, 2017). In line with those
497 studies, our results of the baseline assessment also showed a relatively high amount of McGurk
498 illusions in relation to the auditory percept in both our hard-of-hearing groups. Furthermore, we
499 extended previous results by varying the stimulus-onset asynchronies between the visual
500 information (lip movement) and auditory information (tone). We found that the participants of the
501 control and treatment groups integrated the incongruent information up to SOAs of 220 ms and 270
502 ms, respectively, at the baseline assessment. After six months, the treatment group reported more
503 McGurk illusions than their untreated peers, even up to temporal disparities of 320 ms. The effect
504 was, however, only significant at trend level. The results further showed, that along with an
505 increased McGurk illusion perception, the treatment group showed a 50% reduction in selecting the
506 visual input during McGurk trials, and only a reduction of 20% in selecting the auditory input. This

507 suggests that answers were less likely given for the visual input after six months of wearing a hearing
508 aid. Surprising was however that the McGurk illusion was still perceived more often and the auditory
509 input has been selected fewer than at the baseline assessment. It therefore seems that after hearing
510 aid use of 6 months, the auditory modality is not yet regarded as more reliable than before using the
511 hearing aid. Consequently, no increase in perceiving the auditory syllable, and thus no decrease in
512 McGurk illusion perception, was observed. A similar longitudinal study from Glick and Sharma (2020)
513 also found no change in benefit from visual cues in a speech-in-noise task after six months of hearing
514 aid use. However, the hard-of-hearing group did not significantly benefit from visual cues compared
515 to a normal-hearing control group at baseline, which probably explains the absent change of visual
516 benefit due to wearing a hearing aid. It is possible that a longer period of hearing aid use may cause
517 the auditory input to be perceived as the more reliable modality than the visual input, which may
518 also result in a decrease in the number of perceived McGurk illusions. Another explanation might be
519 that the individuals in the treatment group were measured without their hearing aids which created
520 a rather unusual and difficult listening situation in which the auditory input was not perceived as
521 reliable as with the hearing aids.

522 On a different note, it should be mentioned, that previous research showed rather large variability in
523 the susceptibility of the McGurk illusion (Magnotti and Beauchamp, 2018; Mallick et al., 2015).
524 Differences in susceptibility were attributed to age, gender, culture or native language (Magnotti and
525 Beauchamp, 2018) but also lip-reading abilities (Brown et al., 2018; Strand et al., 2014). Similarly,
526 high variation for fusion effects have been reported for other audio-visual paradigms as for instance
527 the sound-flash illusion (de Haas et al., 2012). Further, unlike other paradigms (such as the sound-
528 flash illusion), the McGurk effect uses syllables as stimuli, which constitute a rather naturalistic
529 setting closer to real world scenarios of audio-visual speech perception. Importantly, the test-re-test
530 correlation in the McGurk susceptibility with a duration of one year between measurements was
531 found to be high ($r=0.91$) in a sample of 165 participants (Mallick et al., 2014). Even though there is a
532 large inter-subject variability in the susceptibility to the McGurk illusion, the McGurk effect is

533 frequently used and probably the most popular paradigm to investigate audio-visual integration
534 (Tiippana, 2014). Despite evidence that McGurk susceptibility may not be a valid measure of
535 audiovisual integration (Van Engen et al., 2017), others found an increased McGurk susceptibility to
536 be related to an audiovisual benefit for sentences (Grant and Seitz, 1998) and to better audiovisual
537 speech in noise perception (Gieseler et al., 2020). Our results showed a positive correlation at trend
538 level between McGurk illusion and audiovisual speech in noise intelligibility, indicating better
539 audiovisual speech perception with more McGurk illusions. This correlation was present at baseline
540 (no hearing aid experience in participants), but not in the re-test assessment (when half of the
541 participants had hearing aid experience for six months). Hence, it seems that in elderly untreated
542 hearing-impaired participants, an increased McGurk illusion is associated with better audiovisual
543 speech perception. Interestingly, we found that an increase in McGurk illusion after hearing aid
544 fitting was related to a decreased improvement in auditory speech in noise intelligibility when tested
545 in an aided compared to unaided condition. This may suggest, that participants were still influenced
546 by the visual input which may have led to an increased McGurk illusion perception. That in turn
547 seems to inhibit the beneficial effect of the hearing aid when tested in auditory only conditions.
548 Thus, our results suggest that changes in McGurk susceptibility may be relevant for everyday life
549 speech comprehension and communication.

550 **4.2 Functional resting state changes associated with hearing aid use**

551 To assess changes in resting state functional connectivity of the auditory cortex with hearing aid use,
552 we computed an interaction analysis between group (treatment/control) x measurement time point
553 (baseline/after six months). We hypothesized a decrease in functional coupling of the auditory cortex
554 to visual brain regions after hearing aid use of six months (Chen et al., 2017; Kral et al., 2016;
555 Puschmann and Thiel, 2017; Shiell et al., 2015). This hypothesis was confirmed by our ROI-to-ROI
556 analysis that showed decreased auditory cortex coupling with the fusiform gyrus in the treatment
557 group. Moreover, we expected a change in number of perceived McGurk illusions and that this would
558 be associated with changes of functional connectivity between auditory cortex, the fusiform face

559 area and M1 lip area (Kanwisher and Yovel, 2006; Kanwisher et al., 1997; Murakami et al., 2018;
560 Rosemann et al., 2020; Schulte et al., 2020). While we found no significant changes in resting state
561 functional connectivity between the auditory cortex and M1 lip area, the change in connectivity
562 between the auditory cortex and fusiform gyrus was significantly different between treatment and
563 control group. The treatment group showed a significant decrease in connectivity, while the control
564 group showed no significant change (which led to a significant interaction of group x measurement
565 timepoint). Furthermore, this change was related to the perception of the McGurk illusion in the
566 treatment group.

567 Surprisingly, the decrease in functional coupling was linked to an increased number of perceived
568 McGurk illusions after six months of hearing aid use in the treatment group. In other words, we
569 found that hearing aid use was associated with 1) a decrease in resting state functional connectivity
570 between auditory and fusiform brain regions, and 2) that this decrease in connectivity was linked to
571 an increase in McGurk illusions. A recent study demonstrated that hard-of-hearing participants
572 compared to normal-hearing participants showed an increased task-modulated functional
573 connectivity between auditory and visual cortex for McGurk as compared to congruent audiovisual
574 stimuli (Rosemann et al., 2020). Other research has also provided evidence for an increased auditory
575 cortex coupling in hard-of-hearing individuals as a sign of cross-modal plasticity (Chen et al., 2017;
576 Kral et al., 2016; Puschmann and Thiel, 2017; Shiell et al., 2015). In a previous study investigating the
577 relationship between resting state functional connectivity and McGurk illusion rate, decreased
578 coupling between auditory and motor regions associated with an increased McGurk illusion rate was
579 demonstrated (Schulte et al., 2020). Hence, it seems that the perception of the McGurk illusion is
580 contrarily associated with functional connectivity between the auditory and motor cortex during the
581 actual McGurk task and between the auditory cortex and fusiform gyrus at resting state. While an
582 increased McGurk illusion rate was found to be associated with an increased functional connectivity
583 between the auditory and visual cortex in hard-of-hearing participants, this increased McGurk
584 illusion response was correlated with a decreased resting state connectivity between the auditory

585 and motor regions. Our study provides evidence that hearing aid use leads to a decrease in resting
586 state functional connectivity between the auditory cortex and fusiform gyrus, most likely indicating
587 less focus on visual input and more reliance on auditory input. However, this decrease was related to
588 an increase in McGurk illusion perception after six months of hearing aid use which was rather
589 surprising. A possible explanation might be that the treatment group was tested without their
590 hearing aids (as mentioned in 4.1). It is probable that these participants may have learnt to rely more
591 on the auditory input due to wearing the hearing aid in everyday life situations (leading to a decrease
592 in resting state functional connectivity between auditory and visual cortex). However, when being
593 tested without the hearing aids, they still may have paid more attention to the visual input which
594 might have led to an increase in McGurk illusion perception.

595 **4.3 Crossmodal plasticity**

596 Crossmodal plasticity in the auditory cortex has mainly been described in deafness (e.g. Lambertz et
597 al., 2005), but also in subjects with slight-to-moderate age-related hearing loss (Campbell and
598 Sharma, 2013; 2014). It was further shown, that neural coupling of the auditory cortex to visual areas
599 is increased as well (Chen et al., 2017; Kral et al., 2016; Puschmann and Thiel, 2017). However,
600 coupling of auditory and visual cortex was found to be decreased with longer durations of hearing aid
601 use in early-deaf individuals leading to the assumption that long term hearing aid use (of several
602 years) might inhibit crossmodal reorganization (Shiell et al., 2015). Other research in cochlear
603 implant patients (Giraud and Lee, 2007; Lee et al., 2007; Sandmann et al., 2012) and hard-of-hearing
604 individuals (Campbell and Sharma, 2014) has shown a negative relation between crossmodal
605 plasticity in the auditory cortex and speech perception outcome. Hence, the visual takeover of the
606 auditory cortex has been described as maladaptive and it has been suggested that an incomplete
607 reversal of this crossmodal plasticity might interfere with the clinical benefit of a cochlear implant or
608 a hearing aid (Sandmann et al., 2012). However, crossmodal plasticity in the visual cortex has been
609 shown to benefit speech perception outcome after cochlear implantation (Chen et al., 2015; Giraud
610 et al., 2001a, 20001b). Similarly, an increased crossmodal plasticity in the auditory cortex was also

611 found to be correlated with audiovisual integration strength in cochlear implant users (Stropahl and
612 Debener, 2017). Hence, there seems to be adaptive and maladaptive plasticity when it comes to
613 speech perception outcome in cochlear implant patients. Unfortunately, studies assessing
614 crossmodal plasticity before and after hearing aid fitting in mild to severe age-related hearing loss
615 are limited. A recent electroencephalography study showed a reversal of auditory cross-modal
616 reorganization after six months of hearing aid treatment (Glick and Sharma, 2020). They further
617 showed that latencies of the right auditory cortex before hearing aid fitting predicted auditory
618 speech perception outcomes six months after hearing aid use (more crossmodal plasticity predicted
619 worse speech perception). A recent resting state functional connectivity study provided evidence of
620 an increased connectivity between right Heschl's gyrus and frontal cortex that also correlated with
621 executive function improvement 6 months after hearing aid use (Ponticorvo et al., 2021). However,
622 neither was the hypoperfusion of the Heschl's gyrus that was found before the hearing aid fitting
623 reversed, nor did speech perception improve in the follow up measurement of the treatment group.
624 Thus, it is currently not clear, how much sensory loss (degree and length of hearing loss) induces
625 crossmodal plasticity in age-related hearing loss and whether these changes predict good or bad
626 hearing aid benefit for speech perception (Stropahl et al., 2017).

627 Moreover, crossmodal plasticity has not only been shown in terms of neural activity in the auditory
628 cortex, but there are several studies assessing functional connectivity of the auditory cortex during
629 different tasks (Chen et al., 2017; Kral et al., 2016; Puschmann and Thiel, 2017; Rosemann and Thiel,
630 2018) or resting state (Chen et al., 2018; Husain et al., 2014; Puschmann and Thiel, 2017; Rosemann
631 and Thiel, 2019; Schmidt et al., 2013; Schulte et al., 2020). Resting state functional connectivity
632 measures temporal correlations of spontaneous activity between brain regions that are organized
633 into coherent networks (Husain et al., 2014). So-called resting state networks such as the default
634 mode, the dorsal attention and the salience network have been found to be reliably detectable and
635 consistently reproducible by previous research and thus have gained attention in a variety of
636 disorders (Smitha et al., 2017; Yang et al., 2020). In contrast to task-based functional neuroimaging,

637 the benefits of resting state measurements are the short acquisition times (~10 minutes) and that
638 results are not confounded by performances in the task. Important for clinical research is that some
639 patient populations such as stroke patients or infants may not be able to perform certain tasks and
640 hence task-based fMRI is not applicable in those patient groups (Canario et al., 2021; Zhang et al.,
641 2019). Further, resting state fMRI allows assessments of functional coupling between specific
642 regions, resting state networks and the whole brain whereas task-based fMRI is limited to neural
643 activity and functional connectivity of brain regions elicited by the particular task (Canario et al.,
644 2021). In our study, we were able to show that functional coupling of the auditory cortex to visual
645 cortex is altered after 6 months of hearing aid use suggesting more widespread changes in underlying
646 network dynamics (that not only affect the auditory cortex during auditory processing).

647 **4.4 Limitations**

648 It seems that hearing aid use in age-related hearing loss is associated with observable neural changes
649 in the auditory cortex that are linked to an increased McGurk illusion response already after a
650 relatively short period of six months. However, we need to point out some limitations of the current
651 study. On the behavioral level, some of the behavioral results were only significant at trend level (for
652 instance increase in McGurk illusions over time, or the relation between McGurk illusions and
653 audiovisual speech in noise intelligibility). This may be due to the small sample sizes and the large
654 variability in the McGurk illusion. A complicating factor that may also serve as an explanation for that
655 result is the fact that the McGurk illusion in the treatment group was only tested in an unaided
656 condition. We chose to measure the treatment group in an unaided condition to enable
657 comparability between groups and to assess potential general changes that are not associated with
658 specific hearing aid settings. Although the level of stimulus presentation was individually adapted for
659 all participants, we cannot exclude that this created a rather unusual and difficult listening situation,
660 in which the auditory input was not perceived as reliable as with the hearing aids. Due to time limits,
661 we were unfortunately not able to conduct both aided and unaided assessments. Regarding the
662 resting state connectivity data, we only observed a significant change in resting-state connectivity in

663 our ROI-to-ROI analysis and not in the whole-brain analysis. A possible explanation might be lack of
664 power due to the small sample size. Hence, the interaction between group and measurement
665 timepoint was shown to be significant in the ROI-to-ROI analysis but might not have survived the
666 correction for multiple comparisons in the whole-brain analysis. Thus, this study can only be seen as
667 a pilot study. However, the results may trigger future research on the influence of hearing aid fitting
668 in age-related hearing loss. How long-term use of a hearing aid (> 1 year) influences cross-modal
669 plasticity in mild to moderate hearing loss and how this relates to speech perception outcomes
670 should be investigated by future research. Further, future studies should consider assessing
671 audiovisual integration in aided and unaided conditions in hearing aid users as well as larger group
672 sizes.

673 **4.5 Conclusion**

674 This is the first study to provide pilot data on the effect of hearing aid fitting on the McGurk illusion
675 and resting state functional connectivity. We demonstrated that hearing aid use is associated with
676 changes in resting state functional connectivity between the auditory cortex and fusiform gyrus,
677 which is also related to the increased number of perceived McGurk illusions. We also found a relation
678 between increased McGurk illusion and decreased hearing aid benefit in auditory speech in noise
679 intelligibility. Our study therefore offers valuable insights into alterations in resting state functional
680 connectivity and changes in audiovisual integration (susceptibility to the McGurk illusion) and speech
681 perception after six months of hearing aid use.

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